

Echo-Doppler transcrânien Aspects techniques

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Conflits d'intérêt

- Aucun

Echography and Doppler of the Brain

Chiara Robba
Giuseppe Citerio
Editors

Brain ultrasonography: methodology, basic and advanced principles and clinical applications. A narrative review

Chiara Robba¹, Alberto Goffi², Thomas Geeraerts³, Danilo Cardim⁴, Gabriele Via⁵, Marek Czosnyka⁶, Soojin Park⁷, Aarti Sarwal⁸, Llewellyn Padayachy⁹, Frank Rasulo¹⁰ and Giuseppe Citerio¹¹

Take-home message

Brain ultrasonography enables assessment of the main structures of the brain, including the parenchyma and major cerebral vessels.

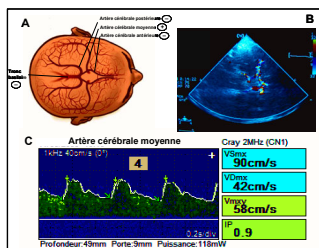
Brain ultrasonography can be performed using commonly used ultrasound systems, through four main acoustic windows (transtemporal, occipital, submandibular and transorbital).

Brain ultrasonography can be used for rapid bedside assessment of pathological changes in neurocritically ill patients, allowing, for example, evaluation of intracerebral haematomas, estimation of raised intracranial pressure, and detection of midline shift and intracranial masses.

Brain ultrasonography is not used exclusively in neurocritical care; clinical applications have been described in different settings, including general intensive care and the emergency department.

Intensive Care Med
<https://doi.org/10.1007/s00134-019-05610-4>

Doppler transcrânien



The British Journal of Radiology, 75 (2002), 615-619 © 2002 The British Institute of Radiology

Short communication

Christian Johann Doppler: the man behind the effect

A ROGUIN, MD

Cardiology Department, Rambam Medical Center, Haifa 31096, Israel

La lumière colorée des étoiles et autres corps célestes
vire au bleu lorsque l'étoile se rapproche de la terre
et vire au rouge lorsqu'elle s'en éloigne

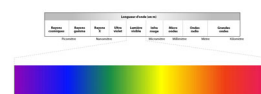


Figure 1. Christian Johann Doppler (1803-1855).

Doppler pulsé



Effet Doppler

Modifications de la fréquence et de la longueur d'onde des ondes réfléchies

$$\Delta f = 2 \cdot f_0 \cdot V/C \cdot \cos\theta$$

Δf : variation de fréquence de l'onde

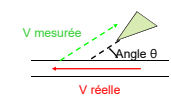
f_0 : fréquence de l'onde émise

V : vitesse du flux sanguin

C : vitesse du son dans le tissu

$\cos\theta$: angle sonde et vaisseau

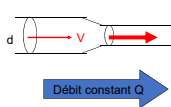
Angle d'insonation



- La vitesse mesurée dépend du cosinus de l'angle d'insonation

$$V_{\text{mesurée}} = \cos \theta \times V_{\text{réelle}}$$

- On sous-estime donc forcément les vitesses...



- A débit constant, la vitesse circulatoire augmente proportionnellement avec la diminution du diamètre du vaisseau

$$V = \text{const.} \times Q / d^2$$

Vitesse n'est pas débit La Garonne

Toulouse



Débit moyen
200 m³/sec

Bordeaux



Débit moyen
700 m³/sec

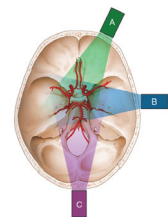
$$Q = V \times \text{section}$$

Chez l'adulte, il y a un os...

