

Monitorage hémodynamique pédiatrique

Les pièges à éviter !

Pr Wodey Eric, MD, PhD

CHU de Rennes

France

eric.wodey@chu-rennes.fr

Pas de conflits d'intérêt

Pas de contrat avec l'industrie

Pas de compte en Suisse ;-)

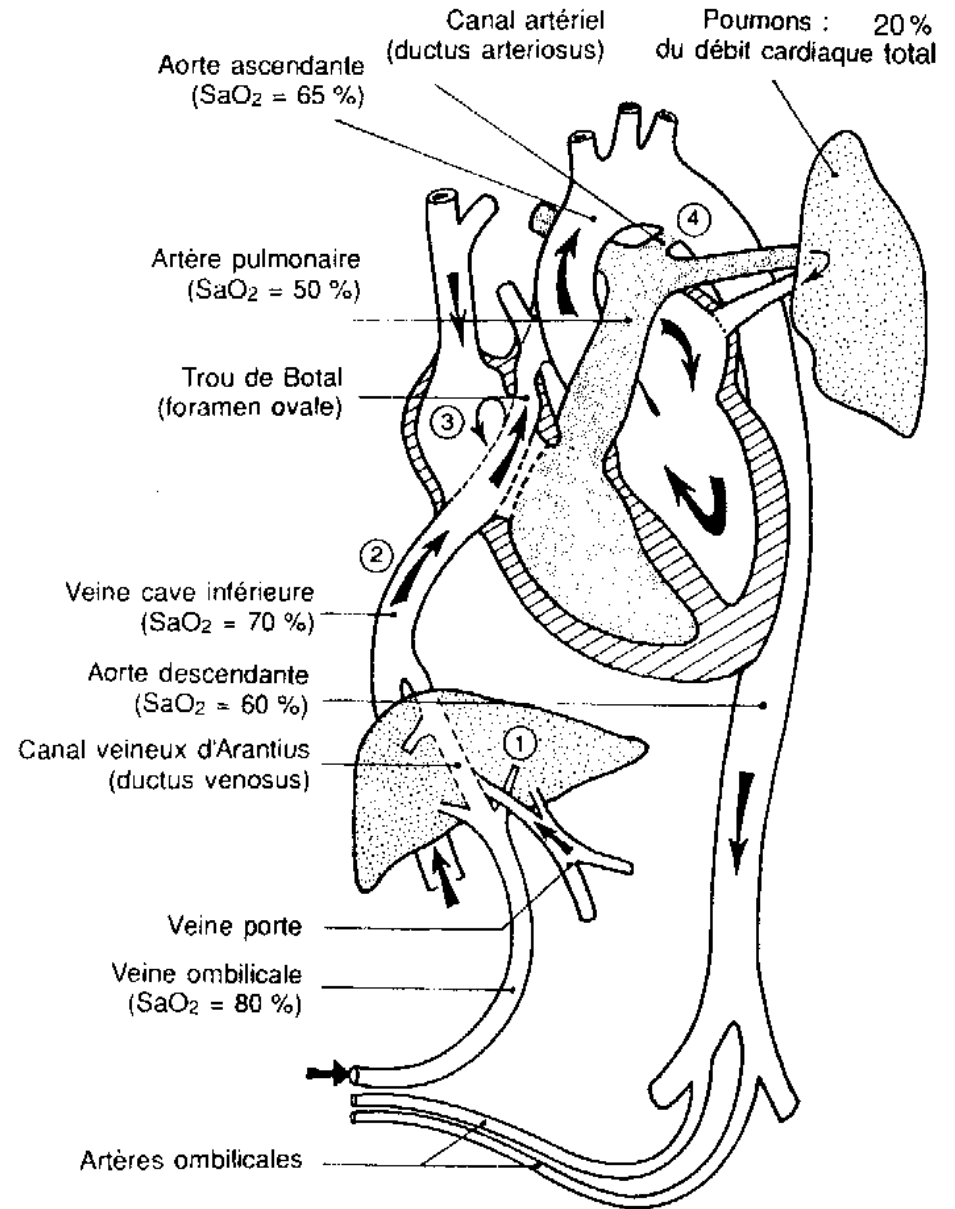
I PHYSIOLOGIE

Transition



Transition

- Aération pulmonaire
 - PaO_2
 - RAP
- Clampage du cordon
 - RAS
- Fermeture shunts
- « Resetting »
- Instabilité
 - catécholamines

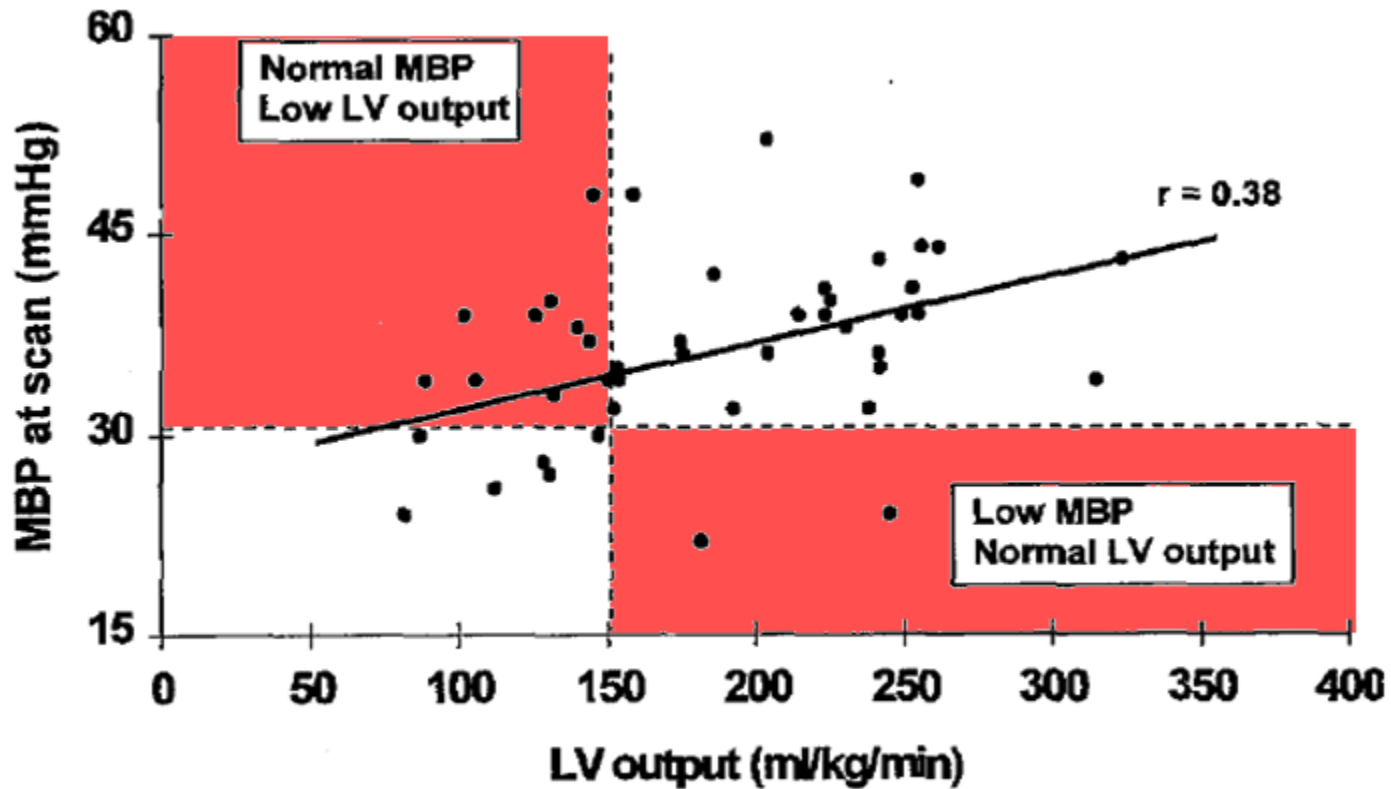


Mécanismes d'hypoTA

NN <24h, 27-32SA

- Bas débit (n = 4) 24%
 - Dysfonction myocardique (<1/2 des cas)
 - RAP élevée (précharge VG basse+ dysfct septale)
 - Hypovolémie (test d'expansion volémique) ➔ RARE
- Débit non bas (n=13) 76%
 - CA significatif associé dans >3/4 des cas (11/13)
 - cinétique ventriculaire toujours normale
 - Diminution isolée des RAS (1/17)

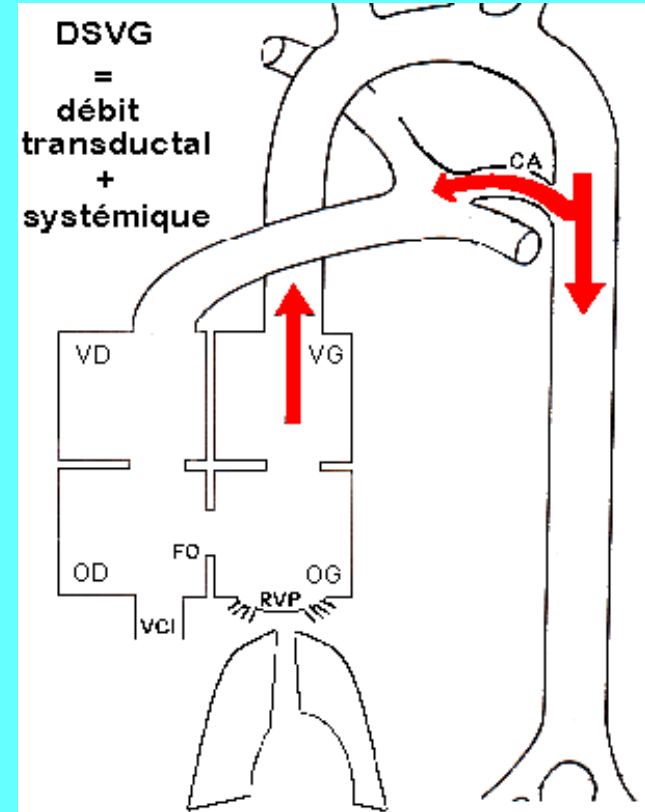
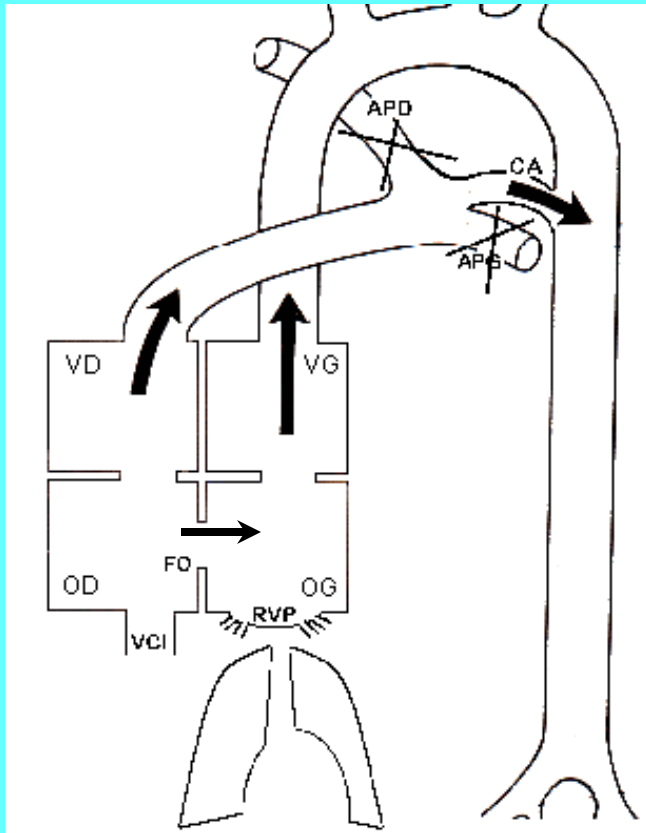
La PA n'est pas la perfusion



45 prématurés <1500g
APN<36h
Intubés ventilés
CA fermé ou <1.5mm

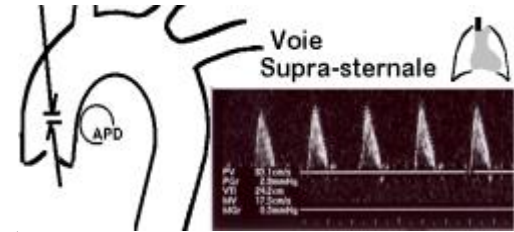
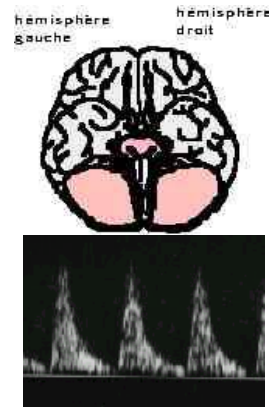
Canal artériel

Évolution hémodynamique



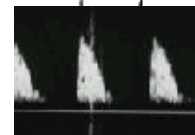
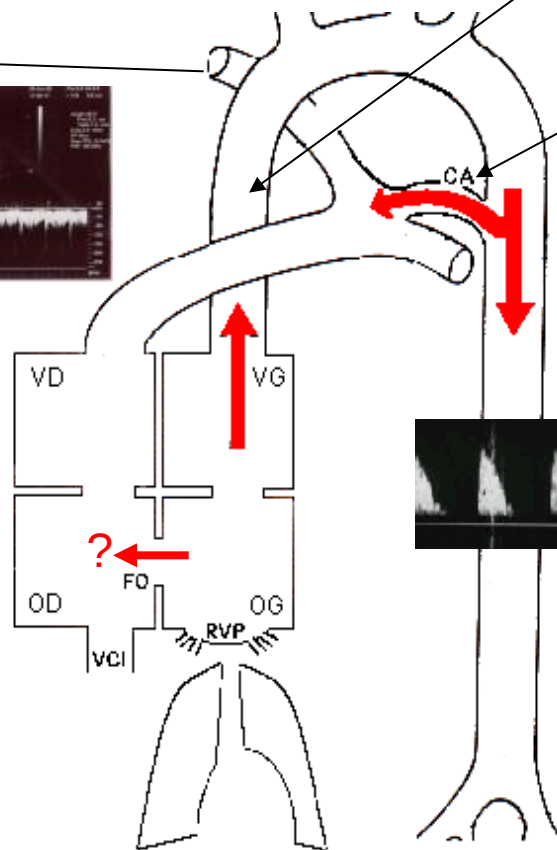
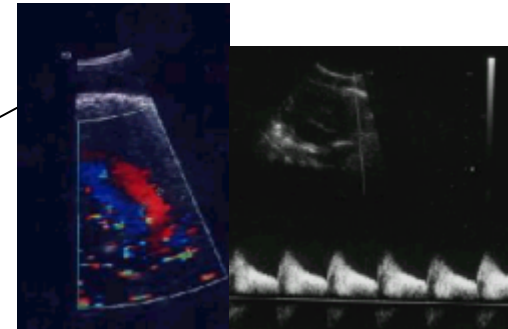
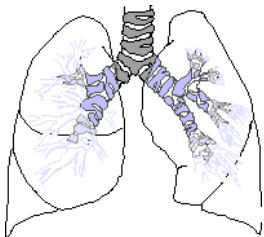
Canal artériel tubulaire

DSVG = D Syst + transductal

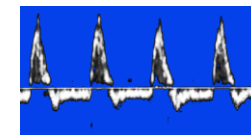


HTAP de débit

Séquestration volémique



ou



↗ pulsatilité

vol systémique

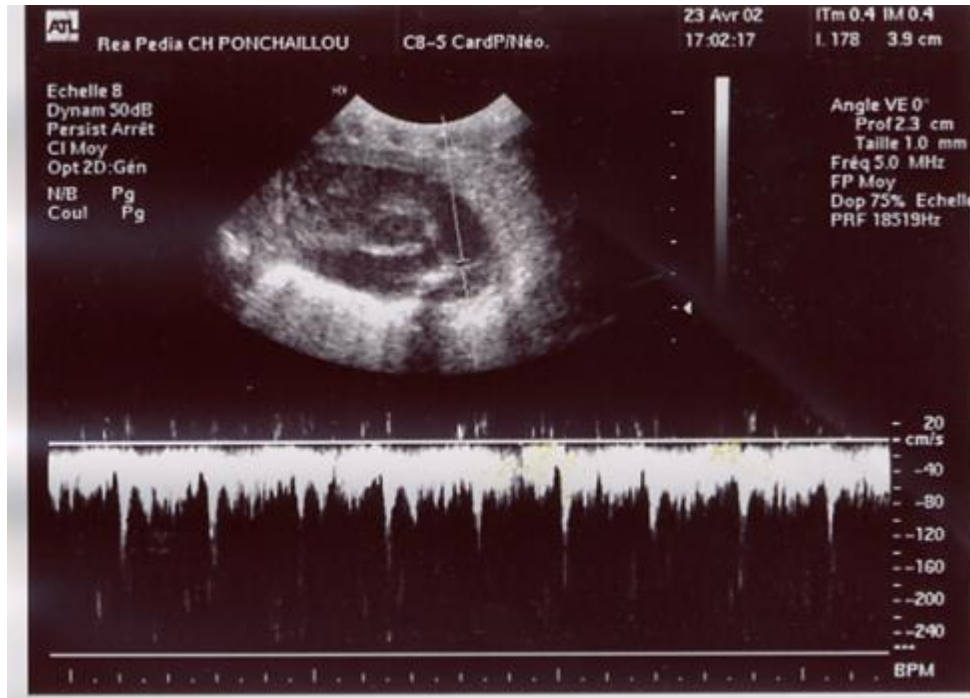
↘ PA,

↘ perfusion d'organes

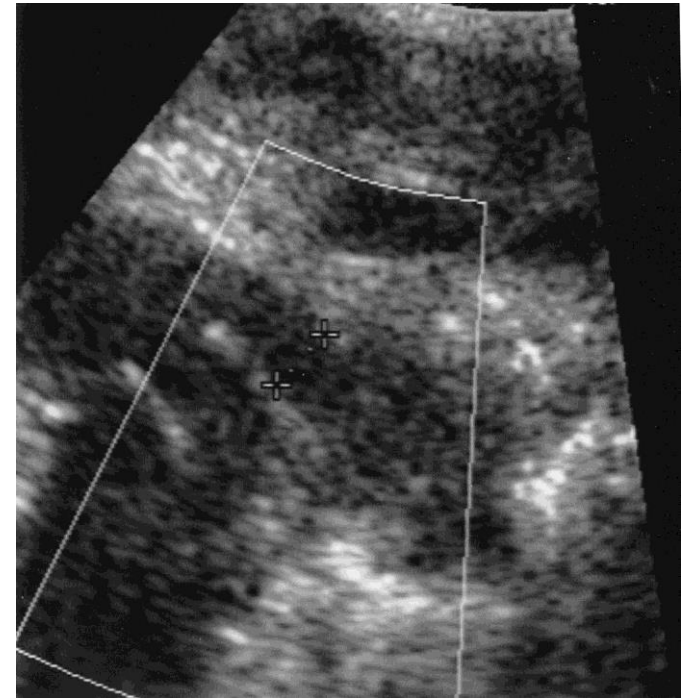
↗ RAS

↗ instabilité hémodyn.

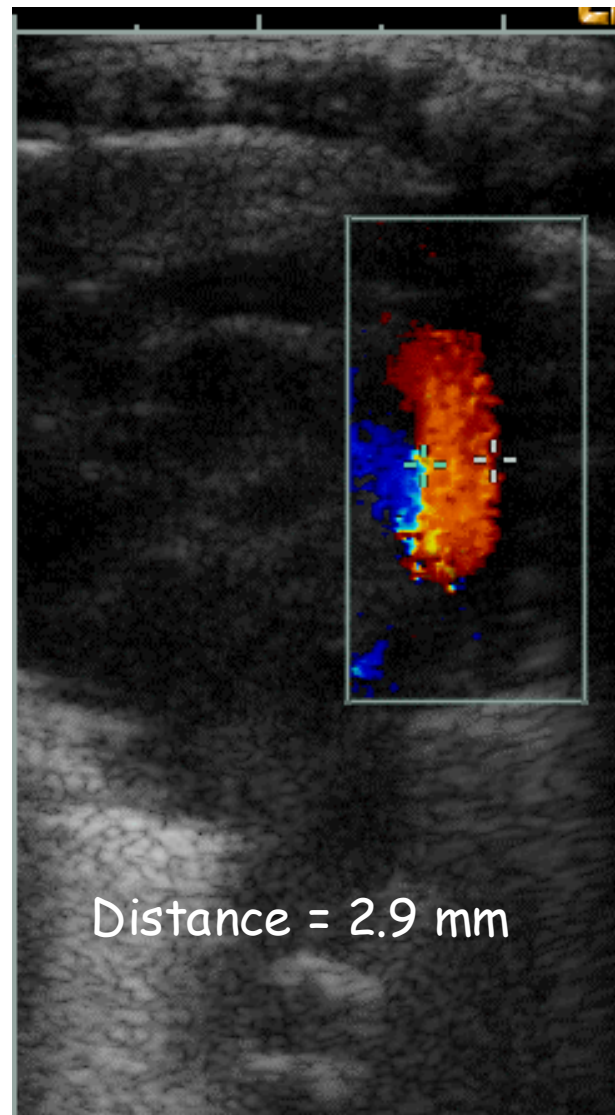
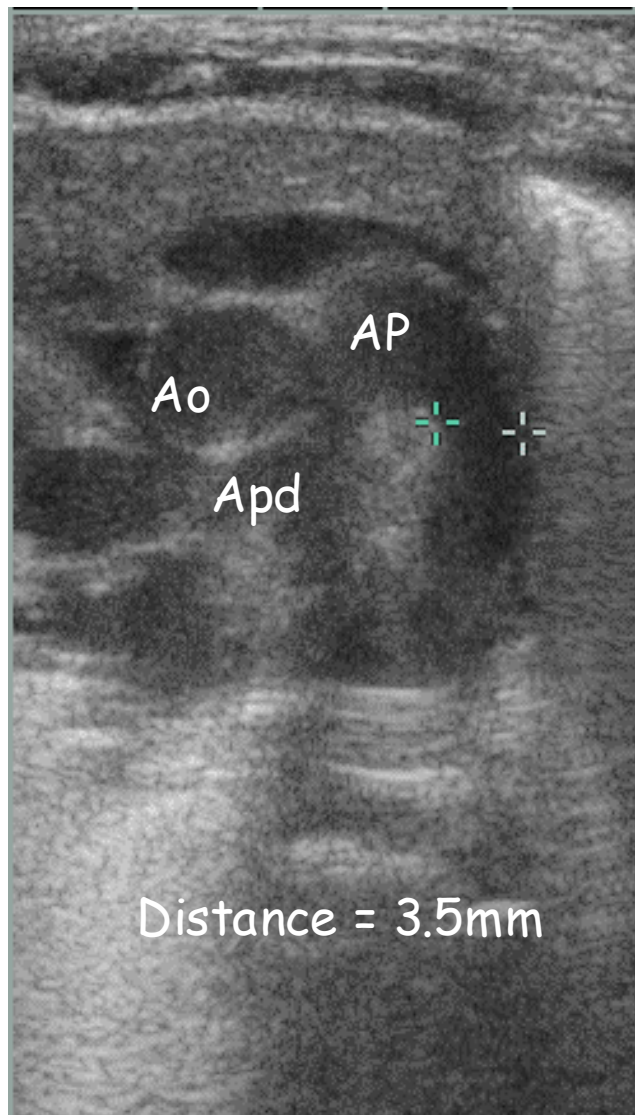
Le CA est il ouvert?



Hyperdébit pulmonaire



« Patte de canard »



Voie: parasternale haute, diamètre interne

Hémodynamiquement significatif ?