- Les fontanelles sont fermées
- Le faisceau d'ultrasons est absorbé en grande partie par l'os
- Pour obtenir un signal acceptable
 - Sonde 2 MHz
 - Sonde 1.8 – 3.6 MHz pour Doppler Couleur
 - Puissance entre 10 and 150 mW/cm²

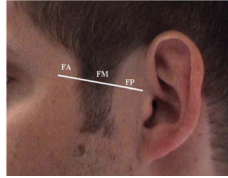
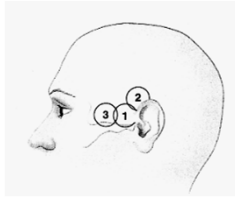
Les fenêtres osseuses

- Transtemporal
- Transorbital
- Sousoccipital
 - Transforamenal
- Sousmandibulaire



Les fenêtres

Temporale



Noninvasive transcranial Doppler ultrasound recording of flow velocity in basal cerebral arteries

RUNE AASLID, PILD., THOMAS-MARC MARKWALDER, M.D., AND HELGE NORNES, M.D.

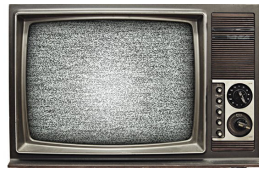
technique during surgery,^{2,8,9} and in children with open fontanels.⁷ In adults, however, the skull is a severe obstacle to the penetration of ultrasound. Bone strongly attenuates the ultrasonic wave, making it impossible to record noninvasively the blood flow velocity from intracranial arteries by conventional Doppler instruments operating in the range from 5 to 10 MHz. At lower frequencies, 1 to 2 MHz, the attenuation in bone and soft tissues is considerably less. The skull bones are of varying thickness, and because the base of the temporal

Doppler recordings of bilateral MCA blood flow velocities were obtained in all 50 subjects. However,

J Neurosurg 57:769-774, 1982

Parfois la fenêtre reste fermée

- Jusqu'à 18% dans les études d'AVC
- Femme
- Age
- Ethnie « non-blanche »



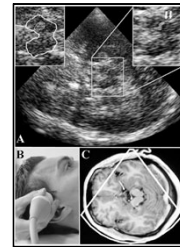
Grolimund P. Transmission of ultrasound through the temporal bone.
In: Aaslid R, ed. Transcranial Doppler sonography. Wien/New York: Springer Verlag, 1985:10-18.

Transcranial sonography of the cerebral parenchyma: Update on clinically relevant applications

Uwe Walter*

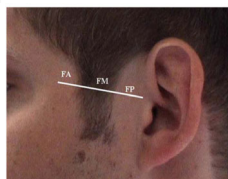
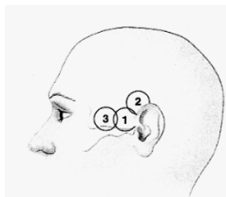
Table 1 Ultrasound system settings for transcranial sonography.

Parameter	Settings
Ultrasound system	Start with 14-16 cm, reduce if needed
Penetration depth	45-55 dB
Dynamic range	Moderate suppression of low echo signals
Postprocessing function	Adjust manually as needed, or use the "tissue optimization" function if available
Time gain compensation	Adjust manually, not too high, or use the "tissue optimization" function if available
Image brightness	As high as possible, ideally, "matrix" probe
Ultrasound transducer	Crystal/channel
Insonation frequency (center frequency)	2.0-3.5 MHz, preferably 2.5 MHz