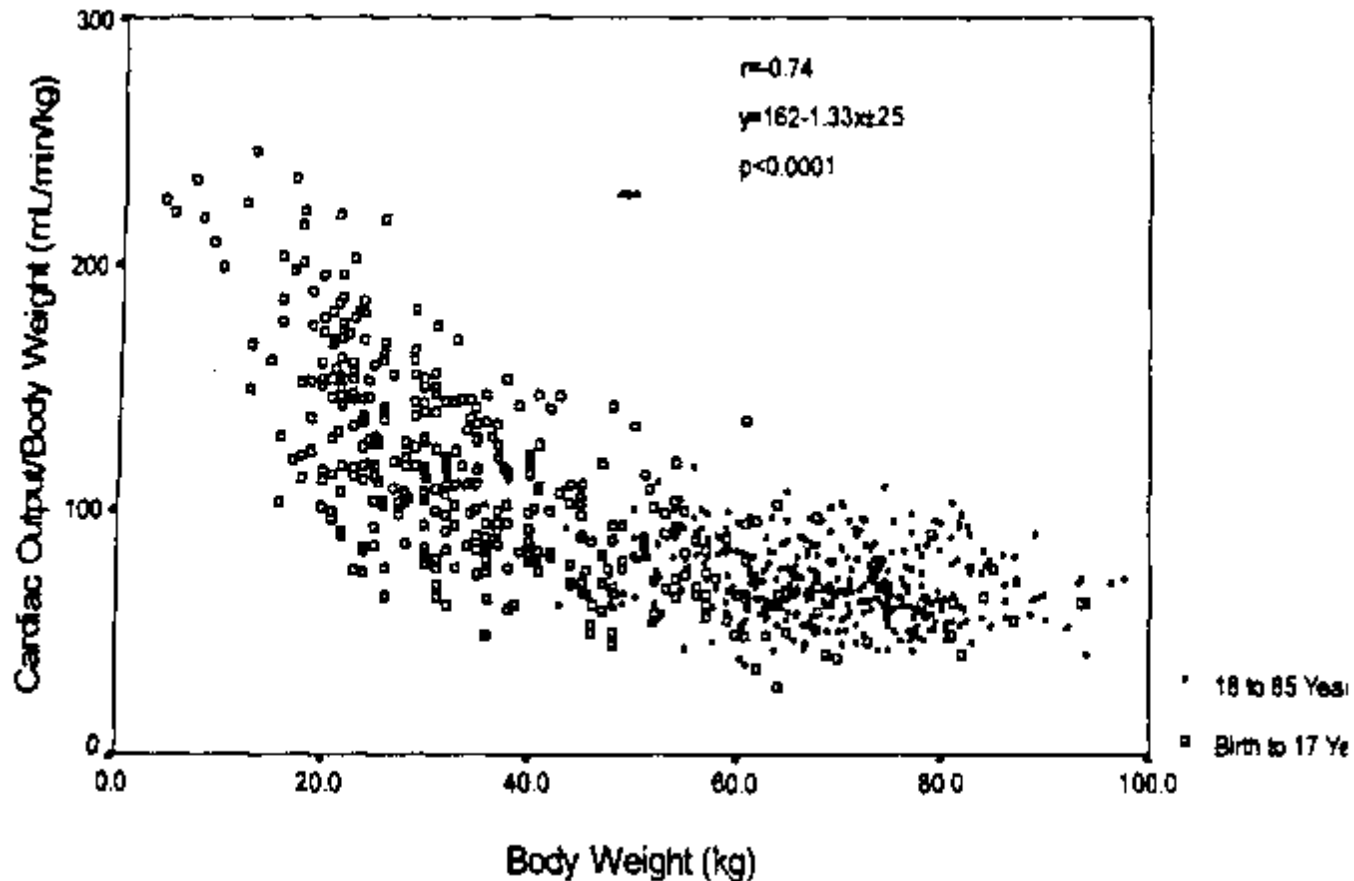
- Diamètre
 $>1.4 \text{ mm/kg}$
 Evans 1995: $>2 \text{ mm}$, risque évolutif entre 1.5 et 2 mm
- OG/Ao
 > 1.4
- V_{moyAPG}
 $>0.5 \text{ m/sec}$ (ou $V_{\text{diast APG}} >0.2 \text{ m/sec}$)
- PAM
 $<10^{\text{ème}}$ percentile
- Flux diastolique absent ou rétrograde dans l'Aorte descendante (sous ductale)
 - $Q_p/Q_s = 1.3 \pm 0.11$ si abs.
 - $Q_p/Q_s = 1.6 \pm 0.18$ si rétr.*Evans J Pediatr 19994*
- Classification de SU
 - Aspect croissant ou pulsatile
- ➡ flux de VCS ($<40 \text{ ml/kg/mn}$)

Au delà d'un mois....

... encore quelques évolutions.

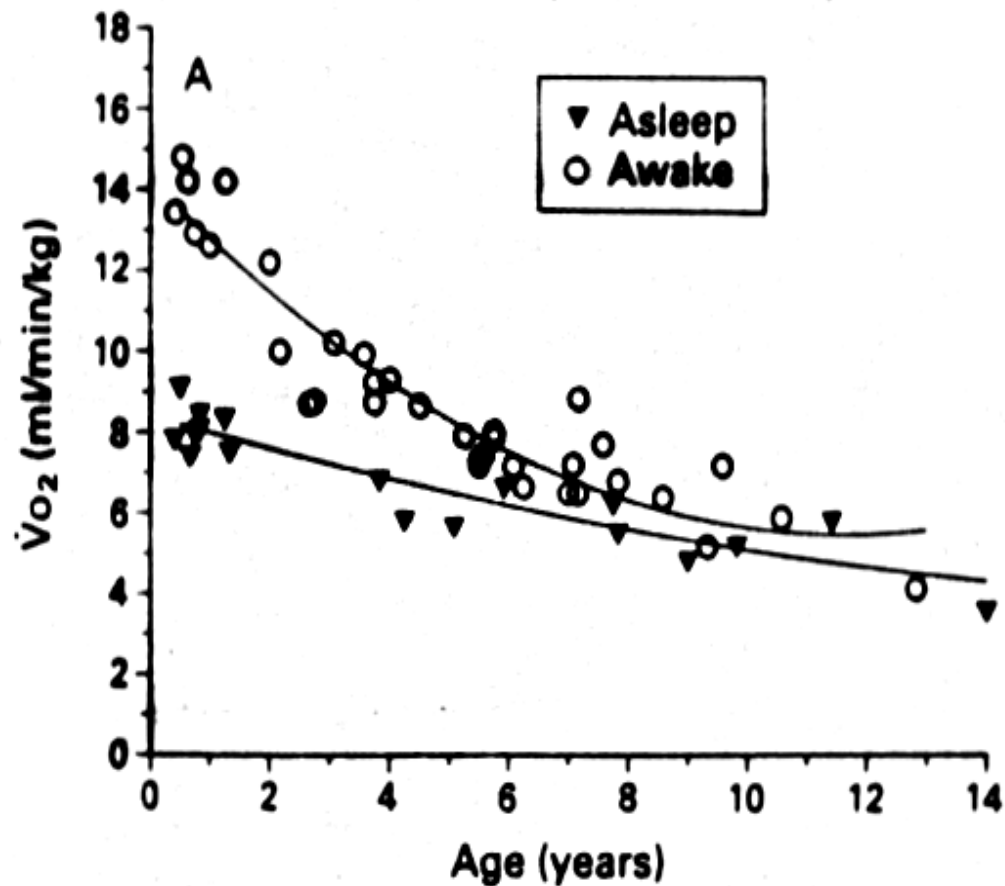


Index cardiaque / poids



de Simone et al. Circulation 1997

VO₂ Enfant



Childs C. Arch Dis Child 1993

Attention: Effet « croissance »

Toutes les variables physiologiques
ne sont pas liées « linéairement » à
l'âge ou au poids!

« Volumes » Respiratoires

Paramètres	1 semaine	1 an	3 ans	5 ans	8 ans	12 ans	
Taille (cm)	48		75	96	109	130	150
Poids (kg)	3,3		10	15	18	26	39
CRF (ml)	75		263	532	660	1174	1855
CRF (ml.kg-1)	25		26	37	36	46	48
Capacité Vitale (ml)	100		475	910	1100	1855	2830
VE (ml.min-1)	550		1775	2460	2600	3240	4150
VT (ml)	17		78	112	130	180	260
VT (ml.kg-1)	6		7,5	7,5	7,5	7	6,5
Fréquence	30		24	22	20	18	16

Morbidity per Op / âge (n = 29220)

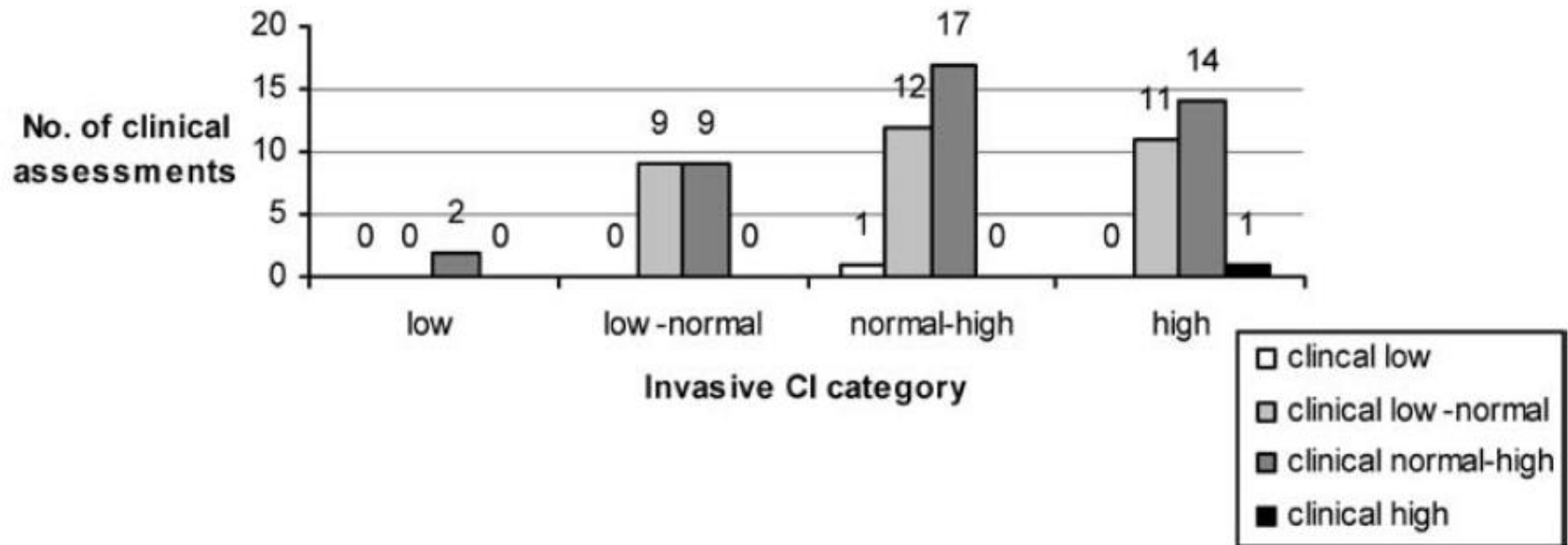
	Age									
	<1 mo (n = 361)		1-12 mo (n = 2,544)		1-5 yr (n = 13,484)		6-10 yr (n = 7,184)		11+ yr (n = 5,647)	
	n	Rate	n	Rate	n	Rate	n	Rate	n	Rate
None	308	8,532	2,368	9,308	12,585	9,333	6,381	8,882	5,126	9,077
Vomiting	1	28	12	47	76	56 ^a	71	99	77	136 ^a
Arrhythmia	6	166	22	86	527	391	670	933	317	561
Blood pressure	14	388 ^a	14	55	30	22 ^a	14	19	26	46
Temperature	3	83	6	24	18	13	6	8	9	16
Cardiac arrest	1	28	3	12	4	3	3	4	3	5
Airway obstruction	8	222	51	200 ^a	133	99	62	86	51	90
Other respiratory	26	720 ^a	81	318 ^a	159	118	59	82 ^a	56	99
Drug incident	0		5	20	27	20	20	28	20	35
Surgical	1	28	8	31	53	39	31	43	22	39
Death	3	83 ^a	2	8	4	3	1	1	1	2

*Cohen MM et al, Anesth
Analg 1990*

Les pièges du MONITORING

Jonathan R. Egan
Marino Festa
Andrew D. Cole
Graham R. Nunn
Jonathan Gillis
David S. Winlaw

Clinical assessment of cardiac performance in infants and children following cardiac surgery

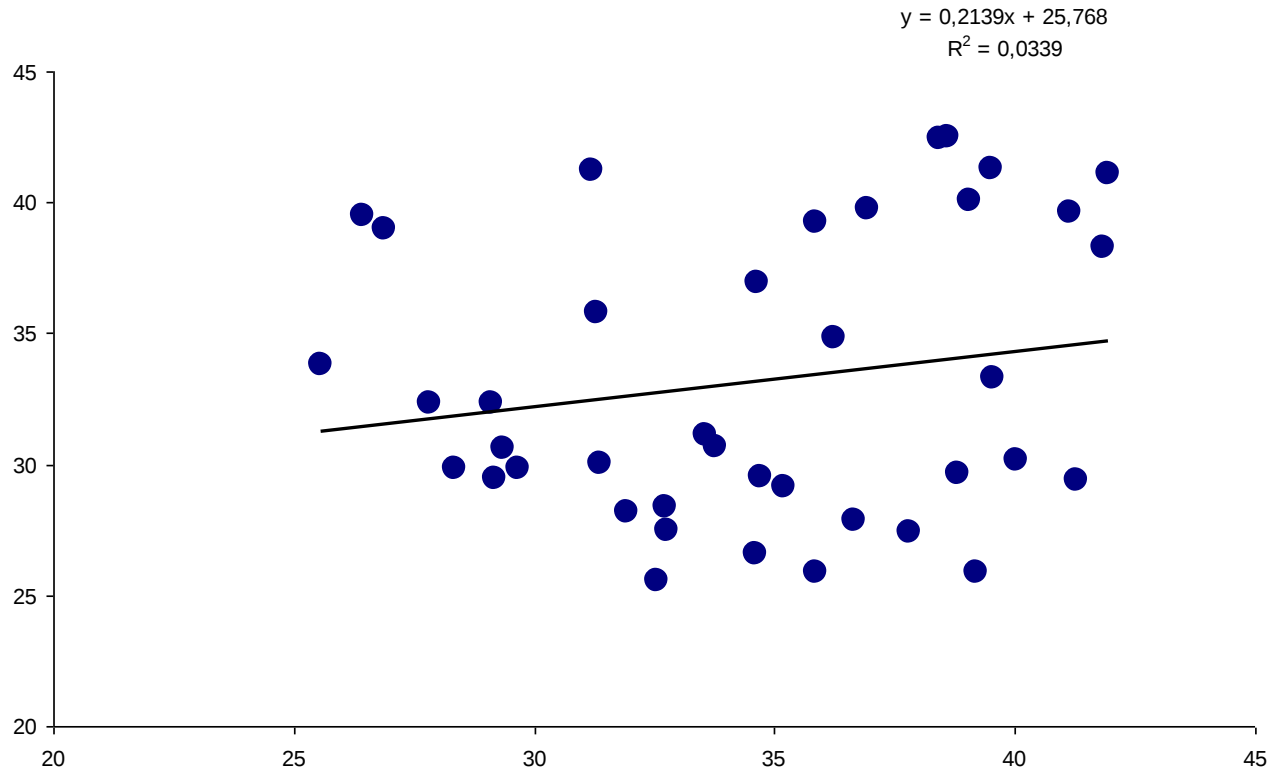


Monitoring : Pourquoi ?

Monitoring: les pièges de bases

Un peu de mathématique...

UA



- Deux séries de variables aléatoires
- de 25 to 42
- Pas de lien entre les variables

UA

Pas de lien

Serie 1 :

Variables a **aléatoires**

x SC
(0,1 to 2 m²)

Serie 2 :

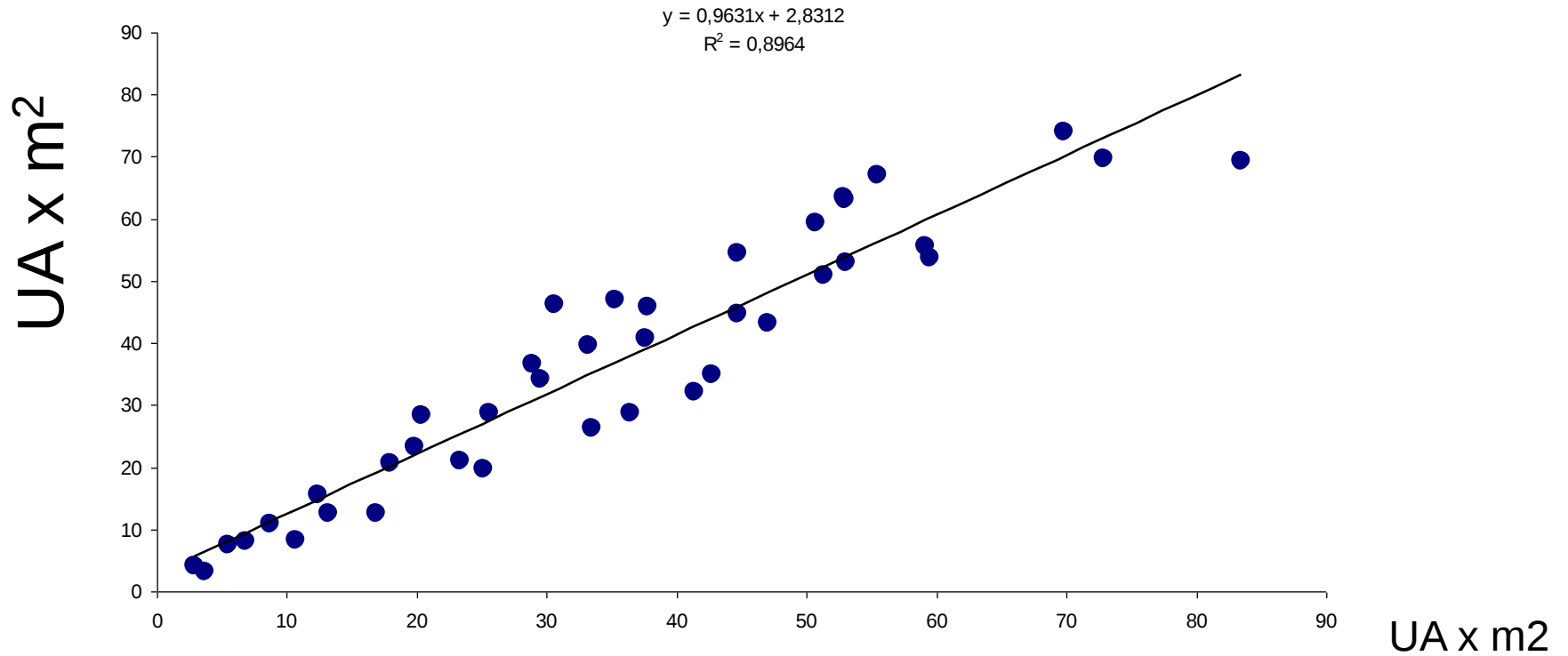
Variables b
aléatoires

Série 1bis :

Série 2bis :

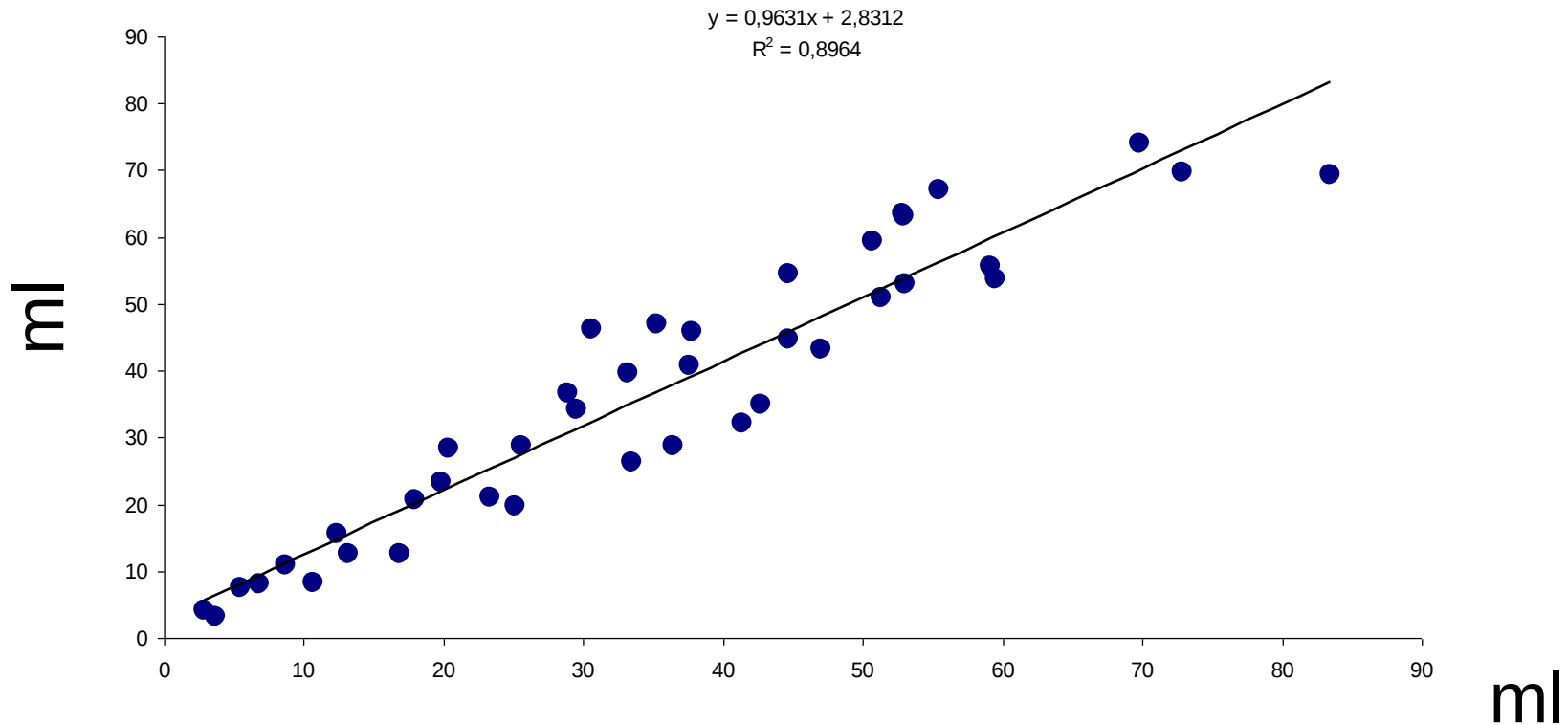
Lien fort

Lien séries 1 bis et 2 bis



$$\boxed{\text{ml/m}^2} \times \text{m}^2 = \text{ml}$$

Lien entre deux variablesà l'origine aléatoires



Pas de lien

Serie 1 : **VESi**
aléatoire

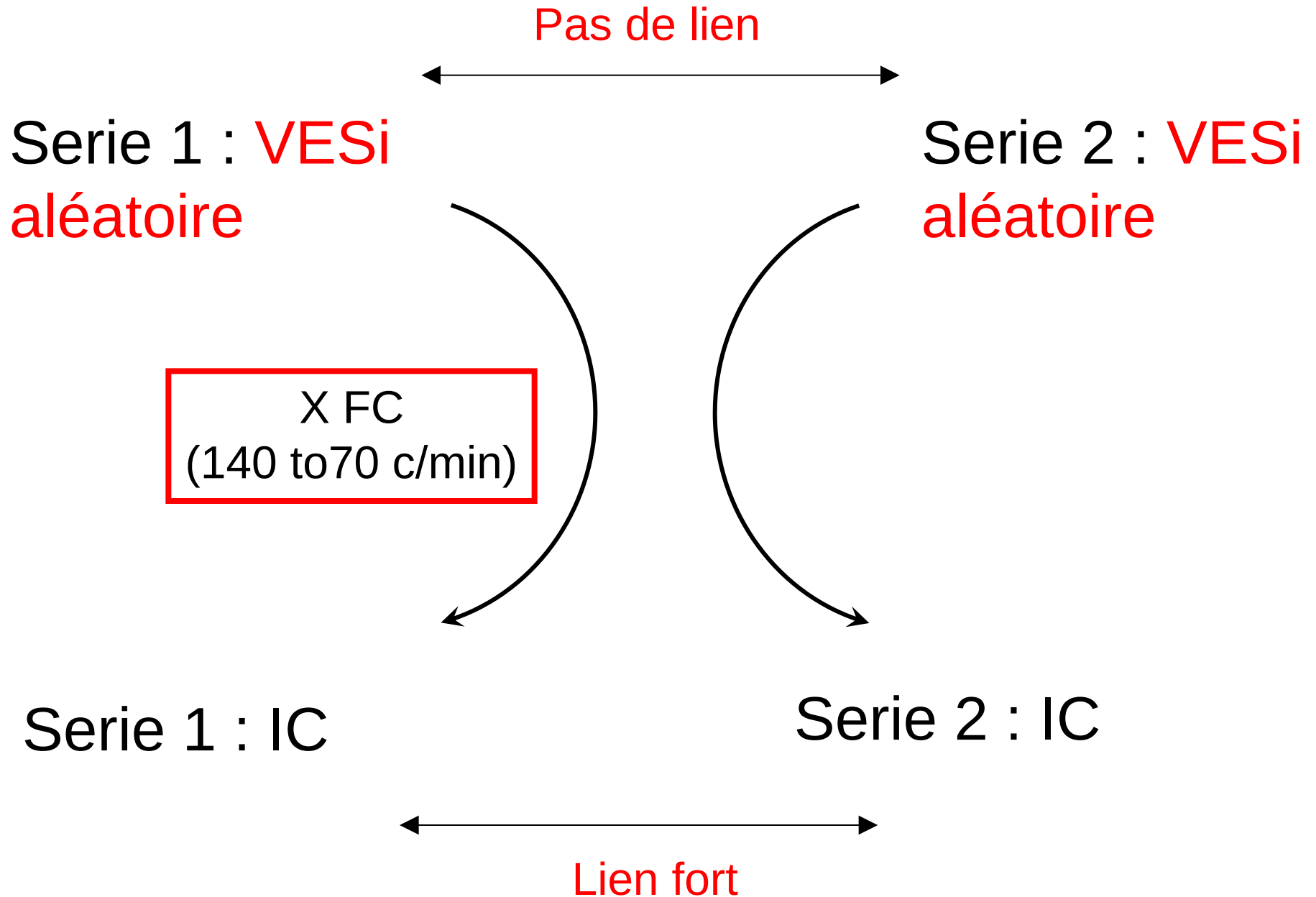
Serie 2 : **VESi**
aléatoire

X FC
(140 to 70 c/min)

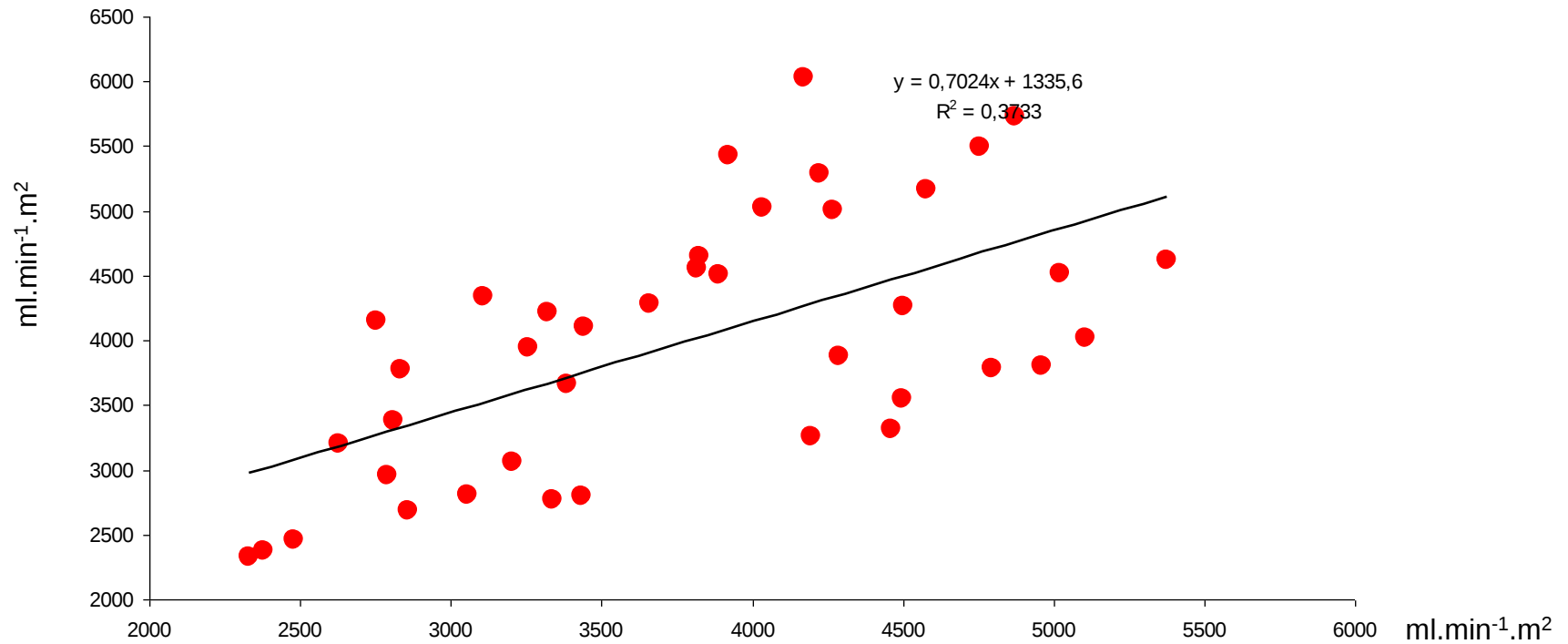
Serie 1 : IC

Serie 2 : IC

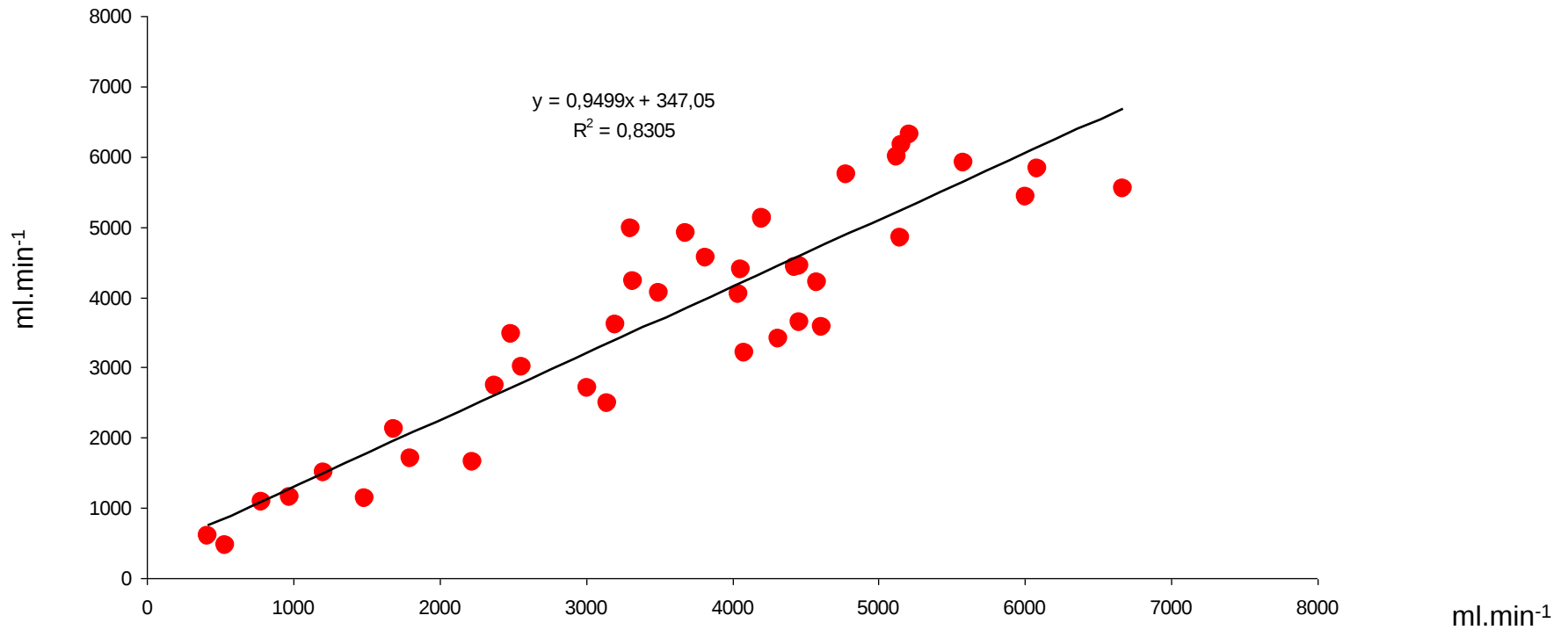
Lien fort



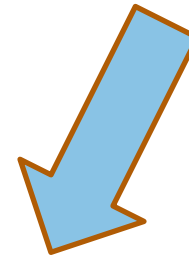
Index cardiaque



Débit cardiaque



“Mesuré”



VES i (ml.m⁻²)

SC

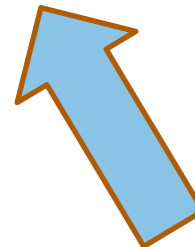
VES (ml)



IC (ml.min⁻¹.m⁻²)

SC

Q (ml.min⁻¹)



“Mesuré”

D'un point de vue scientifique, pour un calcul juste, il est important de faire attention aux unités !

Hauteur: m

Surface: m^2

Volume: m^3

Débit:

$\text{cm}^3/\text{min}(\text{Volume}/\text{Temps})$

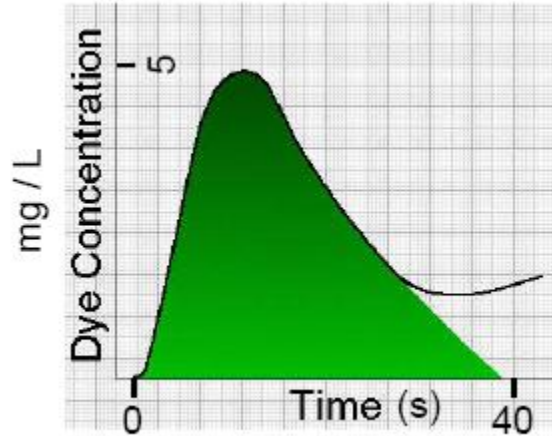
Vitesse : m/sec

(Distance/temps)

Le résultat d'un calcul de vitesse ne peut pas s'affranchir des unités (Kg ?)

Sinon, c'est une approximation...

Dye dilution



Calcul:

$$Q = (\text{masse} / \text{aire de dilution}) \times 60$$

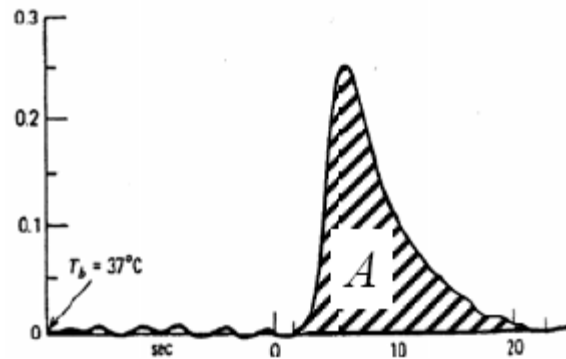
$$m = 5 \text{ mg}$$

$$A = 61 (\text{mg} \cdot \text{L}^{-1}) \times \text{sec}$$

$$Q = ((\text{mg} / (\text{mg} \cdot \text{L}^{-1})) \times \text{sec}) \times 60$$

$$\Rightarrow Q = 4.9 \text{ L/min}$$

Thermodilution



$$Q = V (T_b - T_i) \times (0.891) / \text{area of } T^\circ$$

$$T_{\text{bang}} = 37^\circ \quad T_{\text{injection}} = 5^\circ$$

$$V_{\text{volume injection}} = 5 \text{ ml}$$

$$\text{Aire (A)} = 1.7 ^\circ\text{C} \cdot \text{sec}$$

$$Q = (\text{ml} \times (\Delta C^\circ)) / C^\circ \cdot \text{sec} \times 60$$

$$\Rightarrow Q = 4900 \text{ mL/min}$$

$$= 4.9 \text{ L/min}$$

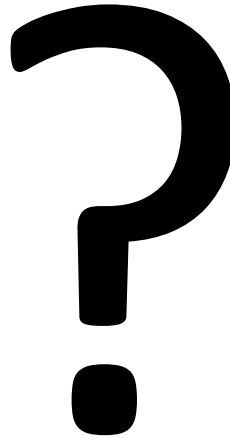
Variable

“Estimée....”

Pas de correspondance des unités

“Calculée”

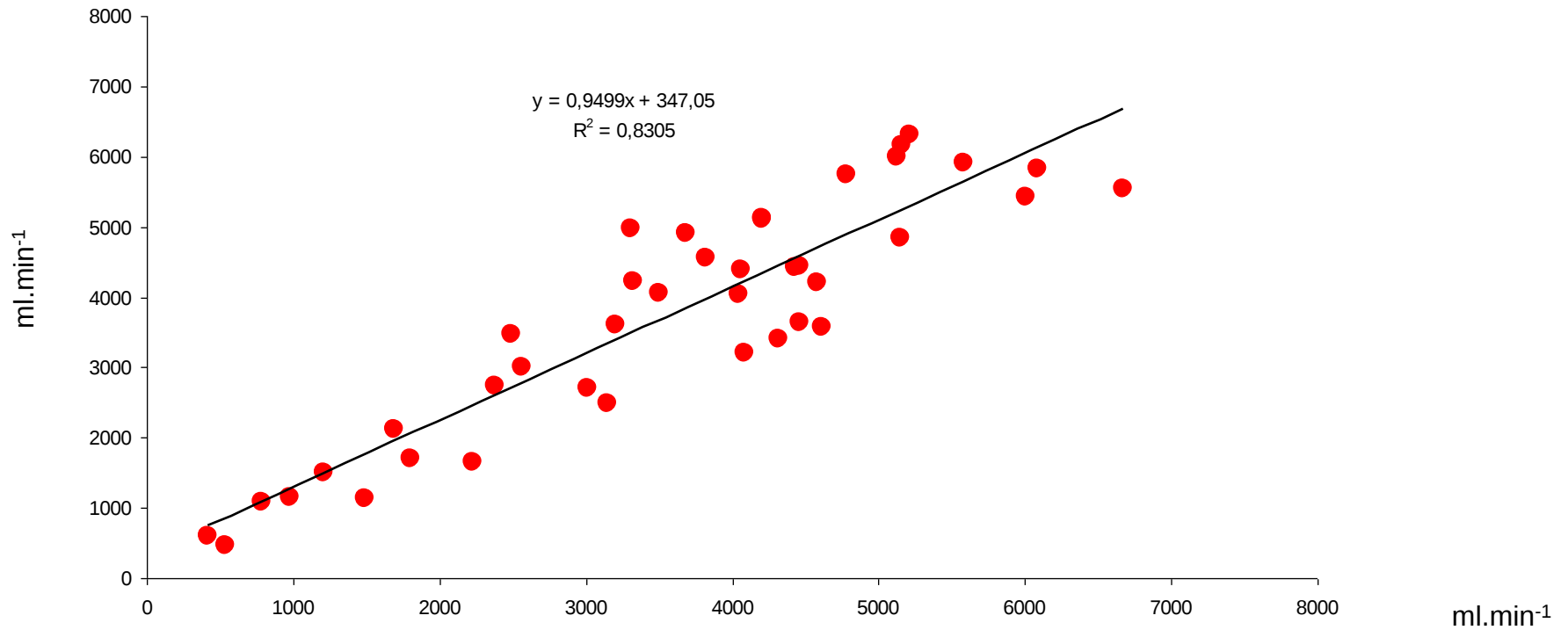
Avec correspondance des unités



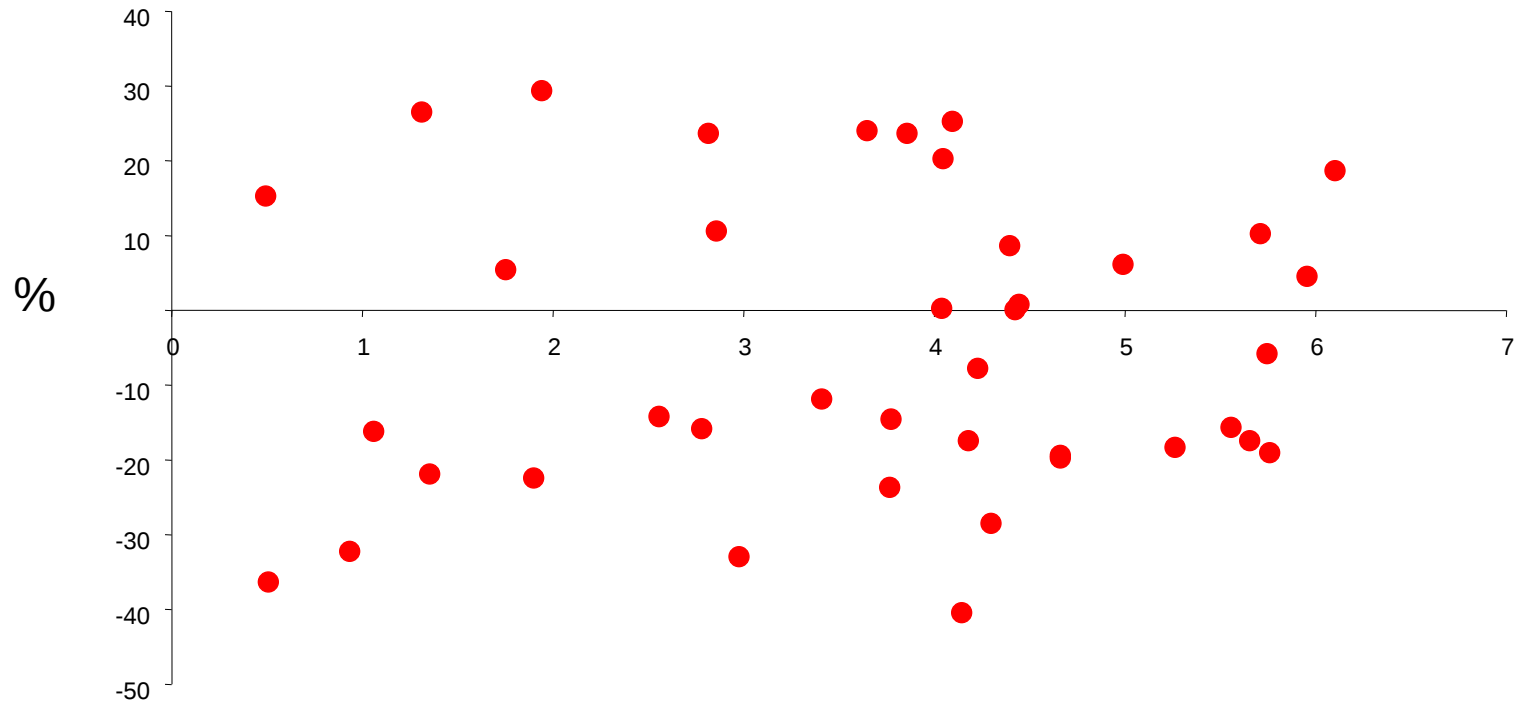
Variable

Variation

Débit cardiaque



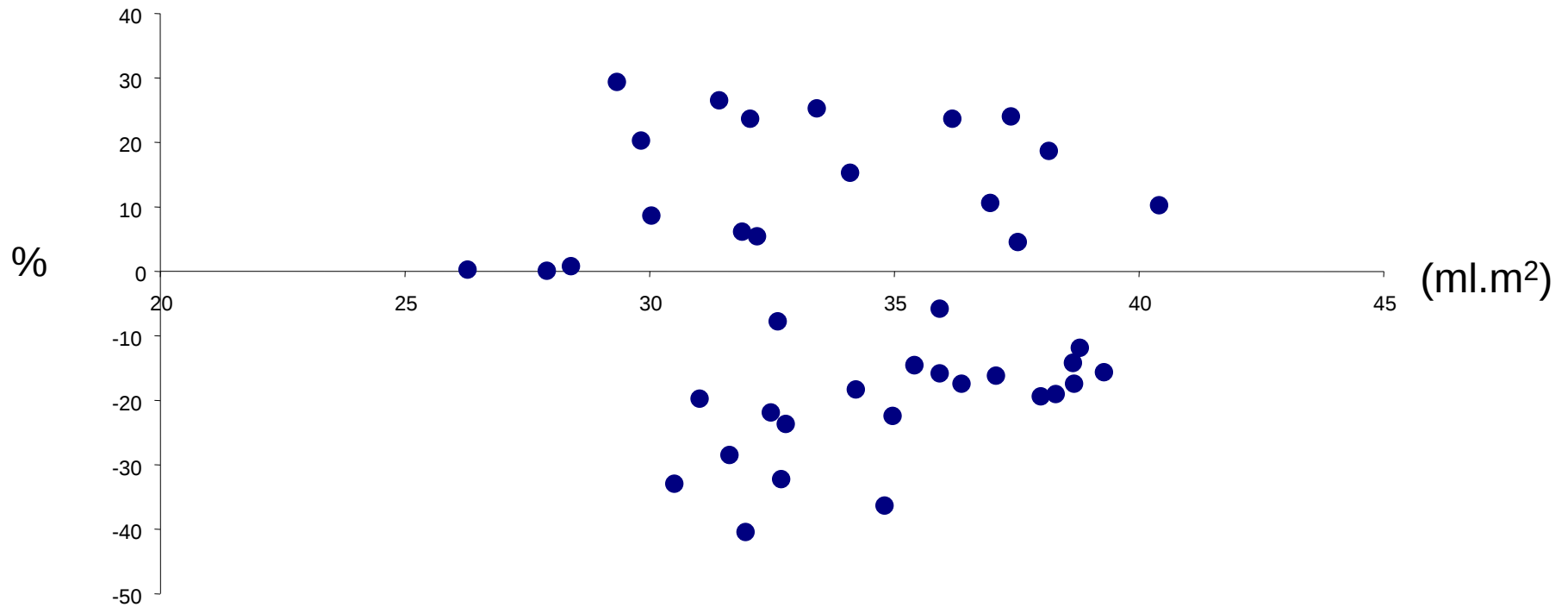
Bland & Haltman (% variation) Débit cardiaque



Biais – 0,05%
Limites d'agrément +/- 40%

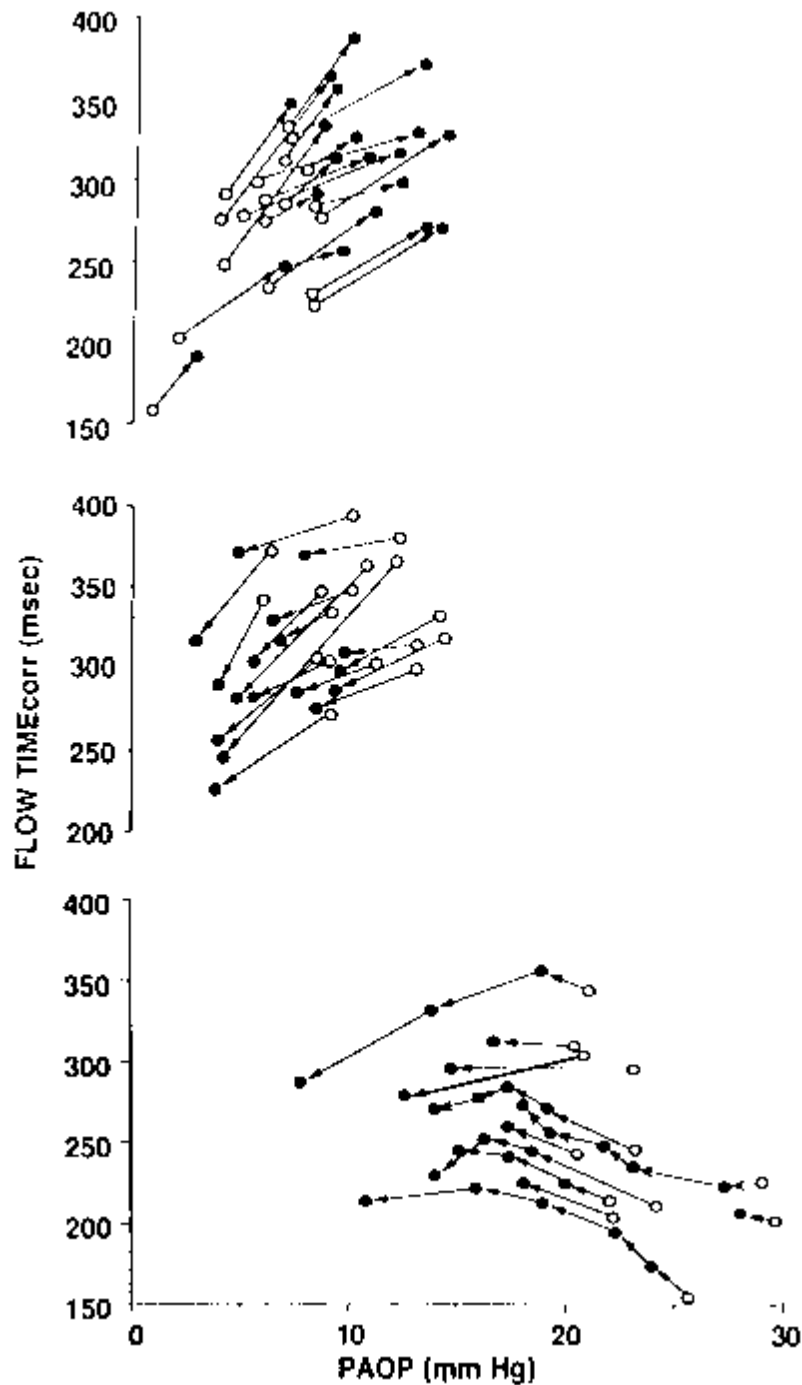
Bland & Haltman (% variation)

VESi

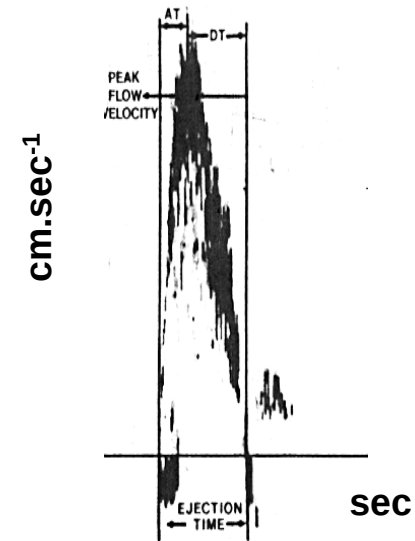


Biais – 0,05%
Limites d'agrément +/- 40%

Les « corrections »: Attention !