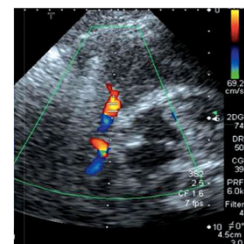


Perspectives in Medicine (2012) 1, 334-343

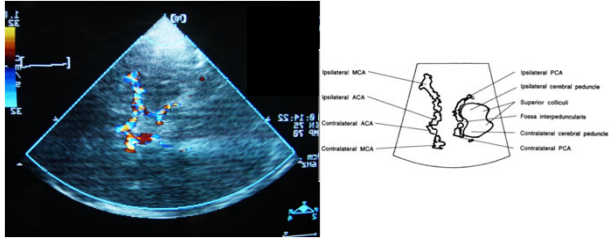
La fenêtre temporelle



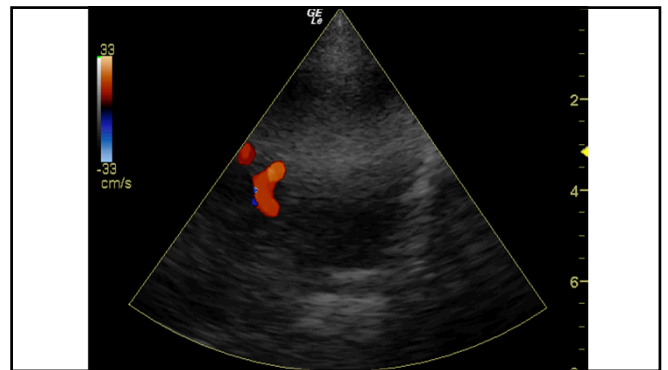
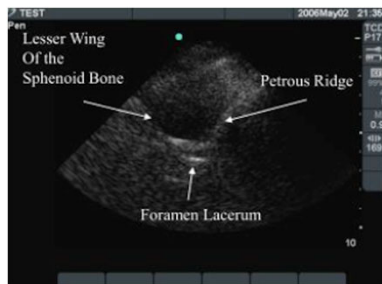
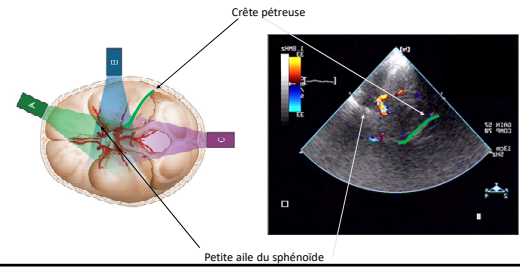
Visualiser le mesencéphale



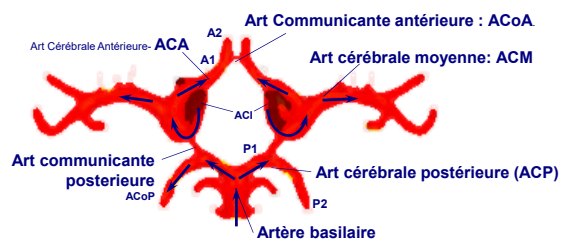
Polygone de Willis



Repères osseux

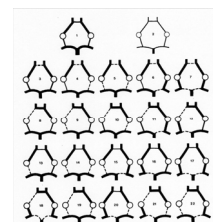


Polygone de Willis

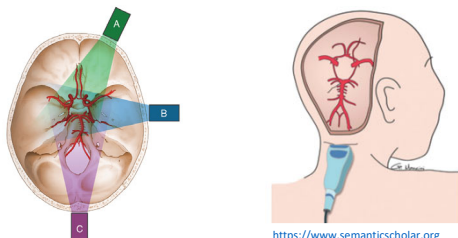


Variantes anatomiques du polygone

- Environ 20% de la population possède un polygone parfait
- 22 variantes

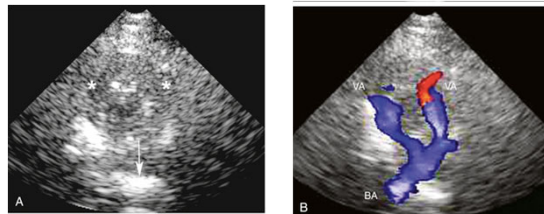


La fenêtre sous-occipitale



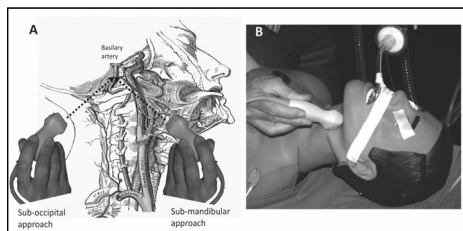
<https://www.semanticscholar.org>

La fenêtre sous-occipitale

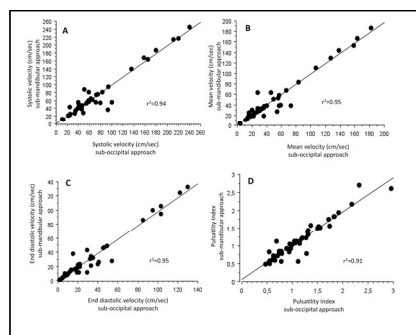


An Alternative Ultrasonographic Approach to Assess Basilar Artery Flow

Thomas Geeraerts, MD, PhD
Wissam Thoms, MD
Sébastien Tansini, MD
Pierre Stienne Lelanc, MD
Jacques Duranton, MD, PhD
Bernard Vigué, MD, PhD