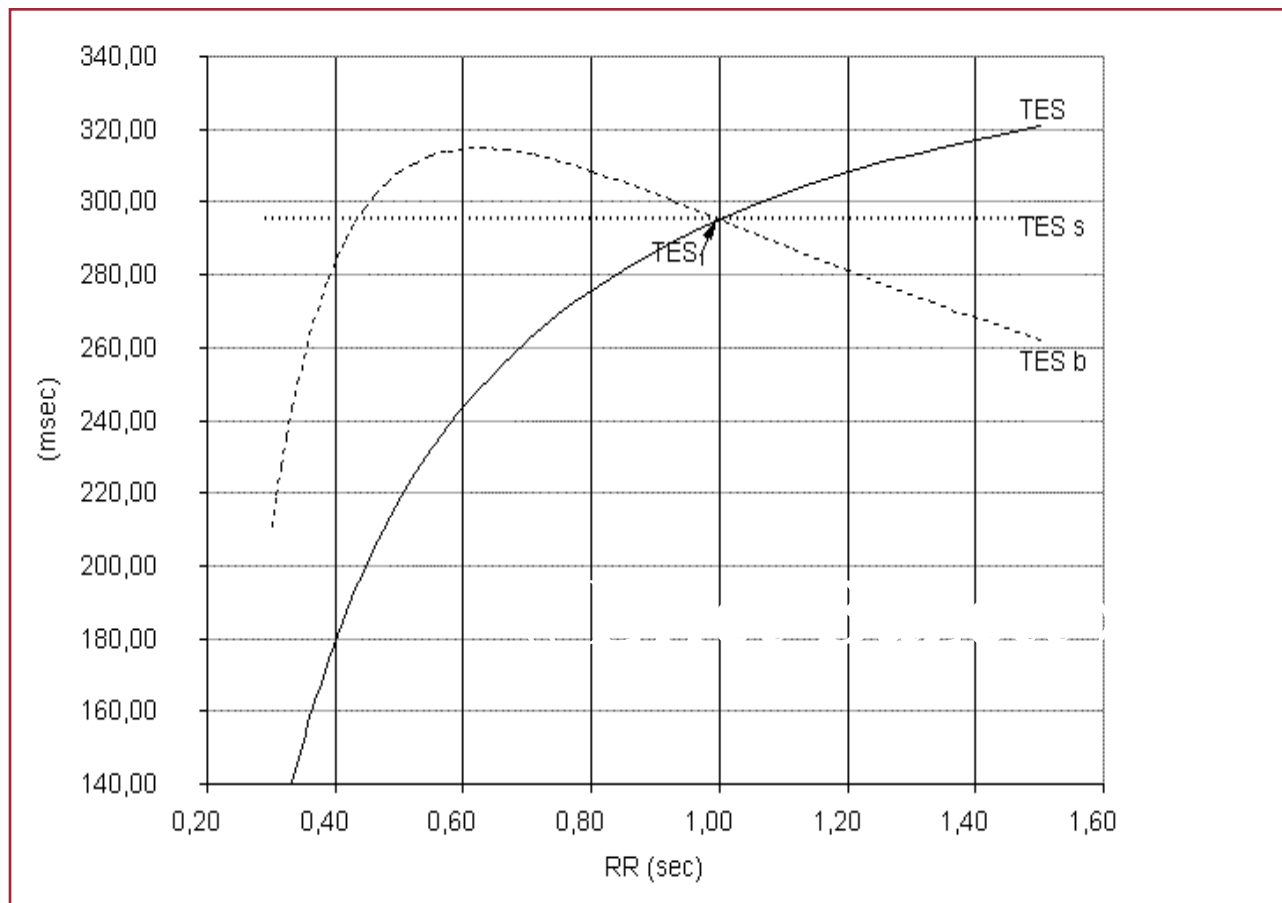


PRECHARGE



$$TES_{\text{corrected}} = \frac{TES}{\sqrt{(RR)}}$$

Singer et al. Crit Care Med 1991



Références

Harris et al. Am J Cardio 1964

Spitaels et al. Circulation 1974

Golde et al. Circulation 1970

Weissler et al. Circulation 1968

Groupes

Enfants

Enfants

Enfants

Adultes

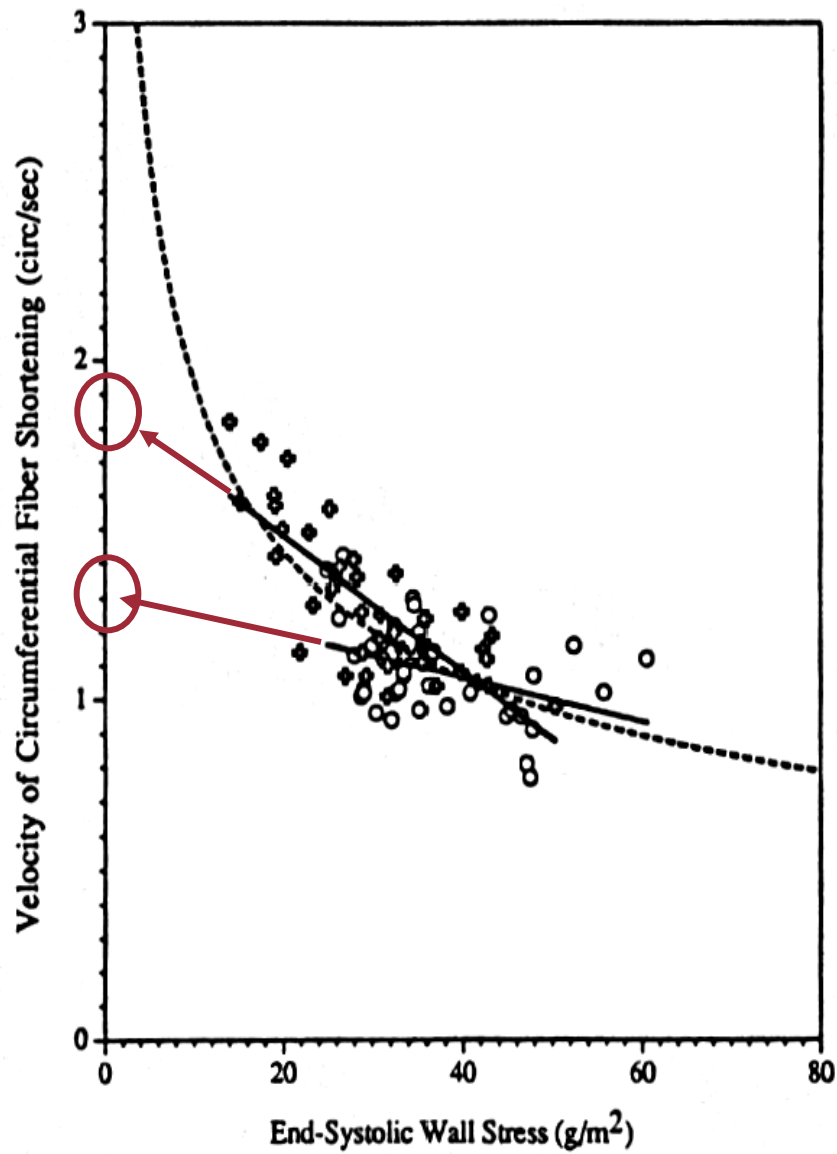
Régression

$$TES = 376 - [Fc.(1,3)]$$

$$TES = 372.7 - [Fc.(1,29)]$$

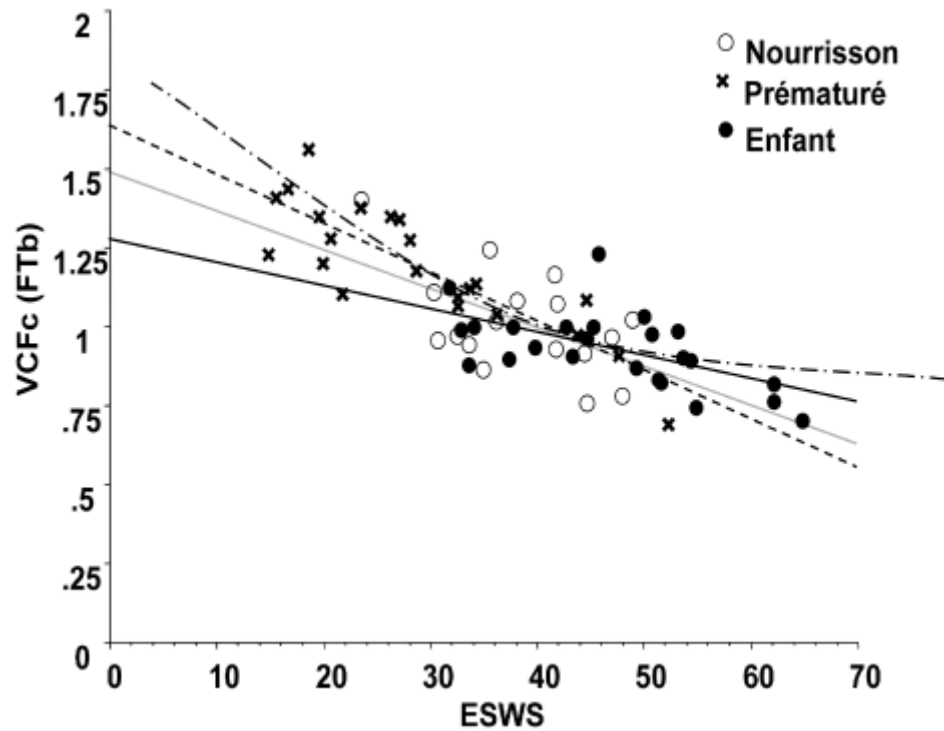
$$TES = 337 + [Mois.(0,35)] - [(Fc).(1,35)]$$

$$TES = 413 - [Fc.(1,7)]$$

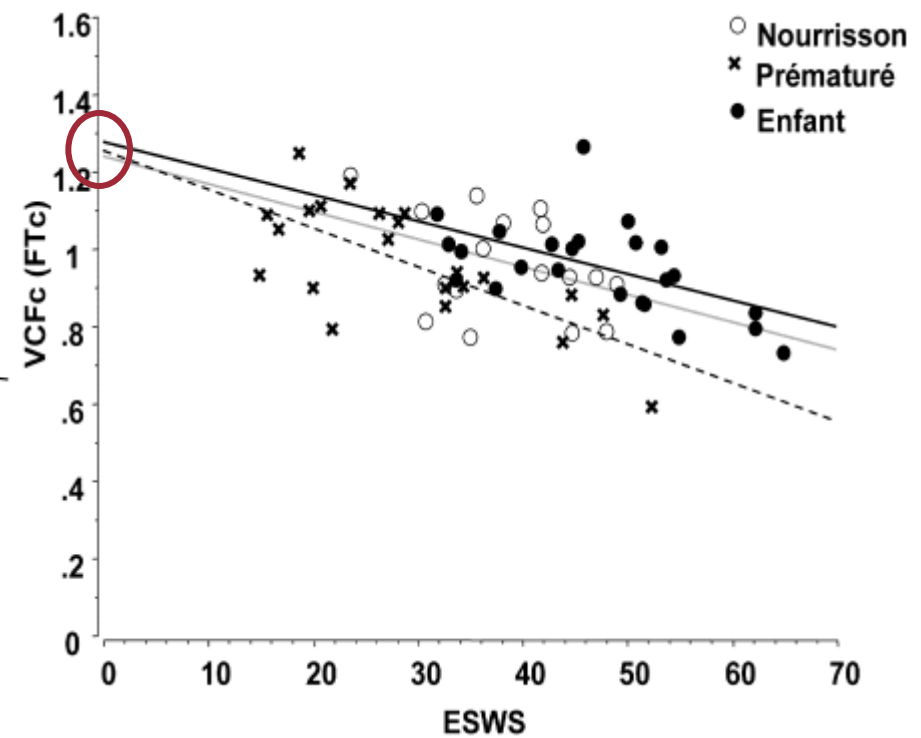


$$VCFc = FR/TES \text{ corrigé}$$

TEScorrigé (Bazett)



TEScorrigé (FC)

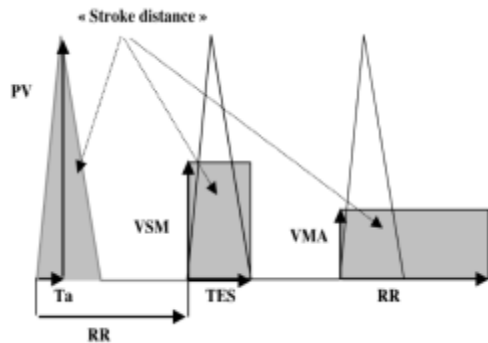


Contractilité ?

« Retomber sur ses pieds » ?

« Dobutamine » et FTcor

	TO	T1	T2	T3	T4	Variation T4-TO
PV	119	120	140	159	184	54,6%
min distance	1364	1408	1587	1718	2032	
HR	56	58	61	62	71	
SV	24,36	24,28	26,02	27,71	28,62	17,5%
RR calculé	1,071	1,034	0,984	0,968	0,845	
FT recalculé	368,43	364,14	334,50	313,69	279,98	
FT cor (calculé)	355,93	358,02	337,27	318,88	304,56	-14,4%
						≠
FT Mesuré	329	329	323	313	296	
FT cor Mesuré	317	324	326	317	321	1,3%
ISVR	572	554	498	487	454	-20,6%

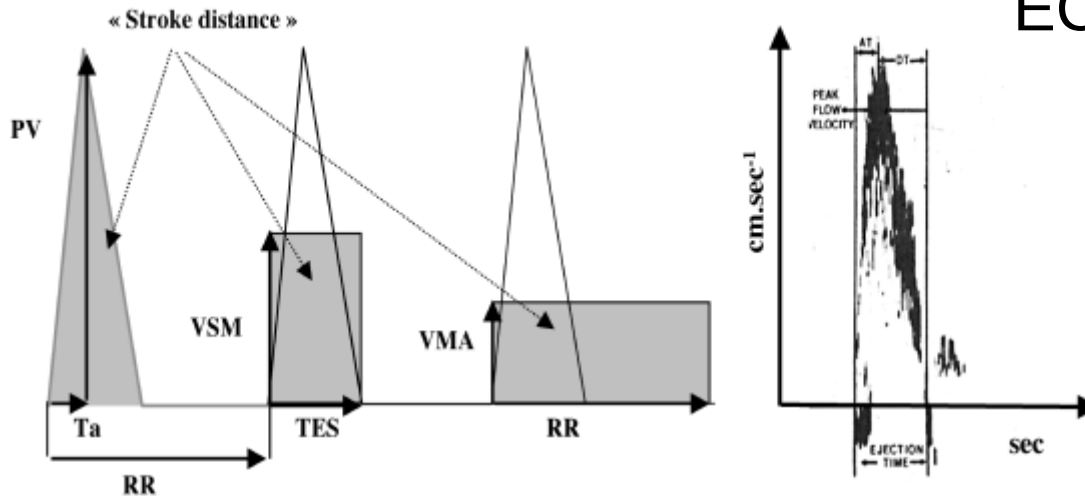


Singer et al. Crit Care Med 1991

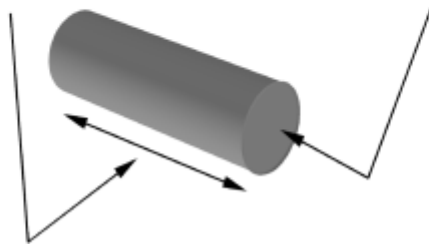
Correspondance des unités !

Echographie Doppler

ECHOGRAPHIE DOPPLER



$$SV \text{ (cm}^3\text{)} = \text{« Stroke distance » (cm)} \times Ao \text{ Area (cm}^2\text{)}$$



Mesure réelle de SV et correspondance des unités

$$VES \text{ (cm}^3\text{)} \times FC \text{ (c/min)} = Q \text{ (cm}^3\text{/min ou ml/min)}$$

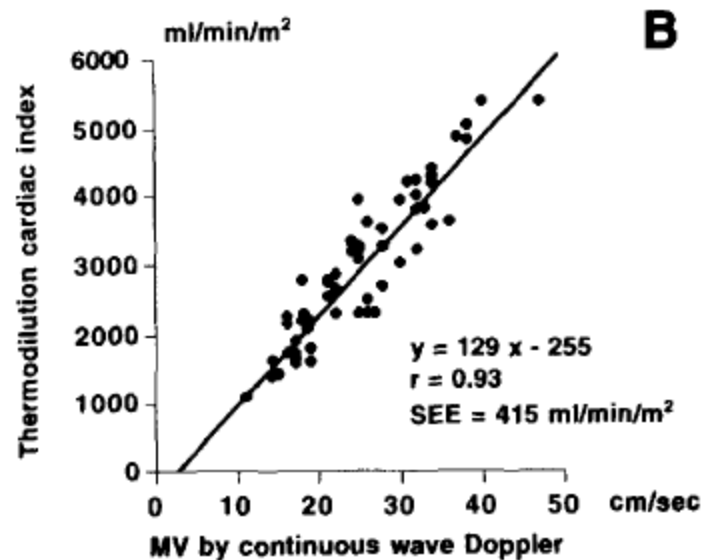
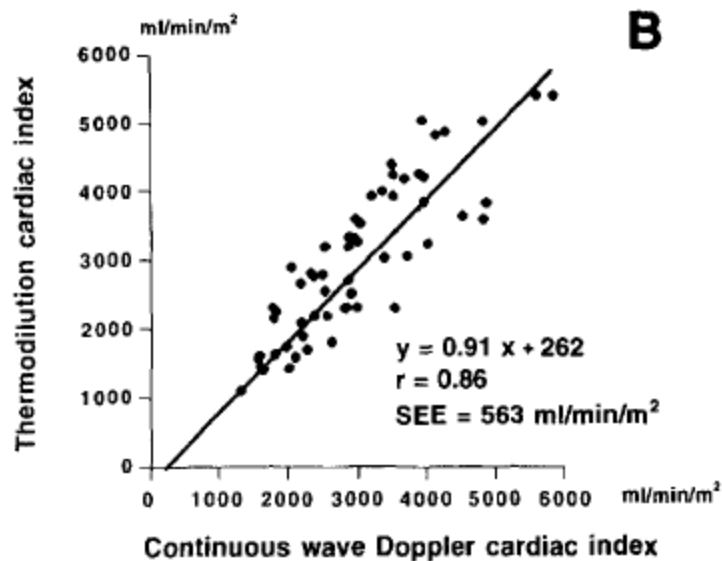
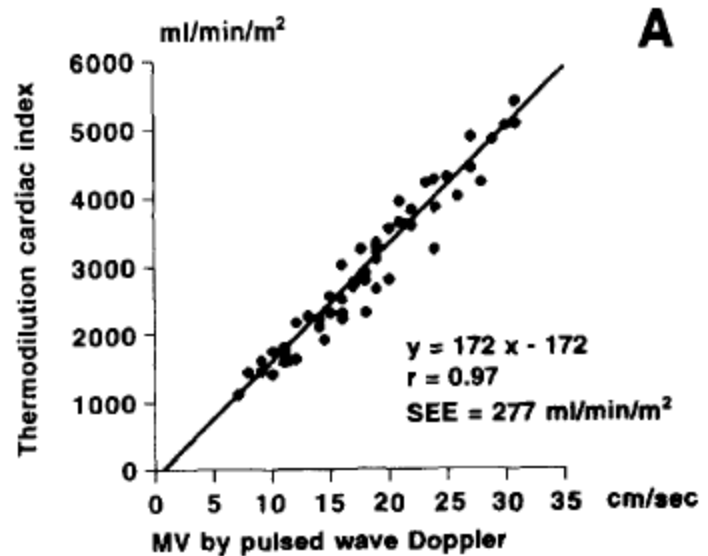
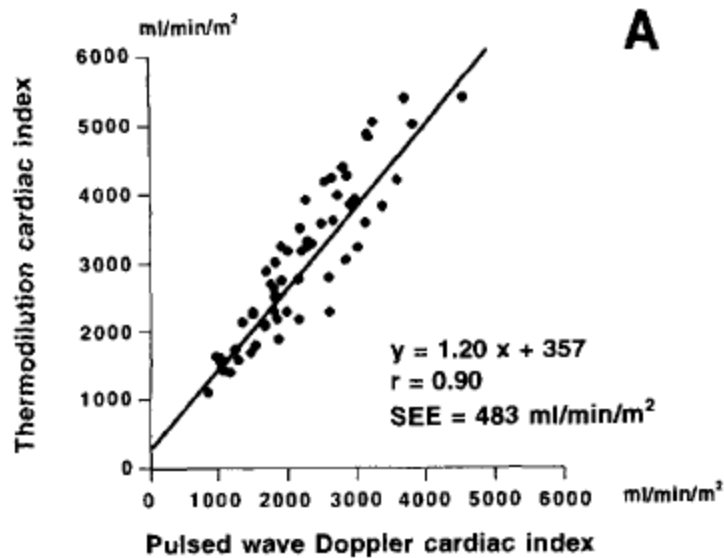
Mesure sur 5 cycles (variations respiratoires)

Cardiac Index Quantification by Doppler Ultrasound in Patients Without Left Ventricular Outflow Tract Abnormalities

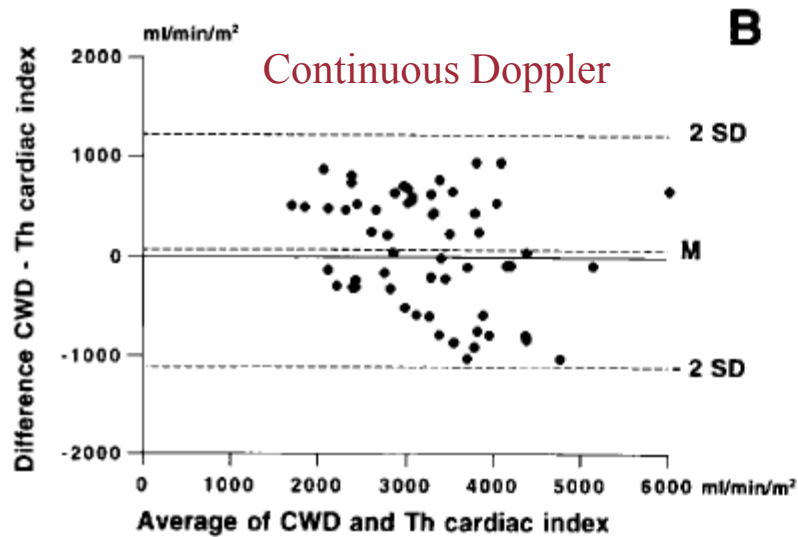
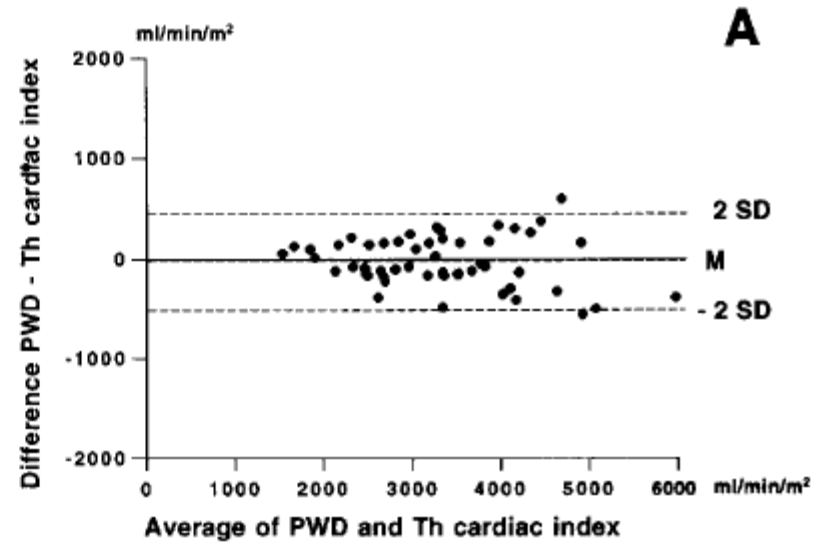
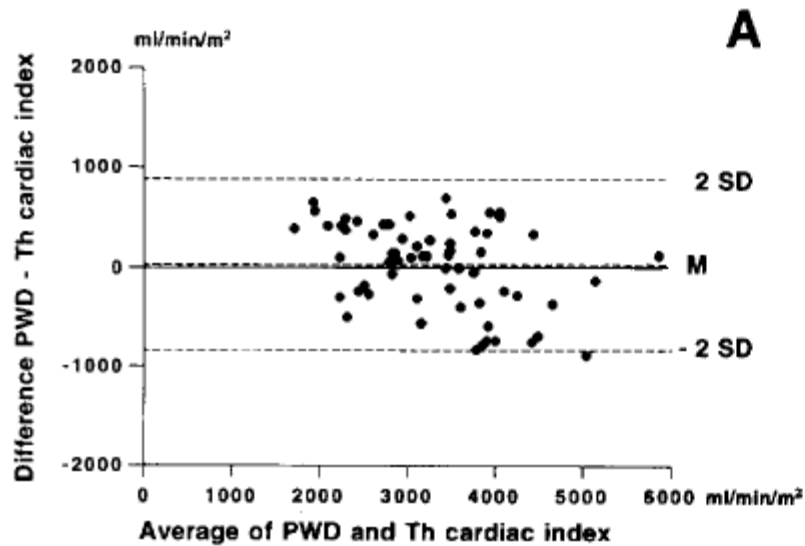
ARTURO EVANGELISTA, MD, DAVID GARCIA-DORADO, MD, FACC,
HERMINIO GARCIA DEL CASTILLO, MD, TERESA GONZALEZ-ALUJAS, MD,
JORDI SOLER-SOLER, MD, FACC

Barcelona, Spain

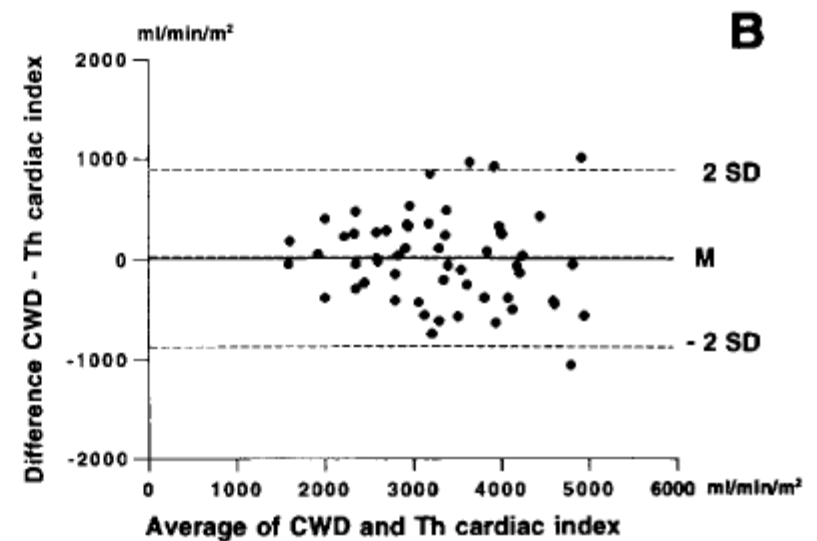
- 156 patients (84 men, 72 women; mean age 37 +/- 20 years, range 6 to 86).
- Patients in the intensive care unit who were undergoing pulmonary artery catheterization
- Absence of left ventricular outflow tract abnormalities



Pulsed Doppler



Continuous Doppler



*Extrapolation of cardiac index from analysis
of the left ventricular outflow velocities
in children: implication of the relationship between
aortic size and body surface area*

ERIC WODEY MD, PhD*, LOTFI SENHADJI PhD†,
FRANÇOIS CARRE MD, PhD‡ AND CLAUDE ECOFFEY MD*

*Department of Anaesthesiology and Surgical Intensive Care, Hôpital Pontchaillou, †LTSI,
INSERM EMI 9934, Université de Rennes and ‡Department of Physiology and Cardiology,
INSERM U127, Hôpital Pontchaillou, Rennes, France

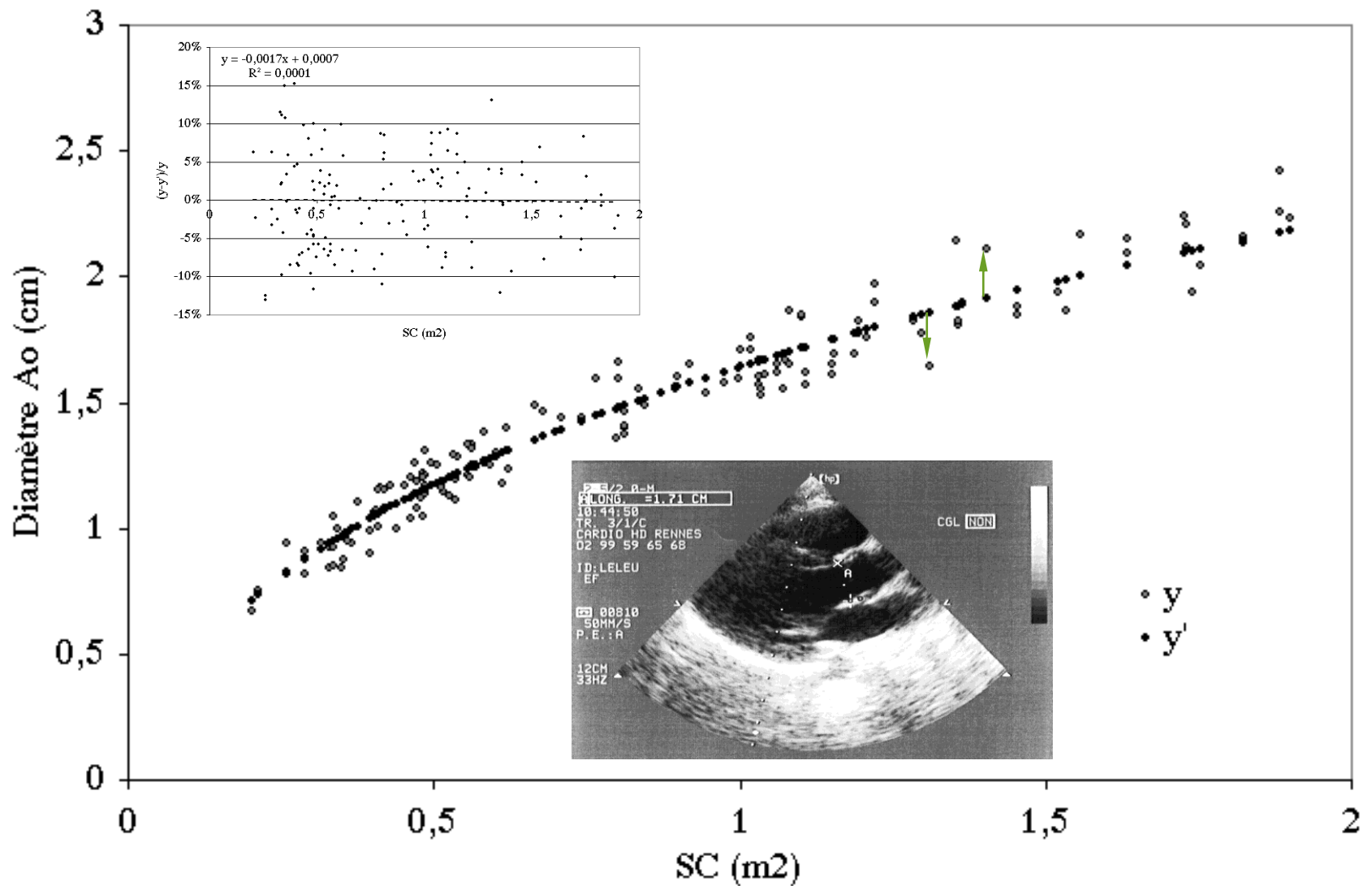
$$(A) \text{ CI (l} \cdot \text{min}^{-1} \cdot \text{m}^{-2}) = 0.129 \times \text{MAVF (cm} \cdot \text{s}^{-1})$$

$$(B) \text{ CI (l} \cdot \text{min}^{-1} \cdot \text{m}^{-2}) = [\text{AA (cm}^2) \times \text{MAVF (cm} \cdot \text{s}^{-1}) \\ \times 60] / 1000 \times \text{BSA (m}^2)$$

$$(C) \text{ AA (cm}^2) = 2.15 \times \text{BSA (m}^2)$$

$$(D) \text{ CI (l min}^{-1} \cdot \text{m}^{-2}) = ([\pi \times \varnothing \text{Ao (cm)} / 4] \\ \times \text{MAVF (cm} \cdot \text{s}^{-1}) \times 60) / 1000 \\ \times \text{BSA (m}^2)$$

$$(E) \varnothing \text{Ao} = 1.65 \times \sqrt{\text{BSA}}$$



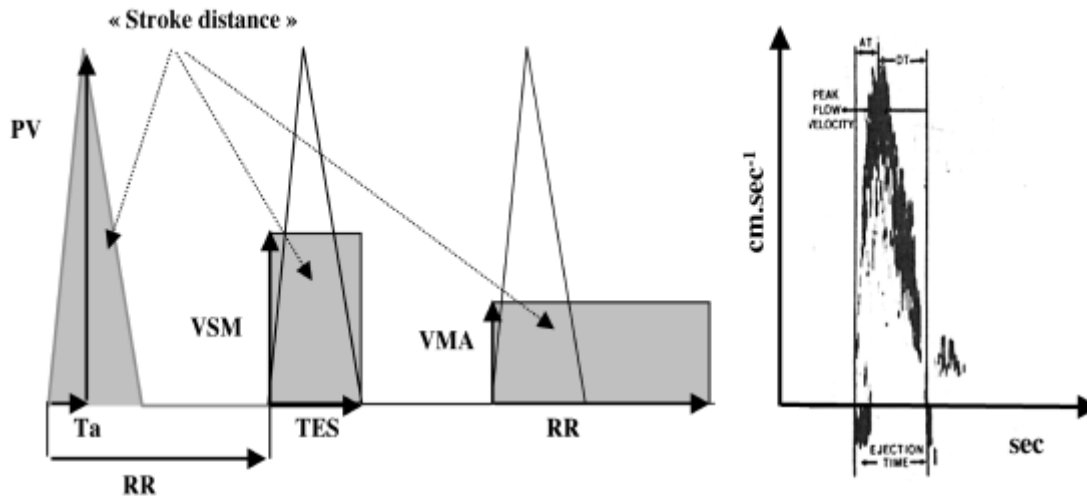
126 enfants et NN (Age 3 jours à 18 ans).

Table 2
Relationship between aortic size and BSA obtained with nonlinear regression method

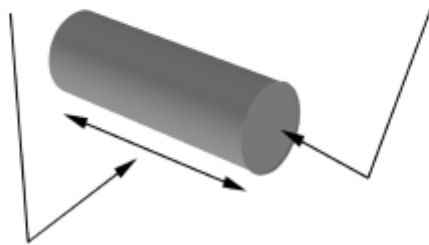
	<i>Model</i>	<i>a</i>	<i>b</i>	<i>c</i>	<i>y - y'/y</i>	<i>SD</i>	<i>P</i>	<i>r</i>
ØAo								
1	$y = a(x^{1/4}) + b$	2.969	-1.315	-	3.29E-03	6.11E-02	0.999	0.974
2	$y = a(x^{1/3}) + b$	2.280	-0.632	-	3.73E-03	6.11E-02	1	0.974
3	$y = a(x^c) + b$	2.208	-0.561	0.345	3.80E-03	6.11E-02	1	0.974
4	$y = a(x^{1/2}) + b$	1.583	0.0519	-	-4.79E-03	6.37E-02	0.999	0.973
5	$y = a(x) + b$	0.84	0.738	-	9.07E-03	8.55E-0.2	0.81	0.962
6	$y = a(x^{1/2})$	1.639	-	-	-5.63E-04	6.27E-02	0.999	0.973
7	$y = a(x^c)$	1.636	-	0.479	5.26E-03	6.34E-02	0.998	0.974
8	$y = a(x^{1/3})$	1.594	-	-	4.12E-0.2	1.12E-01	0.848	0.974
AA								
9	$y = a(x)$	2.093	-	-	4.25E-03	1.25E-01	0.987	0.970
10	$y = a(x^c) + b$	2.228	-0.109	0.894	-1.70E-02	1.26E-01	0.952	0.970
11	$y = a(x) + b$	2.01	0.007	-	-2.19E-02	1.34E-0.1	0.898	0.970
ØAo_{index}								
12	$y = a(x^c) + b$	3.165	-1.508	-0.286	3.62E-03	6.16E-02	0.991	0.970
13	$y = a(x^c)$	1.654	-	-0.492	6.5E-03	6.34E-02	0.861	0.968
AA_{index}								
14	$y = a(x) + b$	-0.082	2.199	-	-1.55E-02	1.27E-01	0.991	0.131
15	$y = a(x^c) + b$	-0.042	2.169	2.12	1.54E-02	1.26E-01	0.998	0.146

$$(E) \text{ } \varnothing \text{Ao} = 1.65 \times \sqrt{\text{BSA}}$$

$$(C) \text{ AA (cm}^2\text{)} = 2.15 \times \text{BSA (m}^2\text{)}$$



$$SV [cm^3] = \text{« Stroke distance » (cm)} \times Ao \text{ Area } [cm^2]$$



$$SVI (cm^3.m^2) = \text{Stroke distance (cm)} \times Ao \text{ Area Index } (cm^3/m^2)$$

• $MAV(cm.sec^{-1}) \Rightarrow CI$

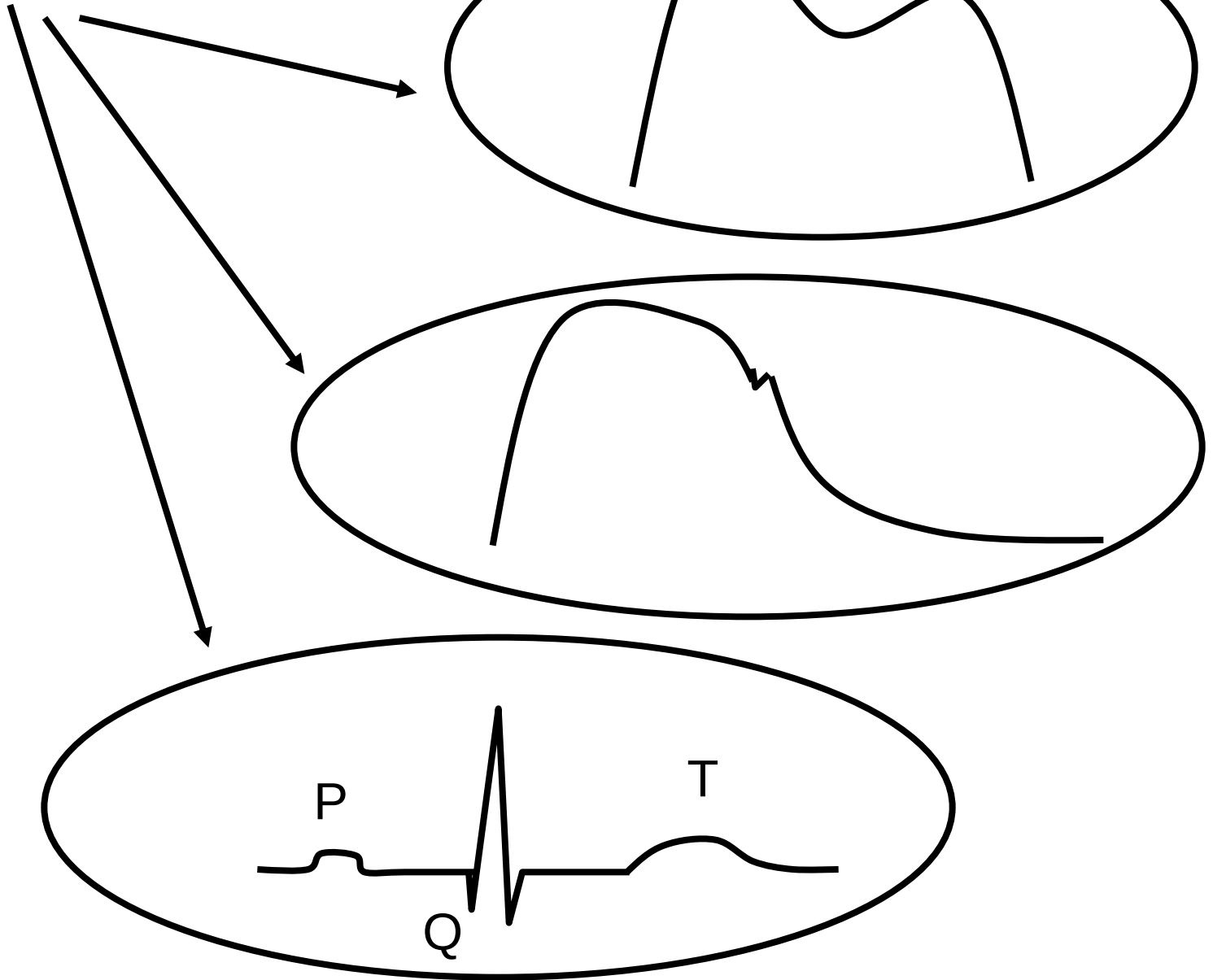
« Estimation en sortie de VG »

• $\text{Stroke D(cm)} \Rightarrow SVI$

Origine du signal mesuré ?

Formes des courbes:
exemple type

Formes Spécifiques



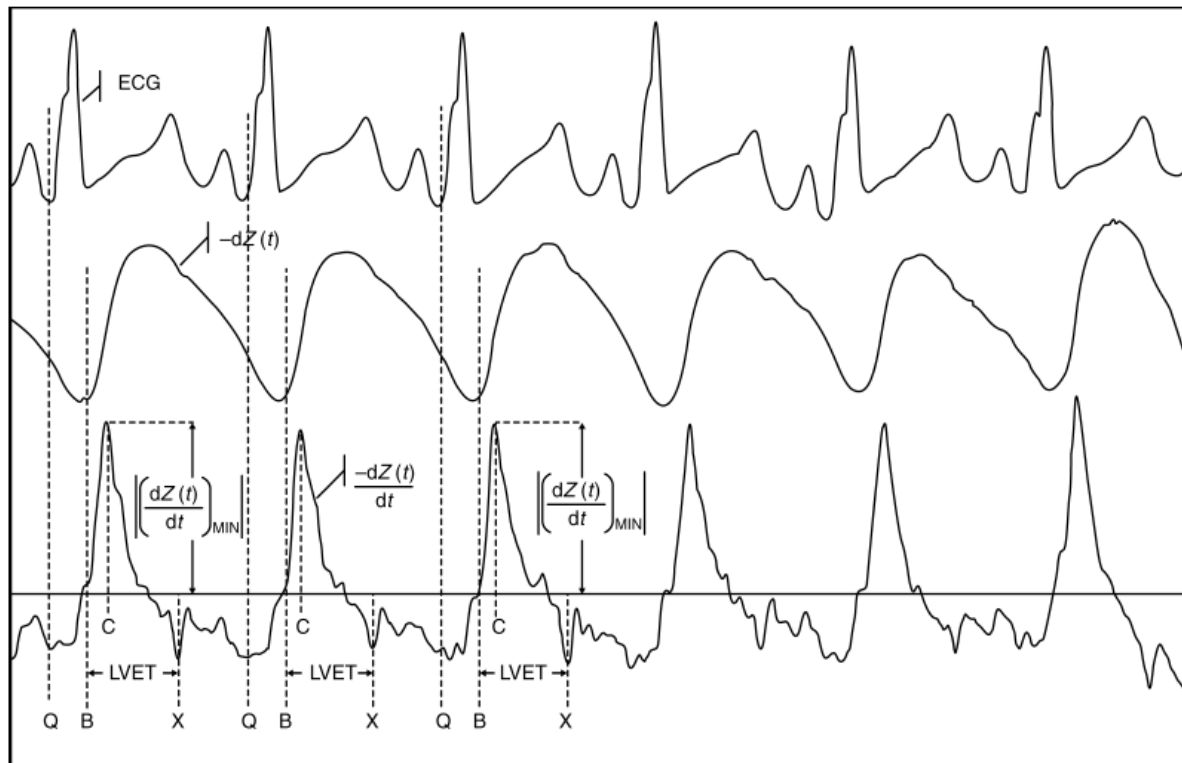
Impédancemétrie Thoracique

- Kubicek WG et al. Aerospace Med 1966
- Wong DH et al. Anesthesiology 1990
- Woltjer HH et al. Eur Heart J 1997
- American Heart Association Congress 1999
« Acte Remboursé »



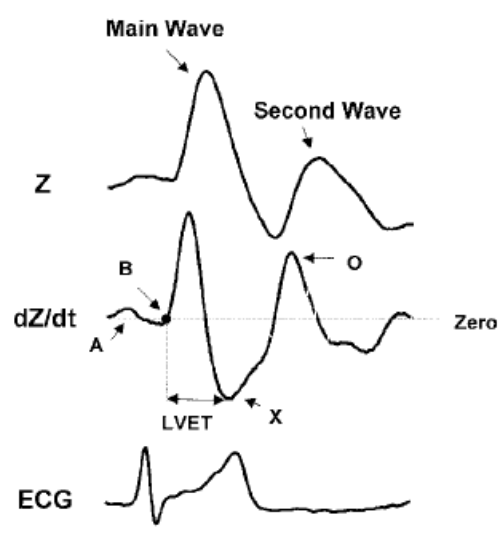
Electrical velocimetry for measuring cardiac output in children with congenital heart disease

K. Norozi^{1*}†, C. Beck¹†, W. A. Osthaus², I. Wille¹, A. Wessel¹ and H. Bertram¹



Impedance cardiographic waveforms in children: Involvement in left ventricular ejection time determination during anesthesia

Eric Wodey, MD, PhD; Lotfi Senhadji, PhD; Jean Yves Bansard, PhD; Xavier Beneux, MD; Claude Ecoffey, MD; François Carre, MD, PhD