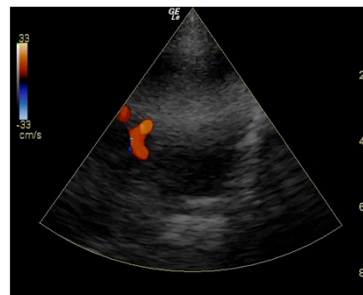


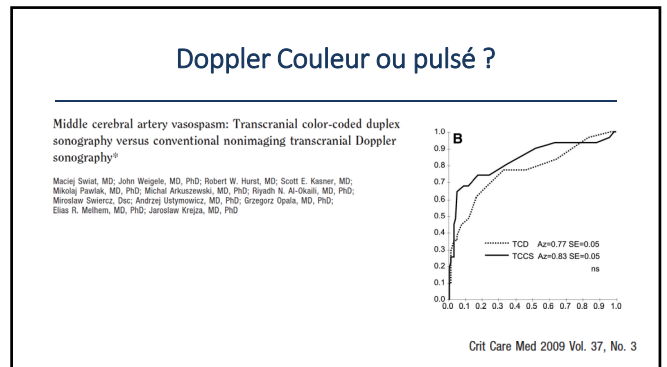
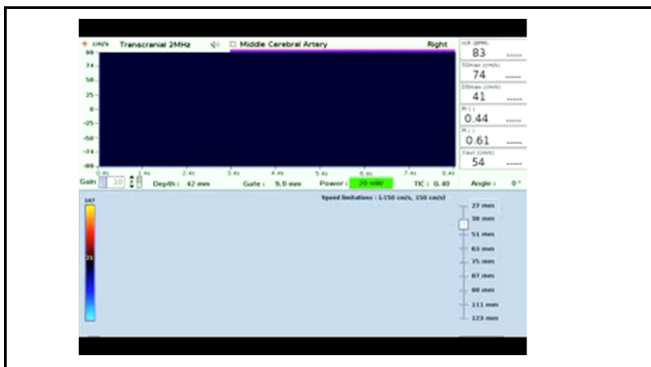
Neurosurgery 68(ONS Suppl 2):ons276-ons281, 2011



Deux méthodes

- Doppler pulsé conventionnel
- Doppler couleur 2D
 - Duplex (couplage échographie-Doppler pulsé)
 - Triplex (couplage échographie, Doppler couleur, Doppler pulsé)





Doppler avec contraste

- Agent de contraste : microsphères lipidiques
- Augmente la précision du DTC
- Efficacité démontrée pour diagnostic
 - Anévrismes
 - MAV, FAV
 - FOP
- Sensibilisation pour confirmation de mort encéphalique ?

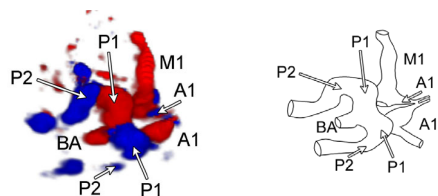
Intraoperative Contrast-Enhanced Ultrasound for Brain Tumor Surgery

71 patients

Neurosurgery 74:542-552, 2014

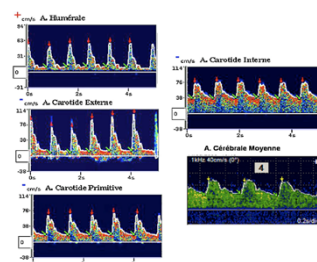
Real-Time 3D Contrast-Enhanced Transcranial Ultrasound and Aberration Correction