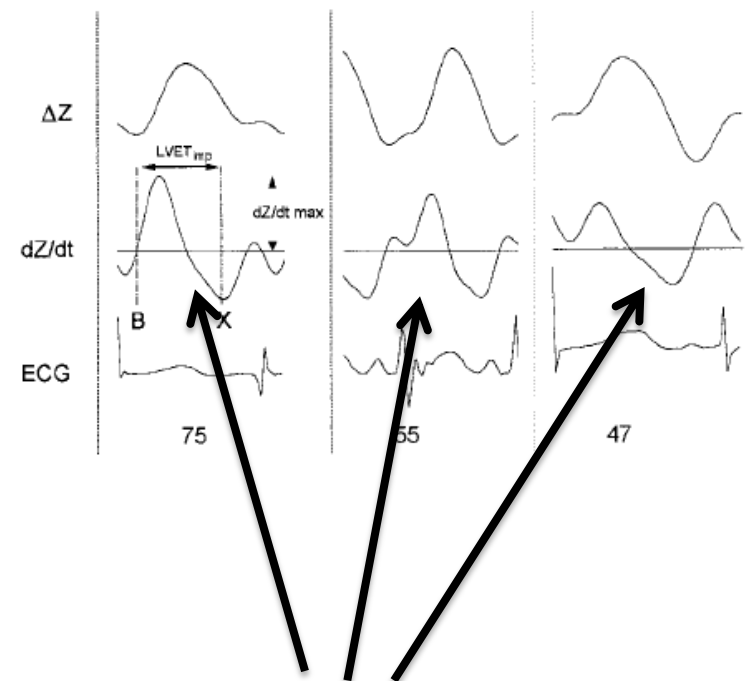
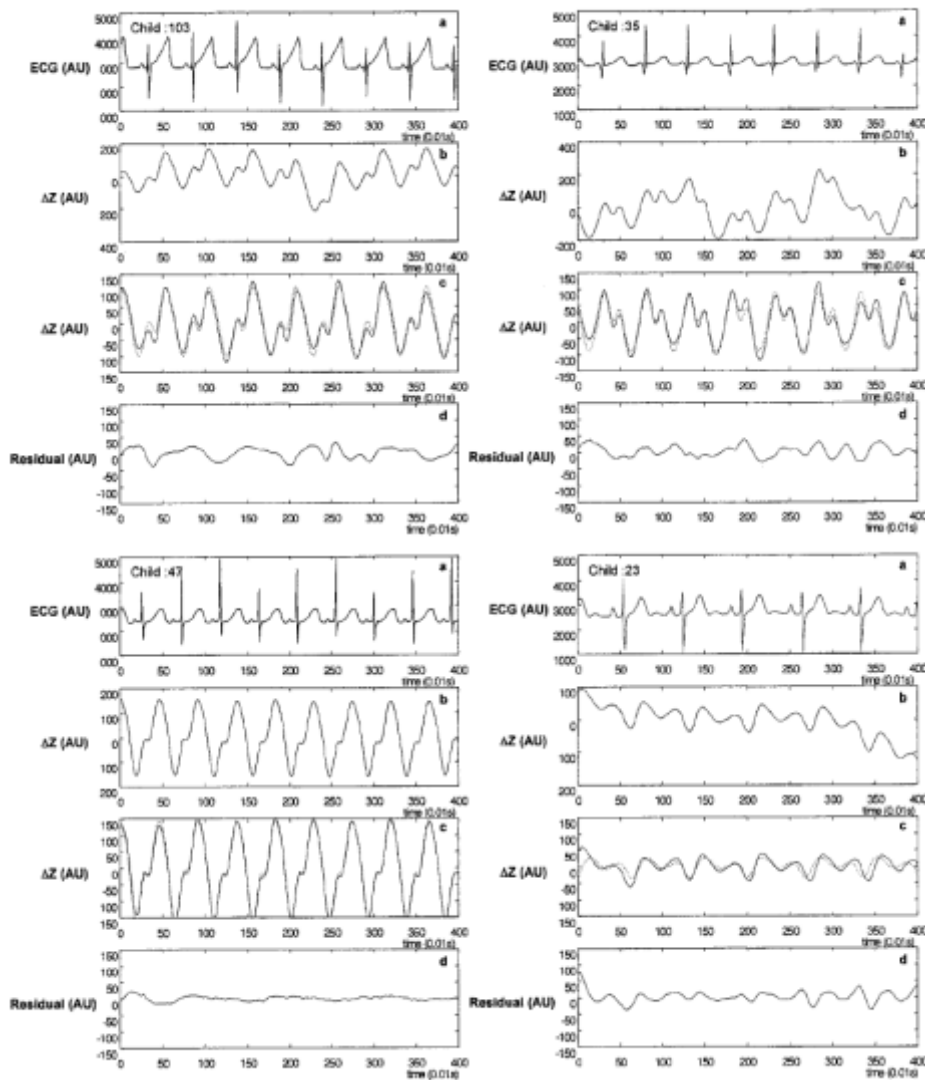


$$SV = \delta \cdot \frac{(0.17 \cdot H)^3}{4.25} \cdot \frac{dZ/dt_{\max}}{Z_0} \cdot \boxed{LVET}$$

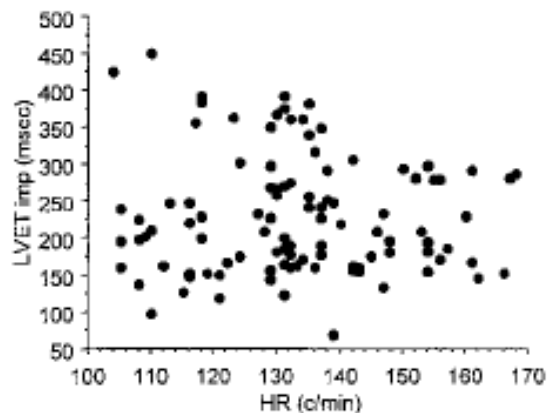
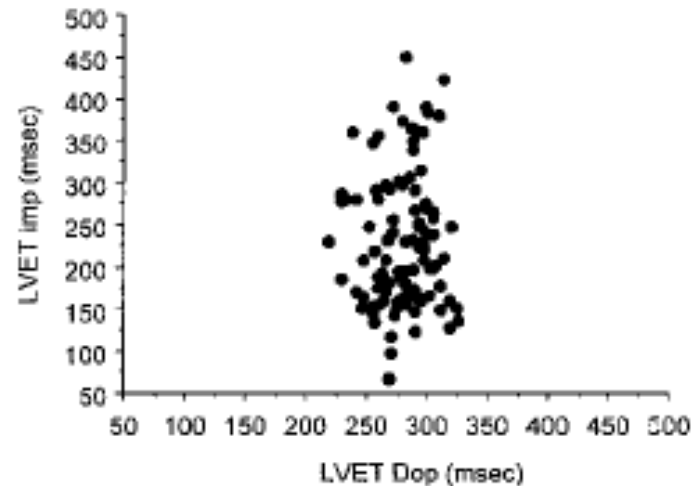
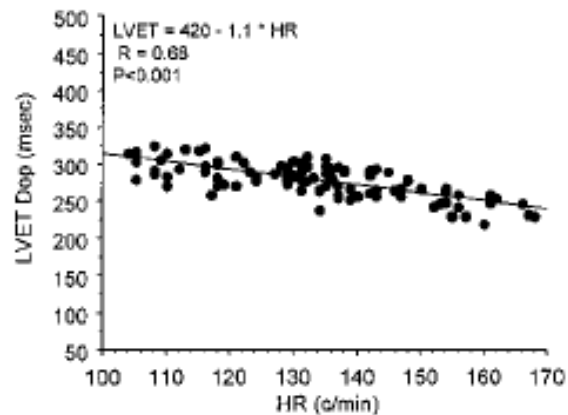
- 103 children of ASA physical status I or II who required general anesthesia for elective surgery.

- Children did not have cardiovascular disease

$$SV = \rho \cdot \frac{L^2}{Z_0^2} \cdot dZ/dt_{\max} \cdot \boxed{LVET}$$



Formes variables



Impedance cardiography appears inadequate to always accurately determine LVET, which is needed for SV calculation during general anesthesia in children and infants.

$$SV = \delta \frac{(0.17 \cdot H)^3}{4.25} \cdot \frac{dZ/dt_{\max}}{Z_0} \cdot LVET$$

$$SV = \boxed{BSA} \times \textcircled{SVi}$$

$$SV = \rho \cdot \frac{\boxed{L^2}}{Z_0^2} \cdot dZ/dt_{\max} \cdot LVET$$

Unité ?

Méthodes (in English)

Invasive

- Dilution techniques
- Dye dilution
- Pulmonary artery thermodilution
- Transpulmonary thermodilution
- Lithium dilution
- Direct Fick

Non-invasive

- Non-invasive Fick using CO₂
- Bioimpedance
- Echocardiography
- Trans-oesophageal doppler
- Pulse contour analysis
- Nicom (Bioréactance)

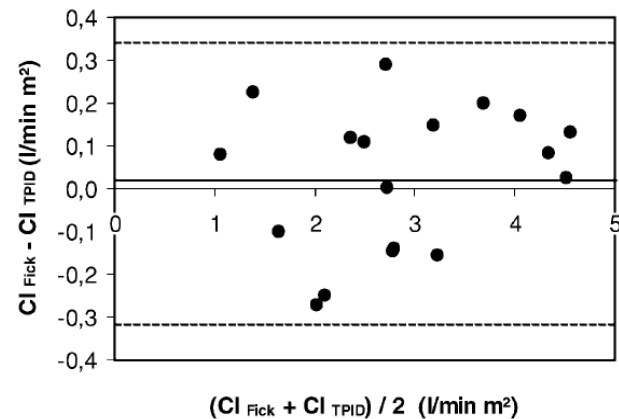
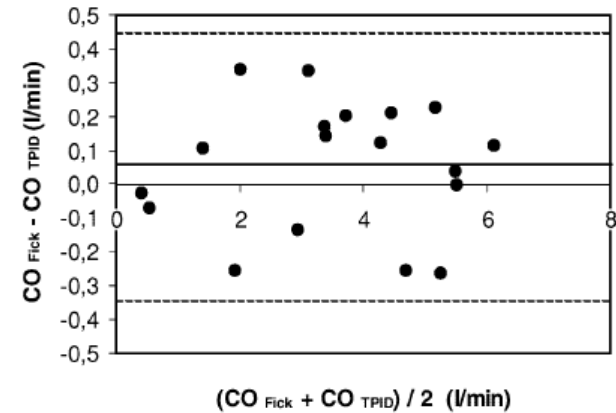
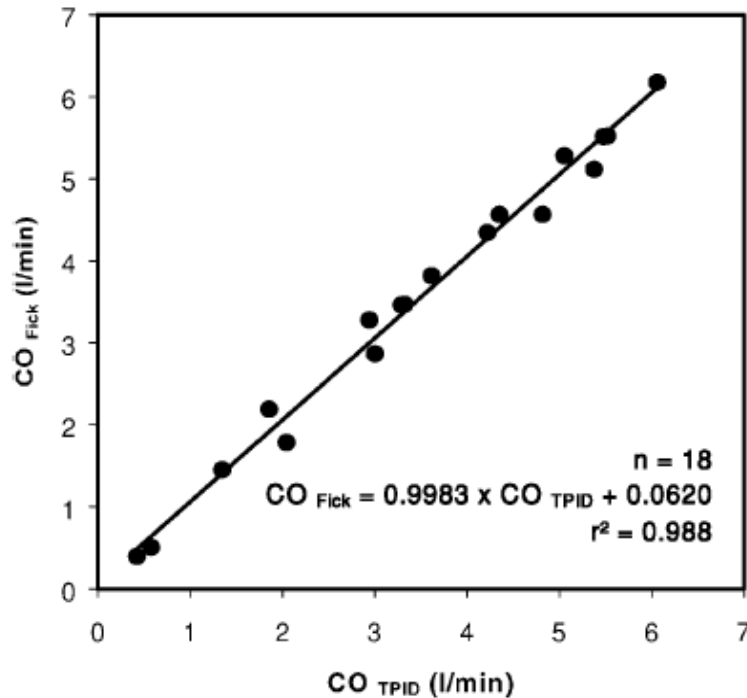
C. Pauli
U. Fakler
T. Genz
M. Hennig
H.-P. Lorenz
J. Hess

**Cardiac output determination in children:
equivalence of the transpulmonary
thermodilution method to the direct
Fick principle**

- Prospective study.
- 18 patients (mean age 12.1 ± 6.4 years) during cardiac catheterisation and after corrective cardiac operation
- No shunt
- Control: Determination of CI by Fick as the clinical “gold standard”

C. Pauli
U. Fakler
T. Genz
M. Hennig
H.-P. Lorenz
J. Hess

Cardiac output determination in children: equivalence of the transpulmonary thermodilution method to the direct Fick principle



Like a dream !

Intensive Care Med (2002) 28:947–952

C. Pauli
U. Fakler
T. Genz
M. Hennig
H.-P. Lorenz
J. Hess

Cardiac output determination in children: equivalence of the transpulmonary thermodilution method to the direct Fick principle

Patient number	Condition	Weight (kg)	CI _{Fick} (l/min·m ²)	CI _{TPID} (l/min·m ²)	CI _{Fick} -CI _{TPID} (l/min·m ²)	Diagnosis
5	Postop	4.3	1.59	1.69	-0.10	Truncus arteriosus repair
10	Cath lab	4.7	1.98	2.23	-0.25	CAVSD repair, severe MI
3	Postop	20.8	4.13	3.96	0.17	ASD repair
11	Cath lab	23.0	3.15	3.30	-0.15	IAA repair, LVOTO
13	Cath lab	25.9	1.88	2.15	-0.27	PS, dilatation of PV
22	Postop	26.6	4.62	4.49	0.13	CoA
18	Postop	27.8	3.78	3.58	0.20	VSD, RVOTO repair
1	Postop	35.0	4.52	4.49	0.03	AS 2°, AI 4°, AVR
7	Cath lab	35.2	2.85	2.56	0.29	TGA, Senning
14	Cath lab	37.3	1.10	1.02	0.08	Hypertrophic CMP
20	Postop	42.0	3.26	3.11	0.15	VSD, AI 4°, repair
2	Cath lab	43.0	2.42	2.30	0.12	Tricuspid atresia, Fontan
19	Postop	48.0	4.38	4.30	0.08	MI 3°
4	Cath lab	49.7	1.49	1.26	0.23	Tricuspid atresia, Fontan
12	Cath lab	53.0	2.70	2.85	-0.15	CCTGA, p.H.
26	Cath lab	70.6	2.72	2.86	-0.14	DORV, RVOTO, Fontan
25	Cath lab	78.0	2.72	2.72	0.00	TGA, LVOTO, Mustard
17	Cath lab	88.0	2.55	2.44	0.11	TGA, Senning

Median of Weight: 35 kg: “Old children”

Steady state

Intensive Care Med (2002) 28:947–952

Pulse Contour Analysis for Cardiac Output Monitoring in Cardiac Surgery for Congenital Heart Disease

Aman Mahajan, MD, Afshin Shabanie, MD, Judi Turner, MD, PhD, Michael J. Sopher, MD, and Jure Marijic, MD

- Prospective study.
- 16 patients undergoing corrective operations for congenital heart disease (median age 7 years)

Pulse Contour Analysis for Cardiac Output Monitoring in Cardiac Surgery for Congenital Heart Disease

Aman Mahajan, MD, Afshin Shabanie, MD, Judi Turner, MD, PhD, Michael J. Sopher, MD, and Jure Marijic, MD

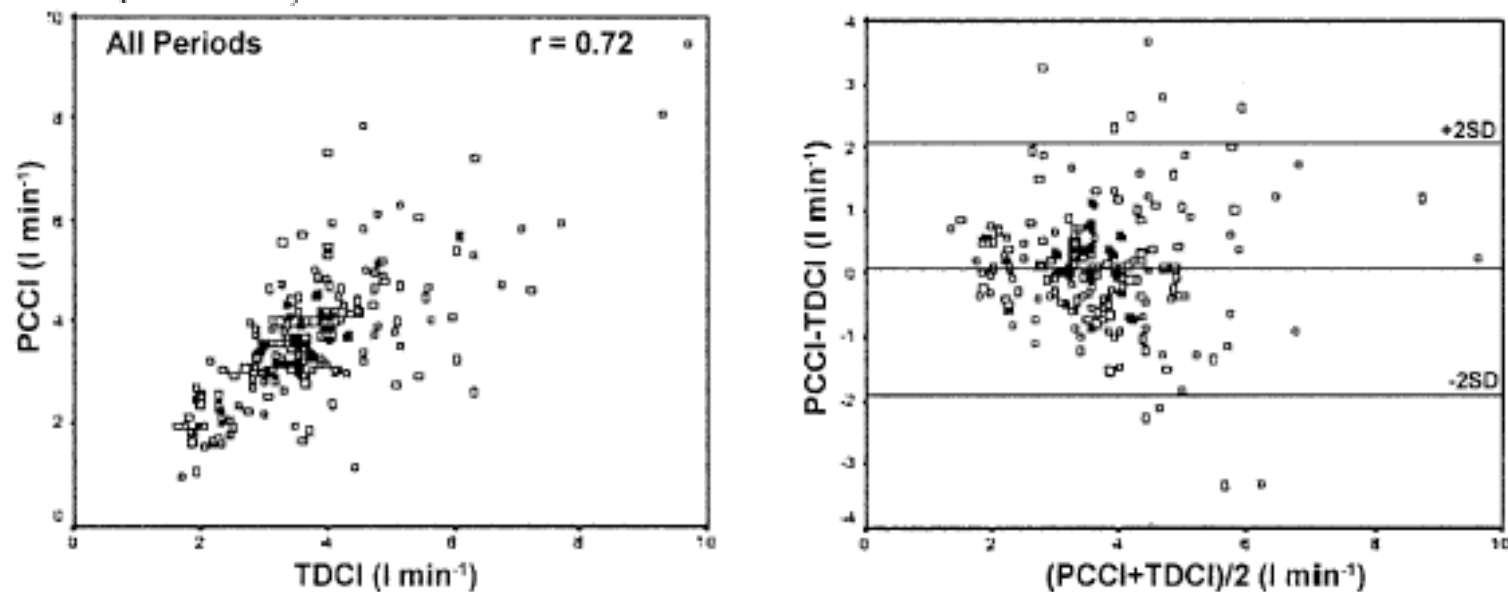


Figure 1. Top panels) Pre-cardiopulmonary bypass (CPB) period. (Middle panels) Post-CPB and intensive care unit (ICU). (Lower panels) All periods linear correlation (left) and mean difference between pulse contour analysis (PCCI) and transpulmonary thermodilution (TDCI) using Bland-Altman analysis (right). Each point represents the mean of three consecutive measures of TDCI and the respective PCCI_{lag} values. The right panels represent the bias between the two different techniques of cardiac output monitoring.

• CI « index » < ? > l.min⁻¹

Anesth Analg 2003;97:1283–8

Pulse Contour Analysis for Cardiac Output Monitoring in Cardiac Surgery for Congenital Heart Disease

Aman Mahajan, MD, Afshin Shabanian, MD, Judi Turner, MD, PhD, Michael J. Sopher, MD, and Jure Marijic, MD

Table 1. Accuracy of Pulse Contours analysis (PCCI) Compared with Transpulmonary Thermodilution (TDCl) During Different Time Periods of Congenital Cardiac Surgery

Group	Patient group/time period	mean bias $\pm$ SD	<i>r</i>	<i>n</i>
1	OR, before bypass (pre-CPB)	-0.13 ± 0.93	0.61	61
2	OR, after bypass (post-CPB)	0.05 ± 0.94	0.72	69
3	ICU	0.24 ± 1.04	0.73	61
4	<u>All data after correction (post-CPB + ICU)</u>	0.08 ± 0.99	0.73	130
5	All patients, all periods	0.10 ± 0.97	0.72	191

r = Pearson's correlation coefficient; Mean bias = (TDCl-PCCI); OR = operating room; ICU = intensive care unit; CPB = cardiopulmonary bypass.

- DS à 0,97 (Limites d'agrément – 1,84 to 2,04 L.min¹.m²)
- soit 50 à 100% d'erreur

Mauvais $r = 0.7$
Correspond à $r^2 = 0.49$

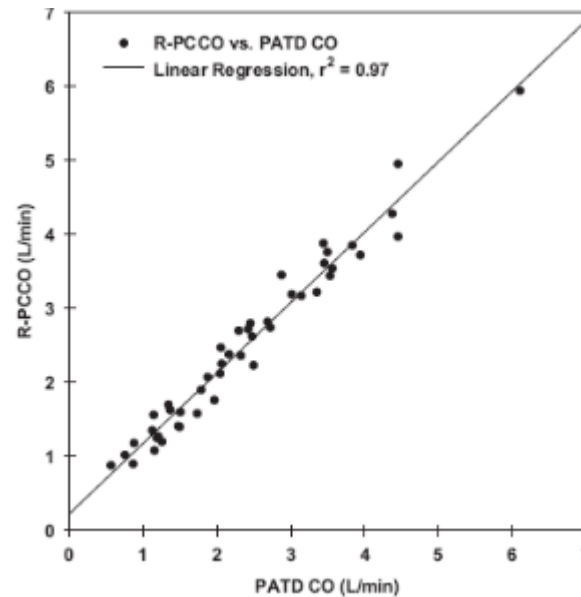
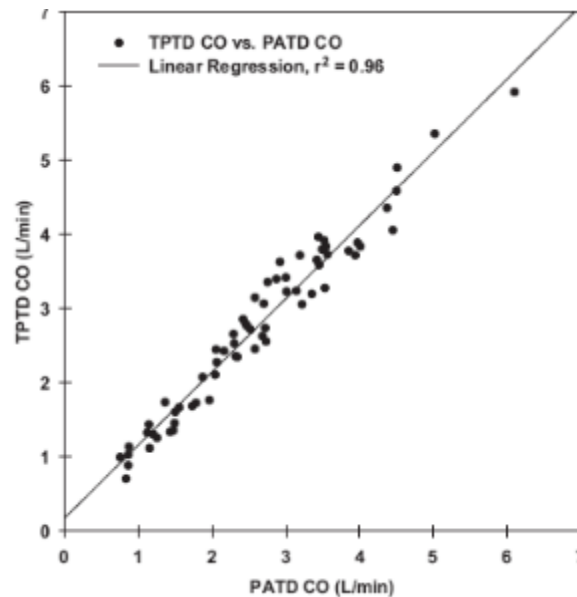
conclusion :

...range as wide as that obtained in our series can limit the clinical utility of the monitor because most anesthesiologists will treat a CI of 1.0 differently from a CI of 3.0 ...

Anesth Analg 2003;97:1283–8

Pulse contour cardiac output analysis in a piglet model of severe hemorrhagic shock*

Mark D. Piehl, MD, MPH; James E. Manning, MD; Shane L. McCurdy, BS; Tim S. Rhue, MA;
Keith C. Kocis, MD, MS, FCCM; Charles B. Cairns, MD; Bruce A. Cairns, MD



“...this study demonstrates that PCCO analysis, when recalibrated by TPTD CO during major hemorrhage and acute changes in MAP, correlates extremely well with PATD CO in a piglet model of hemorrhagic shock”.

“In the setting of large (20%) changes in blood pressure and intravascular volume, PCCO readings can be markedly inaccurate if not recalibrated...”

Recalibration = Bon

Delais = Pas Bon



Question : Quels délais ?

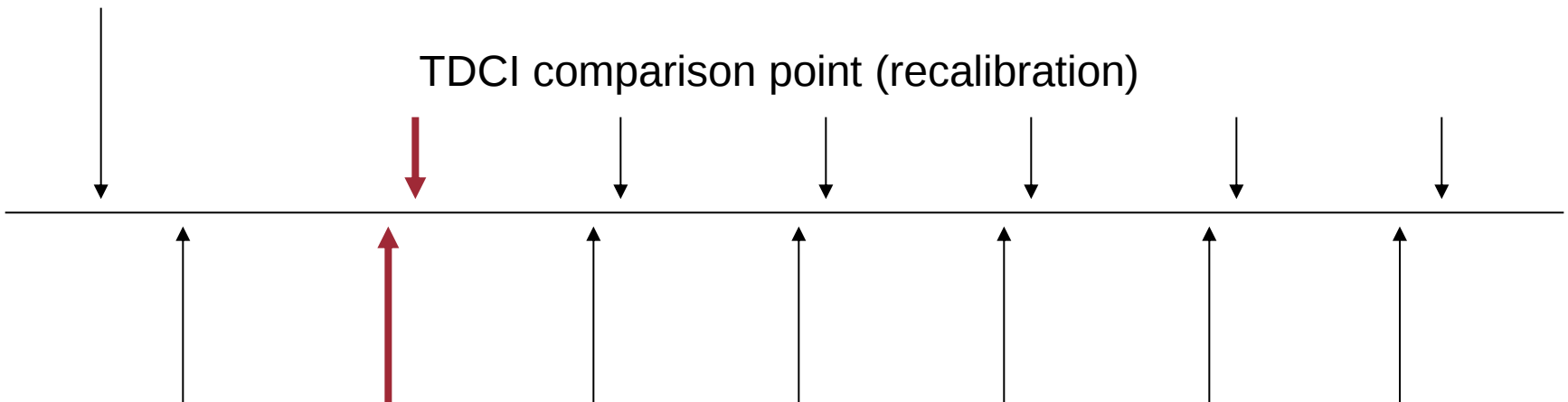
Cardiac index monitoring by pulse contour analysis and thermodilution after pediatric cardiac surgery

U. Fakler, MD,^a Ch. Pauli, MD,^a G. Balling, MD,^a H. P. Lorenz, MD,^a A. Eicken, MD,^a M. Hennig, Dr,^b and J. Hess, MD^a

- Prospective study.
- 24 patients undergoing corrective operations for congenital heart disease (median age 4.2 years)
- Patients with intracardiac shunts were excluded by transesophageal or transthoracic echocardiography.

- Central venous line in the jugular vein
- 3F catheter with a thermistor at the tip (PiCCO system) in the femoral artery

Initial calibration Transpulmonary thermodilution (TDCI)



PCCI: cardiac index derived from pulse contour analysis (just before recalibration with TDCI and self-calibrating)

1 - 4 - 8 - 12 -16 - 20 – 24H

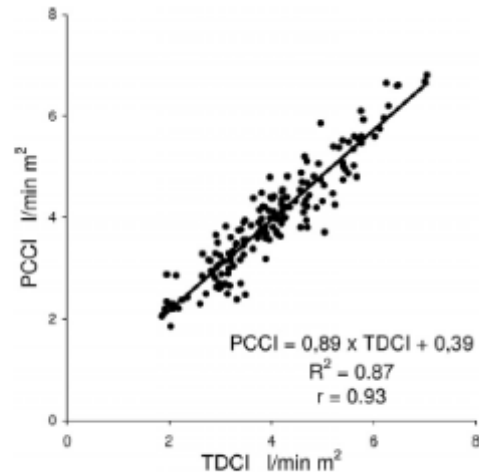


Figure 1. Comparative plot showing the correlation of TDCI and PCCI.