Nikolas M. Vancevich¹, Gianmarco F. Pinton², Heather A. Nicoletto³, Ellen Bennett⁴, Daniel T. Laskowitz¹, and Stephen W. Smith¹



Ultrasound Med Biol. 2008 September ; 34(9): 1387-1395

Résistance artérielle



Geeraerts T, Neurochirurgie, 2008

40 % R



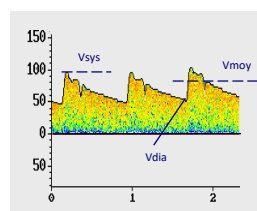
Gros tronc artériel

60 % R



Artérioles

Indices



Index de pulsativité (Gosling)

$$IP = \frac{V_{sys} - V_{dia}}{V_{moy}}$$

Index de résistivité (Pourcelot)

$$IR = \frac{V_{sys} - V_{dia}}{V_{sys}}$$

Valeurs normales

Tableau 1 – Vitesses circulatoires et index de pulsativité : valeurs normales chez l'adulte.

Artère	Profondeur (mm)	Moyenne	Diastolique	Systolique	IR	IP
ACM	40-55	62 ± 12	45 ± 10	90 ± 16	0,4-0,7	0,90 ± 0,24
ACA	60-75	50 ± 13	35 ± 10	71 ± 18		0,83 ± 0,17
ACP	55-80	37 ± 10	26 ± 7	53 ± 11		0,88 ± 0,20
TB	85-100	39 ± 9	31 ± 9	52 ± 9		

ACM : artère cérébrale moyenne ; ACA : artère cérébrale antérieure ; ACP : artère cérébrale postérieure ; TB : Tronc basilaire ; IR : index de résistance ; IP : index de pulsativité

Extra-crânien

- Pressions systémiques
- Volémie
- Tachycardie (↓IP car ↓relaxation diastolique)
- Modification de section dans les artères extra-crâniennes



- Modification de diamètre
- vasospasme
- sténose, occlusion

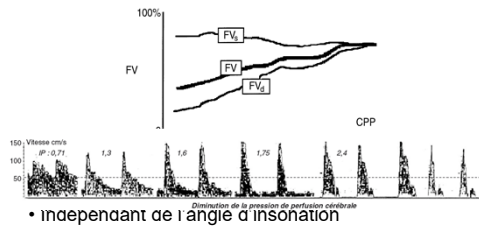


Résistances artérielles

- Hypertension intracrânienne
- Variations de capnie
- Anémie

⇒ Vélocités diastoliques, IP

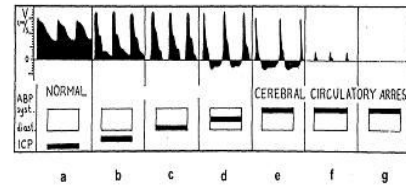
Diminution de la PPC



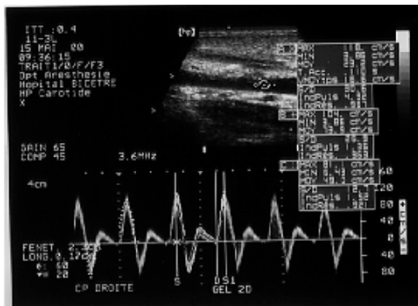
Kirpatrick P, *Head Trauma*, 2000

Bruder N, *EMC*, 2006

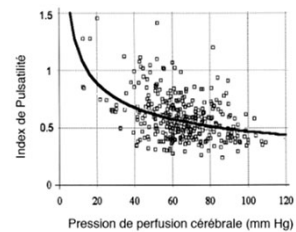
Hypertension intracrânienne



Augmentation des résistances
↓ Vitesse diastolique ↑ IP



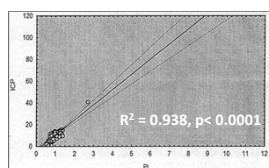
Pression de perfusion cérébrale ?