- Meilleurs limites d'agrément
- Meilleur corrélation

Do not validate the accuracy of the PiCCO method... (vs independent method)

But validate the delay of 4 H to give similar information to TPTD

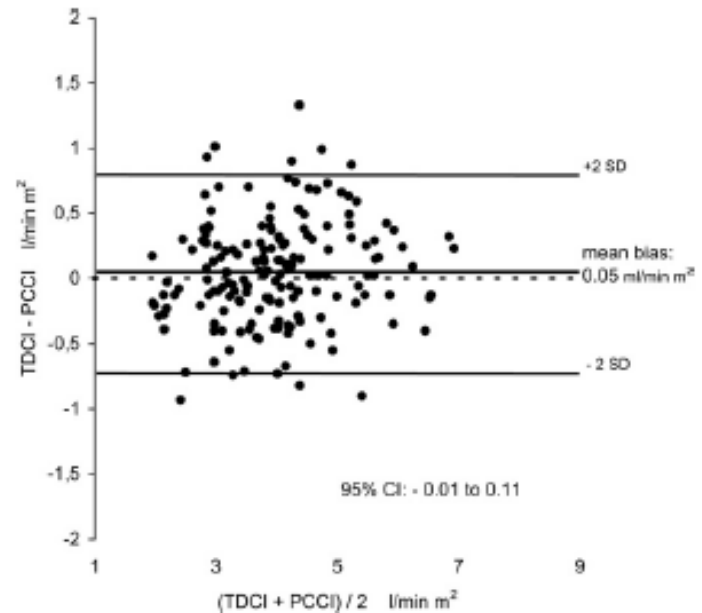


Figure 2. Bland-Altman plot showing the comparison of TDCI and PCCI, expressed by mean bias and limits of agreement and 95% confidence interval (CI). SD, Standard deviation.

Cardiac Output Measurement in Patients Undergoing Liver Transplantation: Pulmonary Artery Catheter Versus Uncalibrated Arterial Pressure Waveform Analysis

« Pulse contour » seul

Biais Matthieu, MD

Nouette-Gaulain Karine, MD, PhD

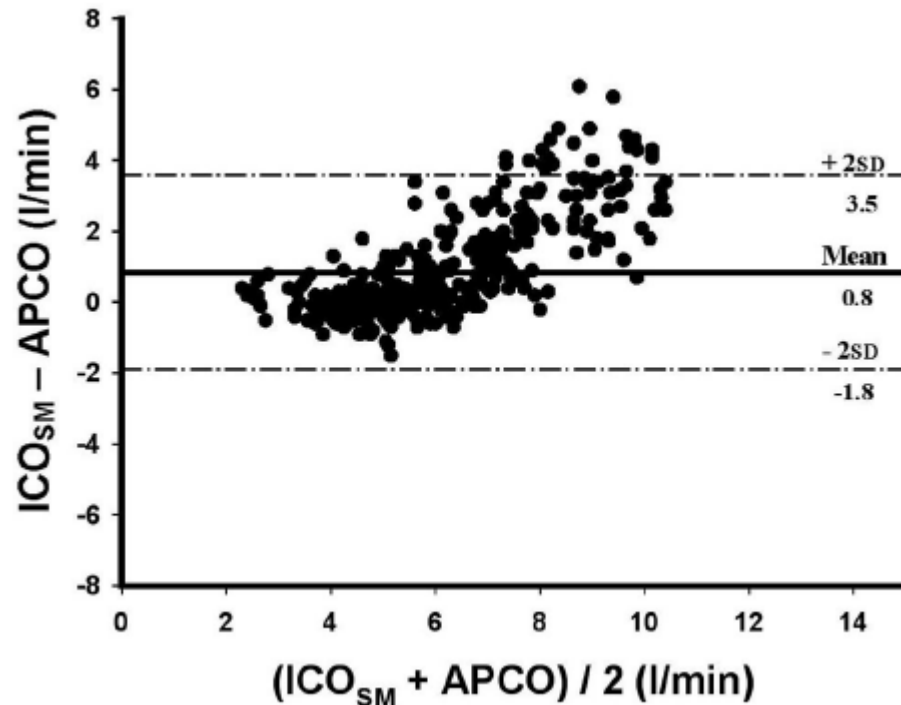
Cottenceau Vincent, MD

Vallet Alain, MD

Cochard Jean François, MD

Revel Philippe, MD

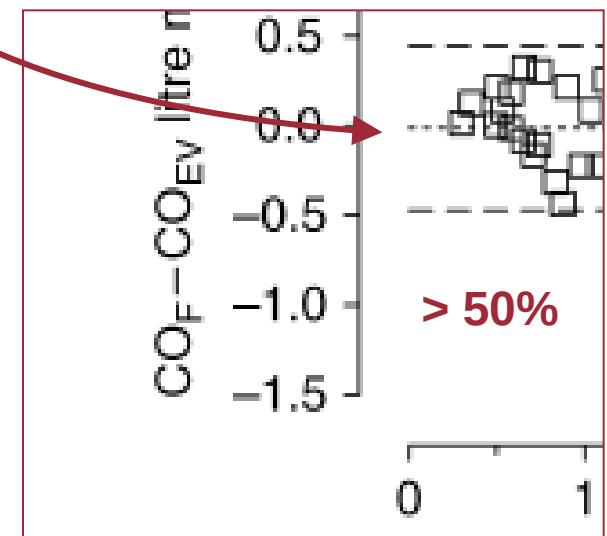
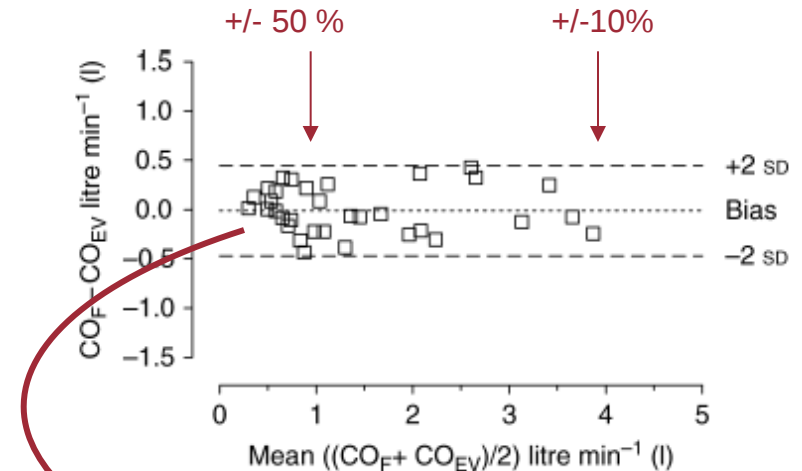
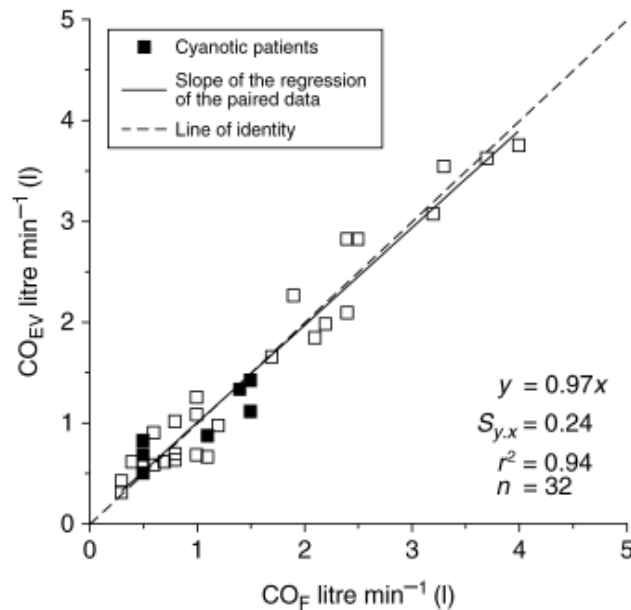
Sztark François, MD, PhD



Doesn't run in adult
Doesn't run in children

Electrical velocimetry for measuring cardiac output in children with congenital heart disease

K. Norozi^{1*}†, C. Beck¹†, W. A. Osthaus², I. Wille¹, A. Wessel¹ and H. Bertram¹

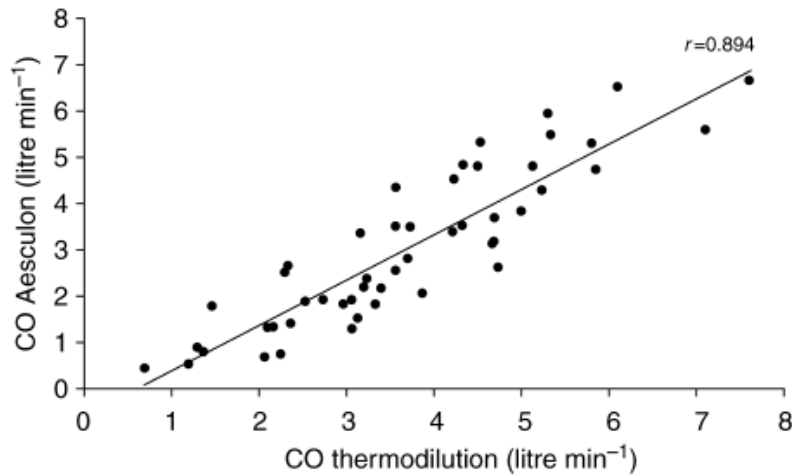


IMPEDANCE

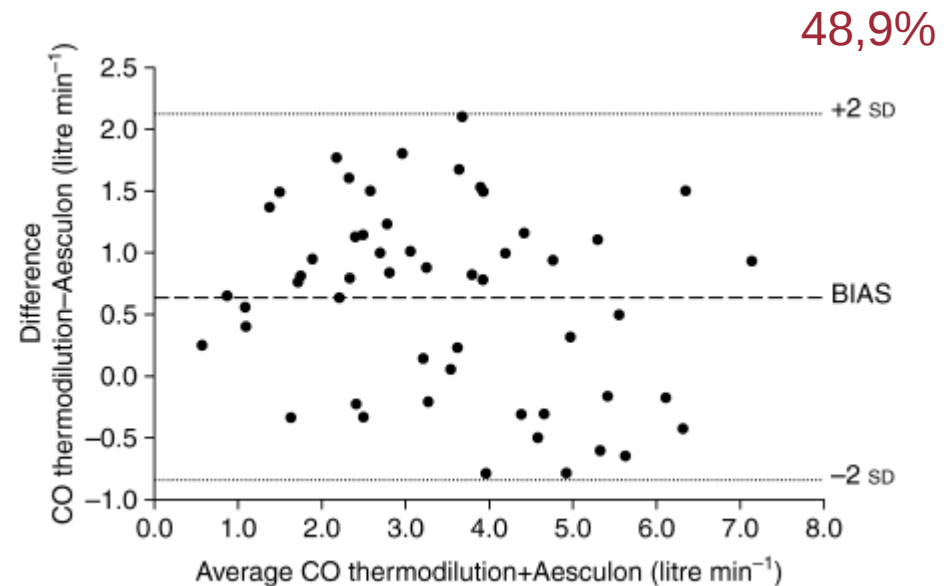
Cardiac output measurement in children: comparison of Aesculon[®] cardiac output monitor and thermodilution

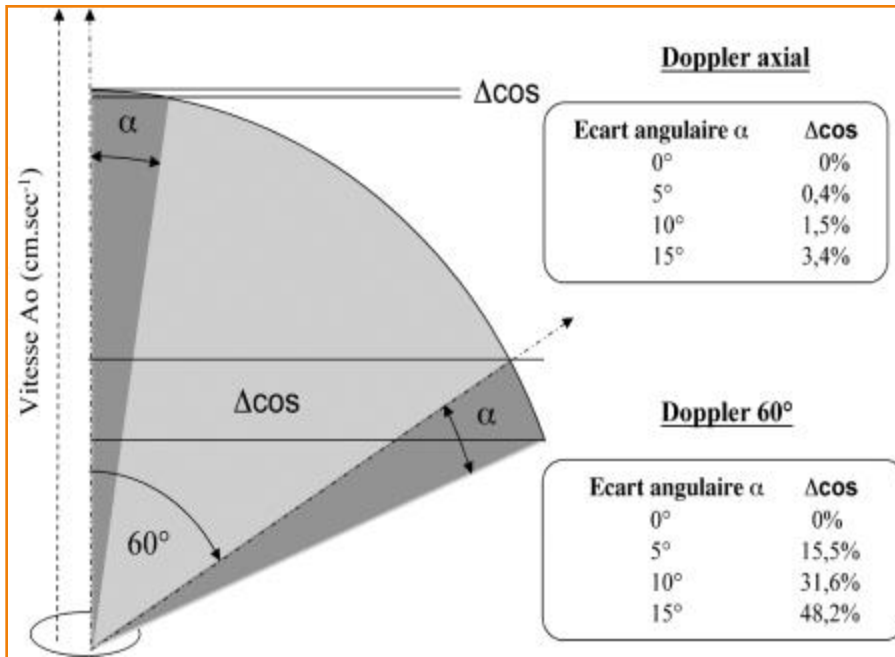
M. Tomaske^{1*}, W. Knirsch¹, O. Kretschmar¹, K. Woitzek^{1 2}, C. Balmer¹, A. Schmitz²,
U. Bauersfeld¹, M. Weiss² and on behalf of the Working Group on Non-invasive
Haemodynamic Monitoring in Paediatrics

50 patients
median (range) age of 7.5 (0.5–16.5) yr



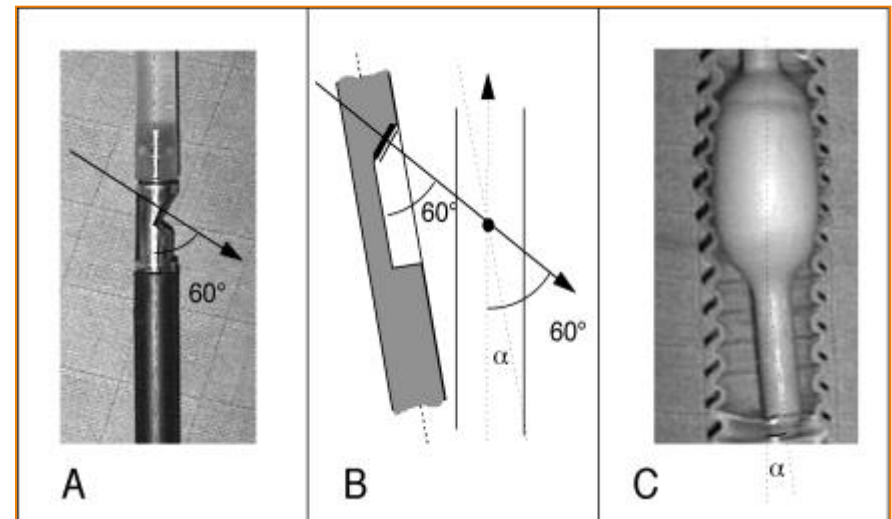
... electrical velocimetry using the Aesculon monitor did not provide reliable CO values in children with congenital heart diseases when compared with PAC thermodilution





Angle 60°

Doppler Oesophagien



Wodey et al. Paediatric Anaesthesia 2001

Walter Knirsch
Oliver Kretschmar
Maren Tomaske
Kathrina Stutz
Nicole Nagdyman
Christian Balmer
Achim Schmitz
Dominique B  ttex
Felix Berger
Urs Bauersfeld
Markus Weiss

Cardiac output measurement in children: comparison of the Ultrasound Cardiac Output Monitor with thermodilution cardiac output measurement

24 patients aged 0.1–16.7 years (median 7.6) and weighing 3.4–51.0 kg (23.0 kg).

.....were excluded a residual shunt following device closure or a residual pulmonary valve regurgitation by transesophageal echocardiography and/or angiography.



USCOM device

Cardiac output measurement in children: comparison of the Ultrasound Cardiac Output Monitor with thermodilution cardiac output measurement

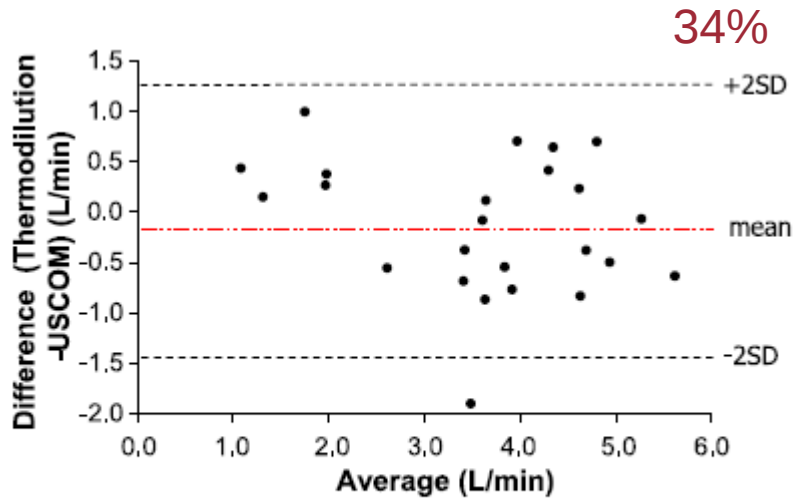


Fig. 2 Bland–Altman analysis to compare cardiac output values obtained by the USCOM and the thermodilution technique in 24 cardiac pediatric patients

- The CO value is calculated using the flow integral, and the **aortic valve diameter** as given by the USCOM internal algorithm based on height and gender.
- Use blind Doppler probe (**continuous Doppler**)

Author's conclusion.....USCOM cannot be recommended for the assessment of absolute CO values in pediatric cardiac patients

Plus récemment !

Philippe Durand
Laurent Chevret
Sandrine Essouri
Vincent Haas
Denis Devictor

Respiratory variations in aortic blood flow predict fluid responsiveness in ventilated children

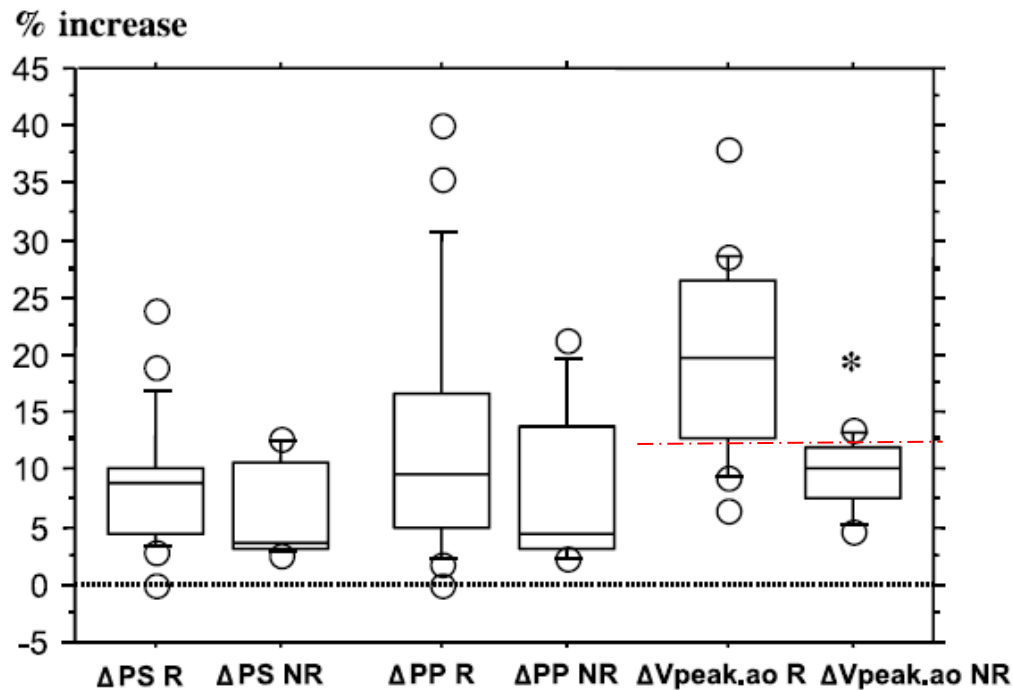
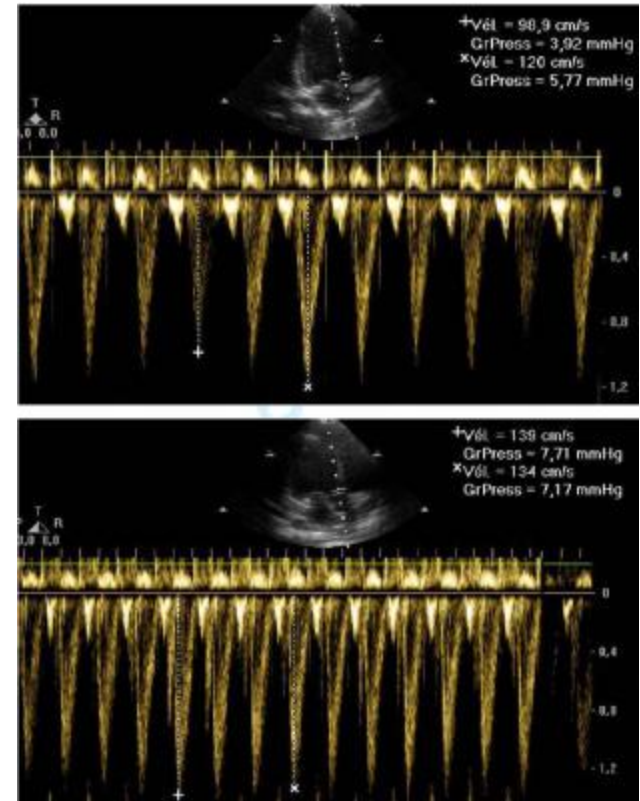


Fig. 1 Δ PS, Δ PP and Δ Vpeak ao at baseline expressed in plot box form (median, interquartile range) in volume expansion-responders (R, $n = 18$) and non-responders (NR, $n = 8$). Values expressed in percent; * $p < 0.001$



Pierre Squara
Dominique Denjean
Philippe Estagnasie
Alain Brusset
Jean Claude Dib
Claude Dubois

Noninvasive cardiac output monitoring (NICOM): a clinical validation

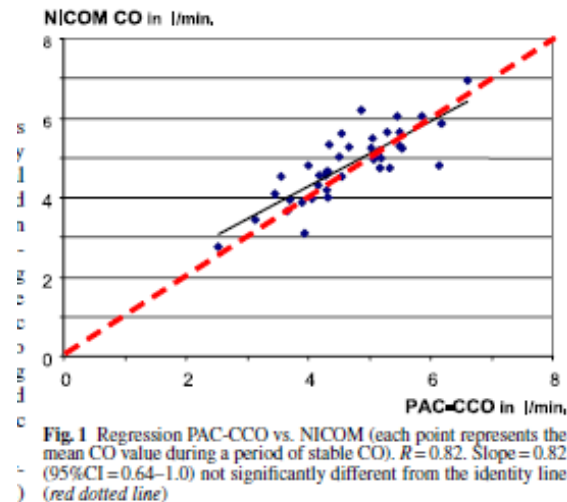


Table 1 CO changes after hemodynamic challenges

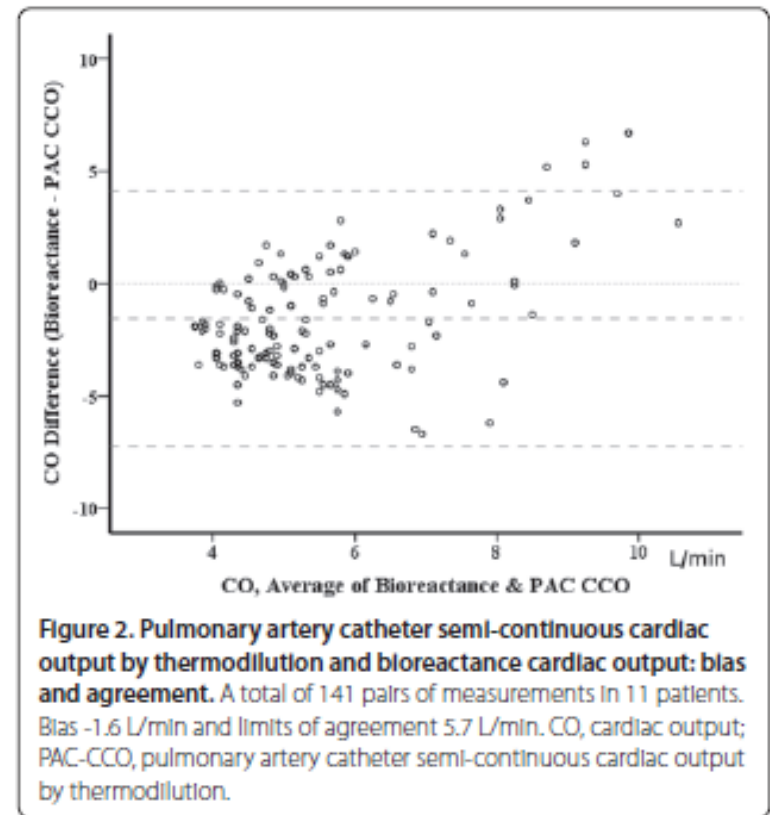
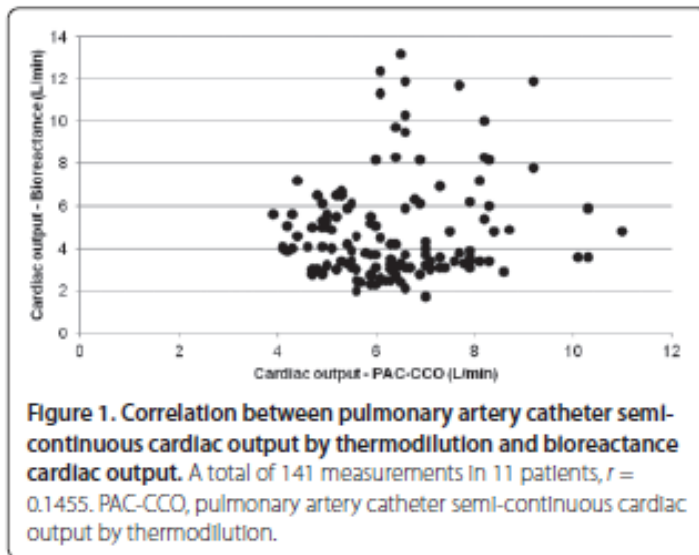
	NICOM	PAC-CCO	<i>p</i>
Negative CO challenge (<i>n</i> = 14)			
Lag time (min)	3.4 ± 1.3	7.1 ± 3.1	0.01
Amplitude (l/min)	-1.7 ± 1.0	-1.7 ± 1.2	0.25
Amplitude (%)	-28 ± 14	-34 ± 20	0.25
Positive CO challenge (<i>n</i> = 23)			
Lag time (min)	4.0 ± 2.2	6.8 ± 3.2	0.003
Amplitude (l/min)	1.5 ± 0.9	1.7 ± 1.3	0.07
Amplitude (%)	40 ± 26	50 ± 33	0.07

Adulte : Ca marche !