Czosnyka M, *J Neurosurg*, 1998

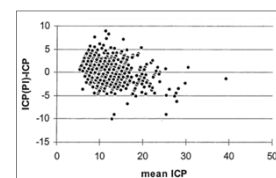
1- Diagnostic de ischémie cérébrale

- Prospective
- n=80 dont 60% HSA et ¼ TC, [2-79 ans]
- Détermination corrélation IP et PIC
 - ⇒ équation de droite de régression linéaire : $PIC_{prédite}$
 - Comparaison $PIC_{mesurée}$ et $PIC_{prédite}$



Bellner J, *Surg Neurol* 2004, 62

1- Diagnostic de ischémie cérébrale

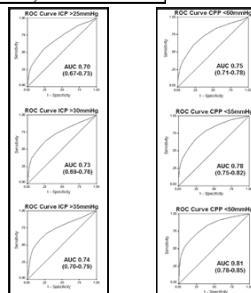


$PIC_{prédite} = PIC_{mesurée} \pm 4.2 \text{ mmHg}$
Dans 95% des cas (précision)

Bellner J, *Surg Neurol* 2004, 62

Reliability of the Blood Flow Velocity Pulsatility Index for Assessment of Intracranial and Cerebral Perfusion Pressures in Head-Injured Patients

290 head-injured patients



Neurosurgery 71:853-861, 2012

Intensive Care Med (2007) 12:445-451
DOI 10.1007/s00134-007-4558-6

ORIGINAL

Catherine Ract
Sophie Le Moine
Nicolas Brédier
Bernard Vignat

Transcranial Doppler ultrasound goal-directed therapy for the early management of severe traumatic brain injury

DTC considéré anormal si au moins 2 des 3 critères suivants:
- Vm < 30 cm/s,
- Vd < 20 cm/s,
- IP > 1.4.

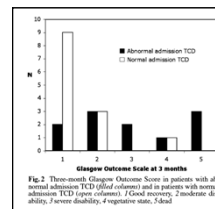


Fig. 2 Three-month Glasgow Outcome Score in patients with abnormal admission TCD (filled columns) and in patients with normal admission TCD (open columns). 1 Good recovery, 2 moderate disability, 3 severe disability, 4 vegetative state, 5 dead

2- Triage et intensification du traitement

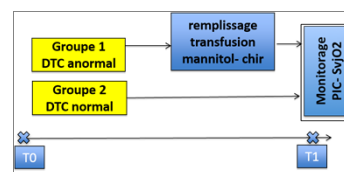
	Abnormal TCD (n = 9)		Normal TCD (n = 9)	
	Group 1	Group 2	Group 1	Group 2
Time from trauma (min)	68 ± 25	143 ± 50	61 ± 14	146 ± 57
Abnormal TCD (n)	9	4	0	0
Systolic velocity (cm/s)	67 ± 21	76 ± 23	79 ± 25	81 ± 17
Mean velocity (cm/s)	28 ± 10 [†]	37 ± 12 [†]	48 ± 14 [†]	53 ± 9 [†]
Diastolic velocity (cm/s)	9 ± 7 [†]	18 ± 11 [†]	33 ± 10 [†]	38 ± 10 [†]
Pulsatility index	2.2 ± 0.6 [†]	1.7 ± 0.4 [†]	0.9 ± 0.3 [†]	0.8 ± 0.3 [†]
MAP (mmHg)	93 ± 25	101 ± 32	72 ± 22	83 ± 19
Haemoglobin (g/dl)	14 ± 1	12	12	12
Arteriovenous malformation (n)	4	2	0	0
Nonreperfusion (n)	—	2	—	3
Mortality (n)	—	7	—	0
Emergency neurosurgery (n)	—	3	—	0
48 h mortality (n)	—	6 [†]	—	1 [†]

- Normalisation par traitement intensif (faisabilité)
- Association doppler ⇔ gravité/prognostic
 - Pas de normalisation: 100% décès, différence entre 2 groupes
 - Doppler initial normal: 0% neurochirurgie

Tazarourte K, Acta Anesth Scand 2011

2- Triage et intensification du traitement

- Etude pilote: prospective, non randomisée, GCS ≤ 8
- Objectifs: FC < 120, PAM > 75, Hb > 10
- Doppler considéré anormal (PPC basse):
 - IP > 1.4, Vd < 20 et Vm < 30 cm.s⁻¹



Ract C, Int Care Med 2007, 33:645-51

Triage

Intensive Care Med (2008) 13:754-760
DOI 10.1007/s00134-008-2636-6

ORIGINAL

Paul Jeffries
Julien Bruns
Philippe Decty
Jean-Luc Besson
Bertrand Fournier
Alfred Schölkens
Daniel Anglade
Claude Jacquet
Jean-François Poyen

Transcranial Doppler to detect admission patients at risk for neurological deterioration following mild and moderate brain trauma

	Group 1	Group 2	p
TCD measurements (cm/s)			
FVm	43 (22-75)	36 (23-51)	0.37
FVs	75 (46-130)	77 (53-112)	0.93
FVd	27 (12-57)	26 (16-37)	0.30
Pulsatility index	1.28 (0.78-2.31)	1.64 (0.96-2.05)	0.05

2- Triage et intensification du traitement

- Prospective, monocentrique, n=98 Trauma GCS [9-15]
 - Marshall 1 et 2
 - doppler « patients stables » vs « dégradation neuro 17 »
 - dégradation: 21/98 (21.4%), 3 décès.

Status on Posttrauma Day 7: Patients With and Without Secondary Neurological Deterioration

	No SND (n = 77)	SND (n = 21)	P
FVm, cm/s	49 (31-80)	31 (18-60)	<.01
FVs, cm/s	84 (47-128)	69 (38-119)	<.01
FVd, cm/s	34 (18-64)	18 (11-36)	<.01
Pulsatility index	1.02 (0.66-1.83)	1.47 (1.07-2.33)	<.01
Injury-to-TCD time, min	215 (42-700)	300 (90-690)	.03

Prediction: Se: 90% / Sp: 91%

Bouzat P, Neurosurgery 2011,68

Transcranial Doppler to Screen on Admission Patients With Mild to Moderate Traumatic Brain Injury

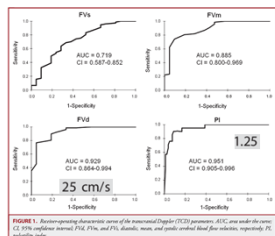
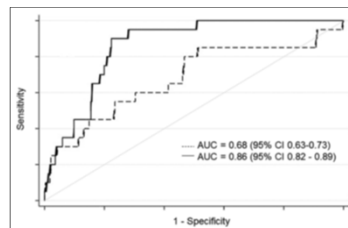


FIGURE 1. Receiver operating characteristic curve of the transcranial Doppler (TCD) parameters. AUC, area under the curve; CI, 95% confidence interval; Pvs, Pvm, Pvd, and PI, diastolic, mean, and systolic cerebral blood flow velocities, respectively; PI, pulsatility index.

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Claude Jacquot, MD*
Stephan Chabardès, MD, PhD‡
Jean-Luc Bouillon, MD, PhD‡
Jean-François Puyes, MD, PhD*

2- Triage et intensification du traitement

- Prospective, multicentrique, n=356 MMTBI = GCS 9 à 15
 - Marshall 2
 - Objectifs: validation seuils IP 1.25 et Vd 25
 - dégradation neuro <17: 20 (6%), 4 décès.



VPN=98%
VPP=18%

Bouzat P et al.,
Anesthesiology
2016

2- Triage et intensification du traitement



R1.4 - Il faut probablement évaluer la gravité initiale des traumatisés crâniens à l'aide du Doppler transcrânien.