Intensive Care Med 2007; 33:1191–1194

Cardiac output measurements using the bioreactance technique in critically ill patients

David Fagnoul, Jean-Louis Vincent and Daniel De Backer*



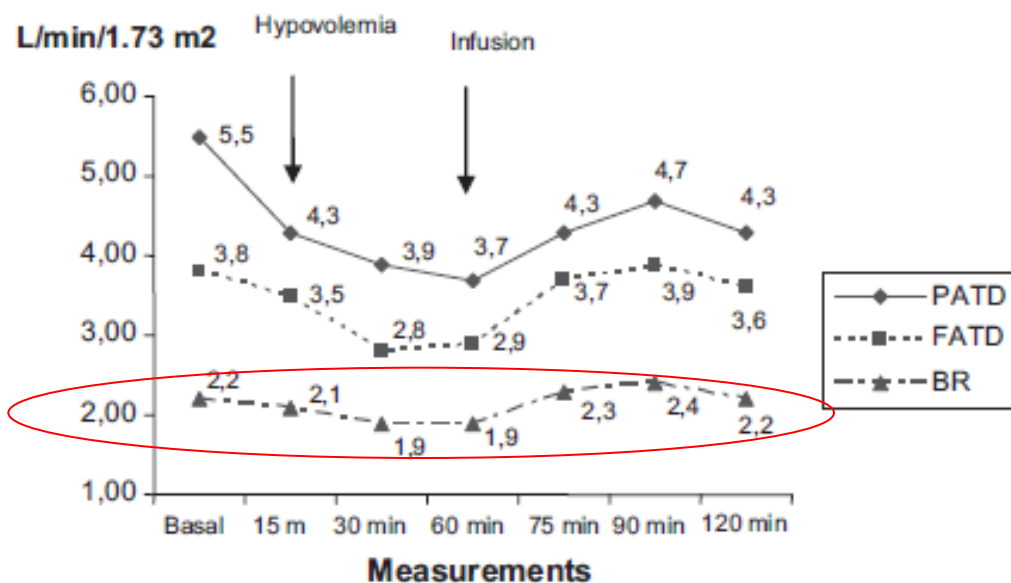
Adulte : Ça marche plus !

Critical Care 2012, **16**:460

Experimental paper

Pulmonary arterial thermodilution, femoral arterial thermodilution and bioreactance cardiac output monitoring in a pediatric hemorrhagic hypovolemic shock model[☆]

Yolanda Ballesteros^{a,c}, Javier Urbano^{a,c}, Jesús López-Herce^{a,c,*}, Maria J. Solana^{a,c}, Marta Botrán^{a,c}, Diego Vinciguerra^{a,c}, Jose M. Bellón^{b,d}



Modèle enfant = Cochon

Fig. 4. Changes in the CI measured by pulmonary artery thermodilution (PATD), femoral artery thermodilution (FATD) and bioreactance (BR).

[Br J Anaesth](#). 2013 Aug 28. [Epub ahead of print]

Bioreactance is not reliable for estimating cardiac output and the effects of passive leg raising in critically ill patients.

[Kupersztynch-Hagege E](#), [Teboul JL](#), [Artigas A](#), [Talbot A](#), [Sabatier C](#), [Richard C](#), [Monnet X](#).

Hôpitaux universitaires Paris-Sud, Hôpital de Bicêtre, service de réanimation médicale, 78, rue du Général Leclerc, F-94270 Le Kremlin-Bicêtre, France.

Abstract

BACKGROUND: Bioreactance estimates cardiac output in a non-invasive way. We evaluated the ability of a bioreactance device (NICOM®) to estimate cardiac index (CI) and to track relative changes induced by volume expansion.

METHODS: In 48 critically ill patients, we measured CI estimated by the NICOM® device (CI_{NICOM}) and by transpulmonary thermodilution (CI_{td} , PiCCO2™ device) before and after a 500 ml saline infusion. Before volume expansion, we performed a passive leg raising (PLR) test and measured the changes it induced in CI_{NICOM} and in pulse contour analysis-derived CI.

RESULTS: Considering the values recorded before PLR and before and after volume expansion ($n=144$), the bias (lower and upper limits of agreement) between CI_{td} and CI_{NICOM} was 0.9 (-2.2 to 4.1) litre $min^{-1} m^{-2}$. The percentage error was 82%. There was no significant correlation between the changes in CI_{td} and CI_{NICOM} induced by volume expansion ($P=0.24$). An increase in CI estimated by pulse contour analysis $>9\%$ during the PLR test predicted fluid responsiveness with a sensitivity of 84% (95% confidence interval 60-97%) and a specificity of 97% (95% confidence interval 82-100%). The area under the receiver operating characteristic curve constructed to test the ability of the PLR-induced changes in CI_{NICOM} in predicting fluid responsiveness did not differ significantly from 0.5 ($P=0.77$).

CONCLUSIONS: The NICOM® device cannot accurately estimate the cardiac output in critically ill patients. Moreover, it could not predict fluid responsiveness through the PLR test.

Adulte : Ca marche plus !

Measurement of Cardiac Output in Children by Bioreactance

Yolanda Ballesteró • Jesús López-Herce •
Javier Urbano • María José Solana •
Marta Botrán • Jose M. Bellón • Angel Carrillo

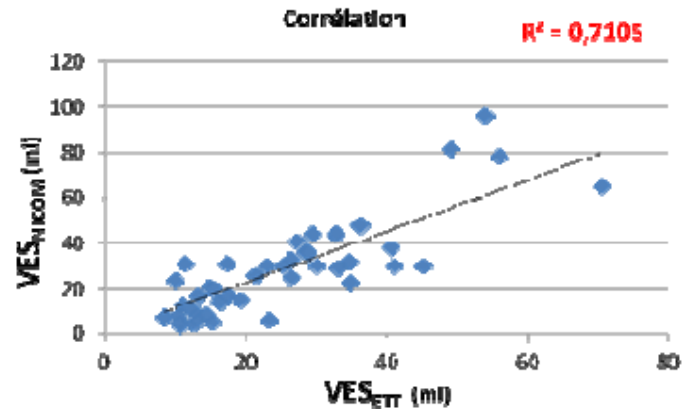
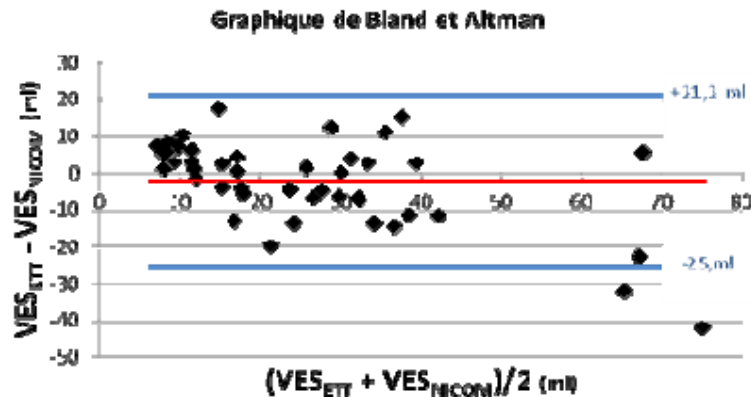
...These data suggest that this method is not useful for evaluating CI in small children.

Enfant : Ça marche pas !

Pediatr Cardiol 2010; 32:469–472

R076

Comparaison de deux méthodes de mesure du volume d'éjection systolique (VES) chez l'enfant :
bioréactance thoracique par NICOM® et échocardiographie trans-thoracique



Matériel et Méthodes: Il s'agit d'enfants âgés de 0 à 16 ans, nées neurochirurgie pouvaient être incl

Comment est calculé le VES (en bioréactance ?)

La bioeactance : une nouvelle technologie pour le monitoring non invasif du débit cardiaque

Bioreactance: A new technology for non invasive cardiac ouput monitoring

P. Squara

individuellement à une erreur significative. Pour résoudre ce problème, un facteur de calibration (CF) multivarié a été déterminé basé sur l'âge, le sexe, la taille, le poids, la surface cutanée, le body mass index (BMI) et si disponibles, la pression artérielle pulmonaire estimée qualitativement et la taux d'hémoglobine. La formule finale du débit cardiaque par bioeactance est donc :

$$DC = FC \cdot \frac{CF}{Z_0^2} \cdot VET \cdot \frac{dX}{dt} \max .$$

$$VES = \frac{CF}{Z_0^2} \cdot VET \cdot \frac{dX}{dt} \max .$$
$$= BSA \times VESI$$

Noninvasive cardiac output measurement using bioreactance in postoperative pediatric patients

Estelle Vergnaud, Charles Vidal, Juliette Montmayeur Verchere, Hanna Taright, Philippe G. Meyer, Pierre A. Carli & Gilles A. Orliaguet

Service d'Anesthésie Réanimation, Hôpital Universitaire Necker – Enfants Malades, Université Paris Descartes, Assistance Publique-Hôpitaux de Paris, Paris, France

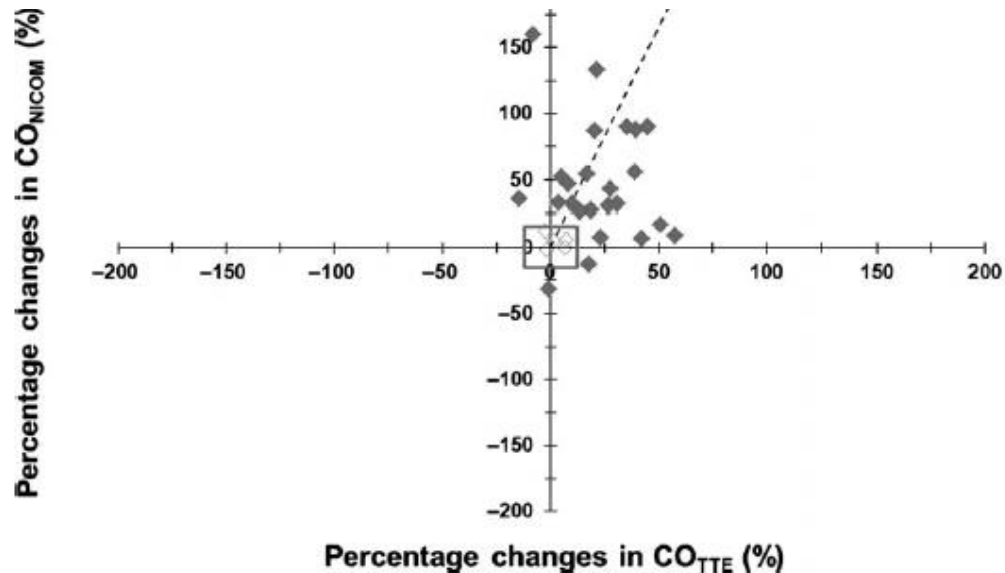
$$\text{CO}_{\text{Nicom}} = \text{HR} \times (\Delta X / \Delta t_{\text{max}}) \times (k' / Z_0^2)$$

with ΔX : system reactance variation, Δt_{max} : left ventricular ejection time, k' : correction factor taking into account the sex and the size of the patient, and Z_0 : initial thoracic impedance.

Noninvasive cardiac output measurement using bioreactance in postoperative pediatric patients

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Variations de Q dans le même sens, mais variations de VES ? (Effect FC ?)

Peut être un synthèse ?

Where do we go from here? Cardiac output determination in pediatrics*

Brian D. Hanna, MD, PhD
Division of Cardiology
Children's Hospital of
Philadelphia
The School of Medicine
University of Pennsylvania
Philadelphia, PA

Transpulmonary thermodilution uses central venous (not pulmonary arterial) and arterial catheters (4F) and gives cardiac output

...thoracic bioimpedance estimates of cardiac output are not robust under all loading conditions.

Transthoracic echo Doppler evaluation has been standard in pediatrics for several years and, in experienced hands, **can also give excellent cardiac anatomical data.**

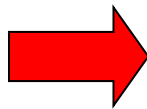
The transesophageal echo Doppler technique has been adapted in the pediatric intensive care unit for more continuous CO measurements since the probe position is more stationary and probe sizes are now small enough for most children. But with changes in load and/or contractility, there is a change in the aortic diameter that limits the trend analysis without remeasurement.

Predicting Fluid Responsiveness in Children: A Systematic Review

Heng Gan, MBBCh, MRCPCH, FRCA,*† Maxime Cannesson, MD, PhD,‡
John R. Chandler, MBBCh, FCARCSI, FDSRDS,§ and
J. Mark Ansermino, MBBCh, MSc (Inf), FFA (SA), FRCPC*†

CONCLUSIONS: Respiratory variation in aortic blood flow peak velocity was the only variable shown to predict fluid responsiveness in children. Static variables did not predict fluid responsiveness in children, which was consistent with evidence in adults. Dynamic variables based on arterial blood pressure did not predict fluid responsiveness in children, but the evidence for dynamic variables based on plethysmography was inconclusive. (Anesth Analg 2013;117:1380–92)

	Potential predictor	Area under ROC with 95% CI (numerical value on right, vertical line is 0.5)	Fluid bolus, n	Setting	Study
Clinical	HR		0.55 33	Neuro OR	Byon ²⁴
			0.62 19	Neuro OR, 0-6 yrs	Pereira de Souza Neto ⁶
			0.66 11	Neuro OR, 6-14 yrs	Pereira de Souza Neto ⁵
	SAP		0.53 27	Cardiac OR	Renner 2011 ⁸
Preload pressure	CVP		0.47 33	Neuro OR	Byon ²⁴
			0.61 19	Cardiac cath	Chandler ⁵
			0.48 21	Cardiac PICU	Choi ²
			0.61 26	Cardiac OR, ASD/VSD	Renner 2012 ⁷
			0.69 26	Cardiac OR, closed ASD/VSD	Renner 2012 ⁷
			0.57 27	Cardiac OR	Renner 2011 ⁸
			0.41 65	Mixed PICU	Saxena ⁹
			0.60 58	Cardiac PICU	Tibby ²⁵
			0.51 36	General PICU	Tibby ²⁵
			0.58 44	Cardiac OR	Tran ²⁶
Thermodilution & US dilution	PAOP		0.67 19	Cardiac cath	Chandler ⁵
	GEDVI		0.59 26	Cardiac OR, ASD/VSD	Renner 2012 ⁷
			0.77 26	Cardiac OR, closed ASD/VSD	Renner 2012 ⁷
	ACV		0.47 65	Mixed PICU	Saxena ⁹
	CBV		0.53 65		
Echocardiography & Doppler	TEDV		0.44 65		
	TEF		0.45 65		
	LVEDA		0.59 19	Neuro OR, 0-6 yrs, TTE	Pereira de Souza Neto ⁵
			0.71 11	Neuro OR, 6-14 yrs, TTE	Pereira de Souza Neto ⁵
	SVI		0.90 50	General OR, TED	Raux ³
	FTc		0.54 58	Cardiac PICU, TED	Tibby ²⁵
			0.76 36	General PICU, TED	Tibby ²⁵



	Potential predictor	Area under ROC with 95% CI (numerical value on right, vertical line is 0.5)	Fluid bolus, n	Setting	Study
Arterial pressure	PPV		0.54 33	Neuro OR	Byon ²⁴
			0.60 19	Cardiac cath	Chandler ⁵
			0.59 26	General PICU	Durand ¹
			0.52 19	Neuro OR, auto PPV, 0-6 yrs	Pereira de Souza Neto ⁶
			0.60 11	Neuro OR, auto PPV, 6-14 yrs	Pereira de Souza Neto ⁶
			0.71 19	Neuro OR, manual PPV, 6-14 yrs	Pereira de Souza Neto ⁵
	SPV		0.60 11	Neuro OR, manual PPV, 6-14 yrs	Pereira de Souza Neto ⁶
			0.79 26	Cardiac OR, ASD/VSD	Renner 2012 ⁷
			0.86 26	Cardiac OR, closed ASD/VSD	Renner 2012 ⁷
			0.61 65	Mixed PICU	Saxena ⁹
			0.58 33	Neuro OR	Byon ²⁴
			0.65 26	General PICU	Durand ¹
Plethysmography	SVV		0.58 65	Mixed PICU	Saxena ⁹
			0.74 44	Cardiac OR	Tran ²⁶
			0.70 26	Cardiac OR, ASD/VSD	Renner 2012 ⁷
			0.78 26	Cardiac OR, closed ASD/VSD	Renner 2012 ⁷
	ΔDown		0.62 33	Neuro OR	Byon ²⁴
	ΔUp		0.64 33	Neuro OR	Byon ²⁴
	ΔPOP		0.56 19	Cardiac cath	Chandler ⁵
			0.51 19	Neuro OR, 0-6 yrs	Pereira de Souza Neto ⁶
			0.57 11	Neuro OR, 6-14 yrs	Pereira de Souza Neto ⁵
Echocardiography & Doppler	PVI		0.77 33	Neuro OR	Byon ²⁴
			0.54 19	Cardiac cath	Chandler ⁵
			0.63 19	Neuro OR, 0-6 yrs	Pereira de Souza Neto ⁶
			0.54 11	Neuro OR, 6-14 yrs	Pereira de Souza Neto ⁶
			0.78 27	Cardiac OR	Renner 2011 ⁸
			0.80 33	Neuro OR, TTE	Byon ²⁴
	ΔV _{peak}		0.83 21	Cardiac PICU, TTE	Choi ²
			0.85 26	General PICU, TTE	Durand ¹
			1.00 19	Neuro OR, 0-6 yrs, TTE	Pereira de Souza Neto ⁶
			1.00 11	Neuro OR, 6-14 yrs, TTE	Pereira de Souza Neto ⁶
			0.92 27	Cardiac OR, TEE	Renner 2011 ⁸
			0.84 27	Cardiac OR, TEE	Renner 2011 ⁸
PLR	ΔVTI		0.37 33	Neuro OR, TTE	Byon ³
	ΔIVCD		0.85 21	Cardiac PICU, TTE	Choi ²
	ΔCI _{IR}		0.71 40	General PICU, TTE	Lukito ⁴
	ΔSV _{IR}		0.75 40	General PICU, TTE	Lukito ⁴

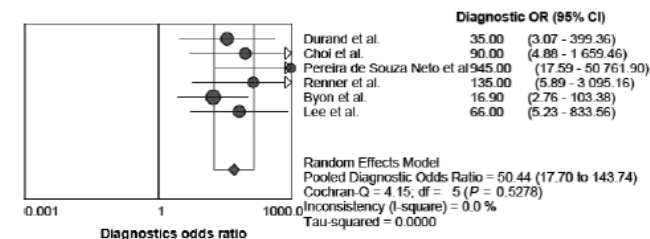
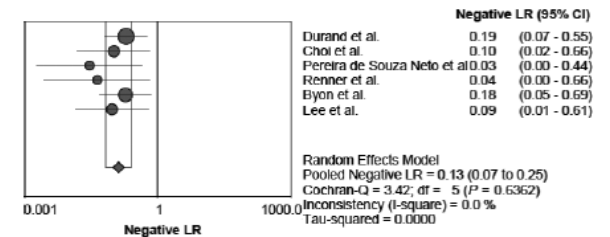
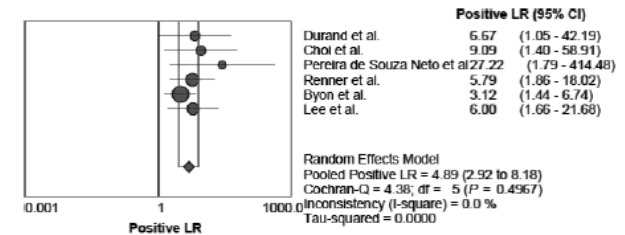
Respiratory variation in aortic blood flow peak velocity to predict fluid responsiveness in mechanically ventilated children: a systematic review and meta-analysis

François-Pierrick Desgranges¹, Olivier Desebbe², Edmundo Pereira de Souza Neto^{3,4,5}, Darren Raphael⁶ & Dominique Chassard¹

Table 3 Results of the studies included in the systematic review

References	Sample size (n)	Percentage of responders (%)	Best threshold value (%)
Durand <i>et al.</i> (17)	26	69.2	12
Choi <i>et al.</i> (18)	21	52.4	20
Pereira de Souza Neto <i>et al.</i> (19)	30	56.7	10
Renner <i>et al.</i> (20)	27	48.1	7
Byon <i>et al.</i> (21)	33	45.5	11
Lee <i>et al.</i> (22)	26	50.0	14

ROC, receiver operating characteristic; CI, confidence interval.



Les moyens pour réfléchir

- Facteurs influençant le VES (précharge, etc...)
- Débit cardiaque, PAM, etc...
- Transport d'oxygène (Q, Sao2, Hb)
- Extraction (SvO2, etc...)
- Oxygénation
 - Sao2 main D et G (réouverture CA)
 - Tissulaire (NIRS)
- Marqueurs terminaux « simple » : Lactate

Peripheral Muscle Near-Infrared Spectroscopy in Neonates: Ready for Clinical Use? A Systematic Qualitative Review of the Literature

Nina Höller Berndt Urlsberger Lukas Miledler Nariae Baik
Bernhard Schwabegger Gerhard Pichler

Division of Neonatology, and Research Unit for Neonatal Micro- and Macrocirculation, Department of Pediatrics,
Medical University, Graz, Austria

Sevoflurane anesthesia and brain perfusion

Ossam Rhondali^{1,2}, Agnès Pouyau¹, Aurélie Mahr¹, Simon Juhel¹, Mathilde De Queiroz¹, Khalid Rhzioual-Berrada¹, Sylvain Mathews² & Dominique Chassard¹

1 Department of Pediatric Anesthesia, Hôpital Mère-Enfant, Lyon, France

2 Department of Pediatric Anesthesia, Hôpital Sainte Justine, Montréal, QC, Canada

Nourrissons de moins de 6 mois, 1 MAC sevoflurane

- PAM > 45mmHg : CBF et rSO₂c ok
- PAM 45 et 35 mmHg : CBF $\searrow$ mais balance O₂ , variation + de rSO₂c (car CMRO₂ $\searrow$)
- **PAM < 35 mmHg**: CBF $\searrow$ et peu de variation+ de rSO₂c (état limite ?)

Conclusion

Dans tous les cas

Restez curieux

Comme un enfant !