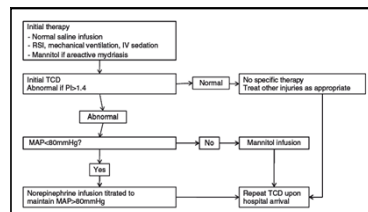
(GRADE 2+) Accord FORT

Argumentaire :

Chez les traumatisés crâniens, l'indice le plus sensible au Doppler transcrânien (TCD) pour détecter la baisse de Pression de Perfusion Cérébrale (PPC) est l'index de pulsatilité (IP). Tant que l'on ne dispose pas d'un monitoring

Pre-hospital transcranial Doppler in severe traumatic brain injury: a pilot study

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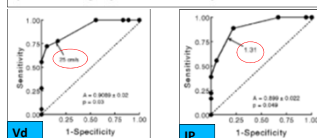
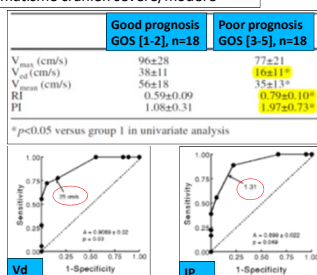


Acta Anaesthesiol Scand 2011; 55: 422-428

2- Triage et intensification du traitement

- Prospective monocentrique, n=36 enfants
- Traumatisme crânien sévère/modéré

Tabard F, Int Care Med 2004; 30



3- Dissection carotidienne

Critères de Denver

- Fractures du rachis cervical
- Déficit neurologique inexpliqué
- Fr base au niveau du canal carotidien
- Fr Lefort II et III
- Hématome cervical
- Souffle cervical < 50 ans
- AVC ischémique
- TCG avec score de GCS < 6
- pendaison

Critères de Memphis

- Fractures du rachis cervical
- Déficit neurologique inexpliqué par l'imagerie cérébrale
- Fr base au niveau du canal carotidien
- Fr Lefort II et III
- Syndrome de CBH
- Lésions des parties molles cervicales

Cothren CC, Clinics 2005

3- Dissection carotidienne

- **Rétrospective**, dissection vs. contrôles appariés 1:4
- Profil doppler cas avec dissection confirmée/CTA

	TICAD	Controls 1	Controls 2	p
FN (cm/s)	51 (23-92)	91 (57-123) ^a	80 (46-115) ^a	<0.01
FN (cm/s)	36 (18-64)	53 (31-73) ^a	35 (25-44) ^a	<0.01
FN (cm/s)	29 (15-53)	40 (18-55) ^a	25 (12-47) ^a	<0.01
PI	0.70 (0.18-1.45)	0.98 (0.68-1.75) ^a	1.36 (0.84-2.09) ^{a, b}	<0.01
PI < 0.80 (n)	10	4	0	<0.01
FN asymmetry (%)	47 (7-86)	12 (0-25) ^a	12 (0-41) ^a	<0.01
FN asymmetry (%)	37 (4-81)	12 (0-29) ^a	15 (0-36) ^a	<0.01
FN asymmetry (%)	29 (0-40)	14 (0-28)	16 (0-50)	0.18
PI asymmetry (%)	46 (16-85)	9 (1-39) ^a	13 (0-53) ^a	<0.01
FN asymmetry >25% (n)	9	0	5	<0.01
PI < 0.80 and FN asymmetry >25% (n)	9	0	0	<0.01

- ↓ vitesses et IP homolatérale à la dissection
- ↑ asymétrie des vitesses si dissection

Bouzat P, Int. Care Med. 2010

3- Dissection carotidienne



Recommandations Formalisées d'Experts 2016

R3.2 - Il faut probablement faire précocement une exploration des troncs supra-aortiques et des vaisseaux intracrâniens par angiotomodensitométrie chez les patients présentant des facteurs de risque.

(GRADE 2+) Accord FORT

Conclusion

- Progrès techniques certains
- Taux de succès augmente
- Anatomie cérébrale et Doppler transcrânien
- Développement futur pour l'anesthésie réanimation
 - Contraste
 - 3D
- Attention à la toxicité des ultrasons

Je vous remercie de votre attention

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